

Introduction to Pharmacokinetics

Novartis-Academia Hackathon

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Overview

- Target Audience: people with a quantitative background that are new to pharmacometrics.
 - Simple, linear differential equations will be used
- Topics covered
 - Absorption, Distribution, Metabolism and Elimination (in reverse order)
 - Clearance (the most important PK parameter)
 - Volume of distribution
 - 1 and 2 compartment models
 - Allometric scaling
- Key take-aways
 - The “fundamental law” of PK: $C_{avg,ss} = \frac{F \cdot Dose}{CL \cdot \tau}$ (true for linear PK)
 - PK models are motivated by known pharmacology, but parameters are empirical and may not directly relate to physiological parameters

Acknowledgements

(Based on material from)

- Rowland, M., Tozer, T. N. *Clinical pharmacokinetics and pharmacodynamics: concepts and applications*
- Peter Bonate, Astellas
- Richard Brundage, U Minnesota
- Leon Aarons, U Manchester
- Jean-Louis Steimer, Novartis
- Martin Fink, Novartis
- Nick Holford, U Auckland
<http://holford.fmhs.auckland.ac.nz/Teaching/pharmacometrics/advanced.php>

Motivation – the importance of finding the right dose of a drug

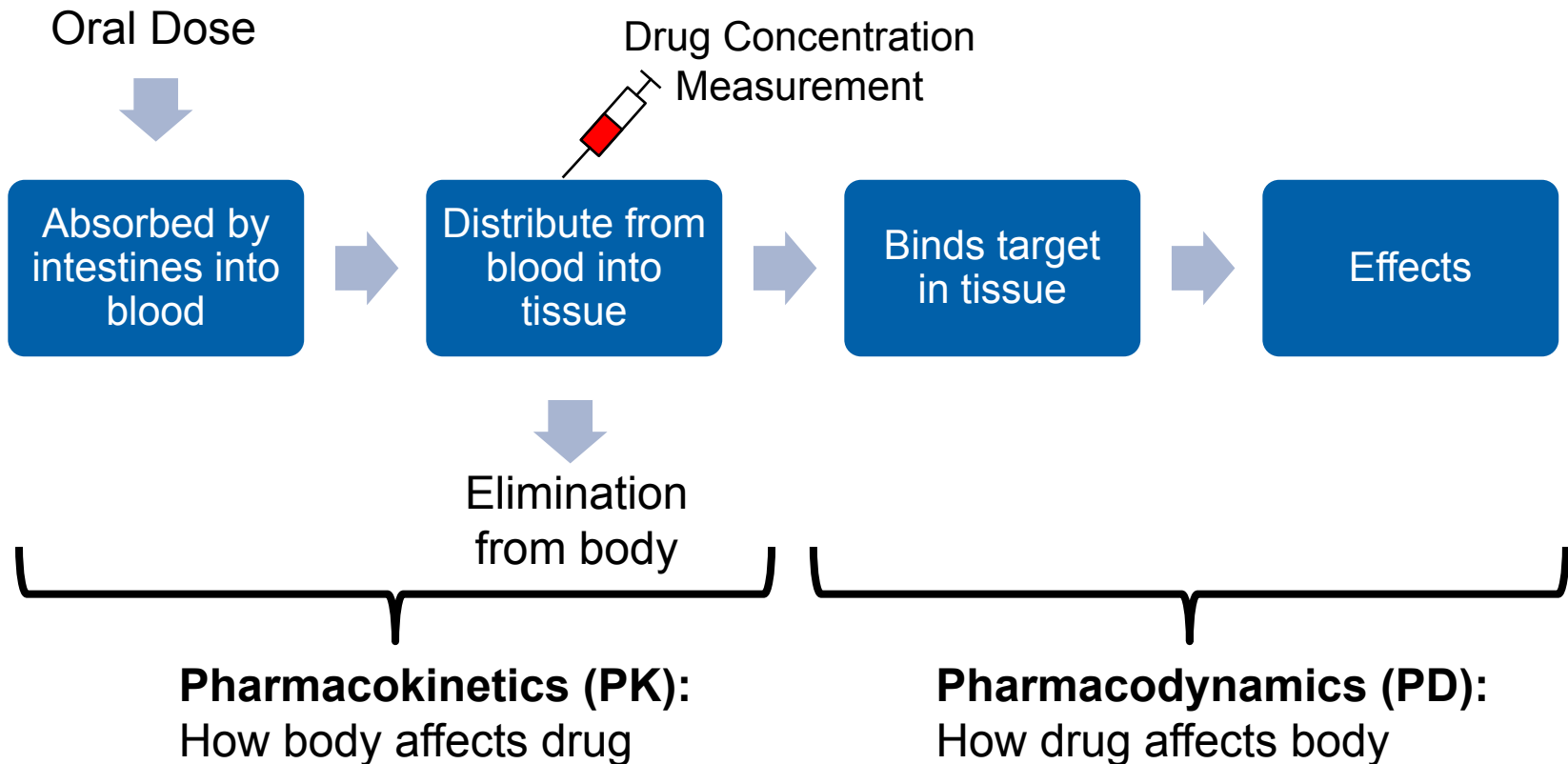
- Tylenol helps to reduce pain and fever and is safe at daily doses $\leq 3,000$ mg/day
- $>5,000$ mg/day can cause liver damage
- $>10,000$ mg/day can be lethal.
- You can learn about safety and efficacy from clinical trials
- Making best use of this data requires models to integrate the data



(paracetamol)

Johnson & Johnson

The “PKPD” pathway of drug effect



Should children and adults receive the same dose?

What dose is needed to shrink a tumor without causing severe neutropenia

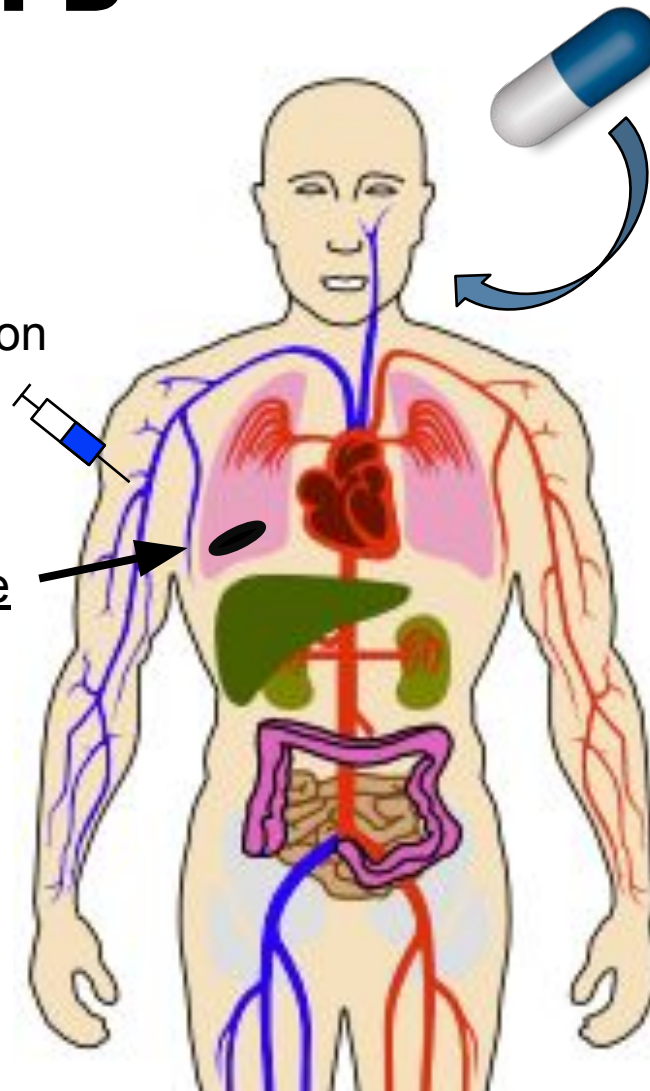
Measuring PKPD

PK (Pharmacokinetics) example

Measurement of drug concentration from circulation

PD (Pharmacodynamics) example

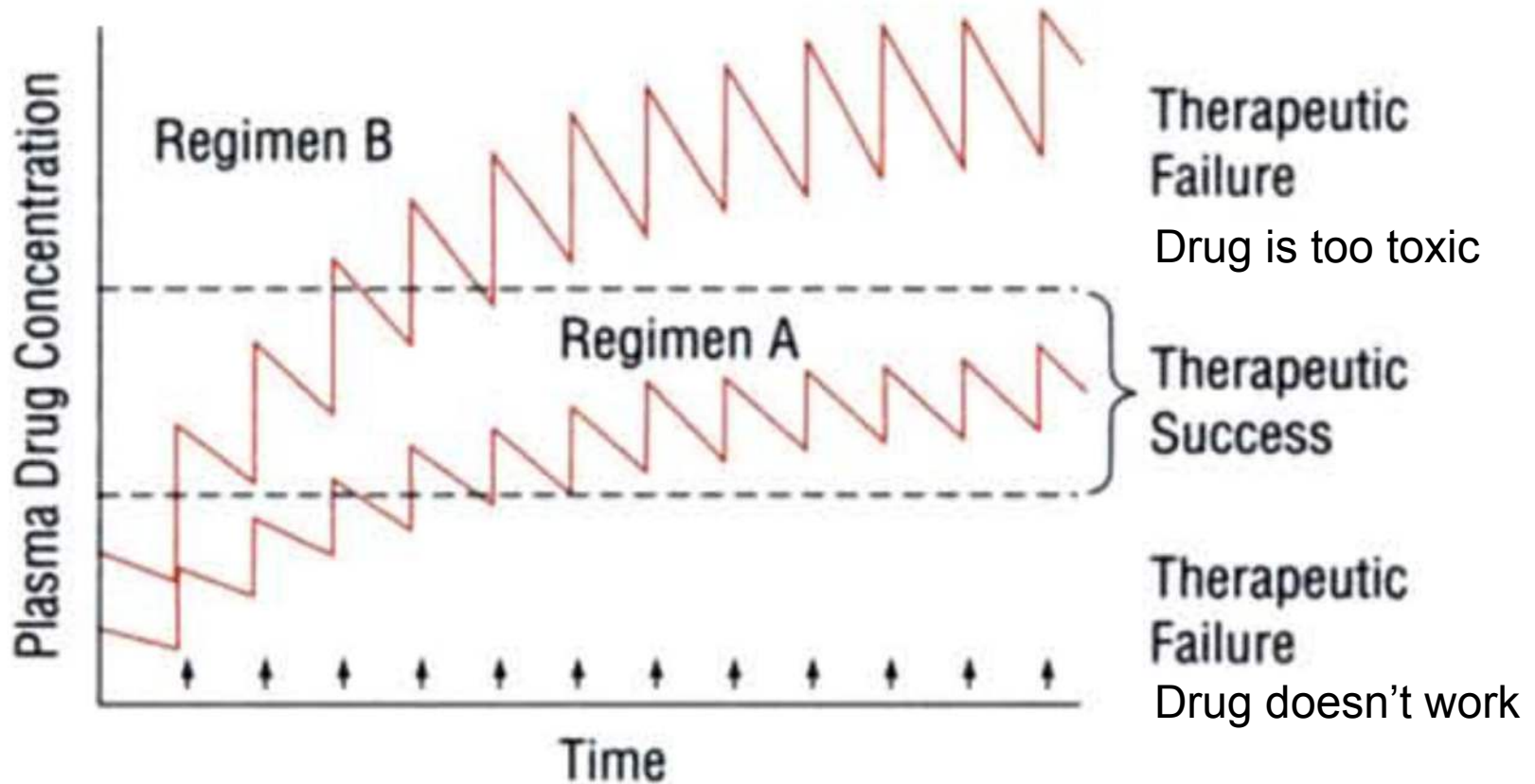
Change in tumor size, as measured by X-Ray



Dose Regimen

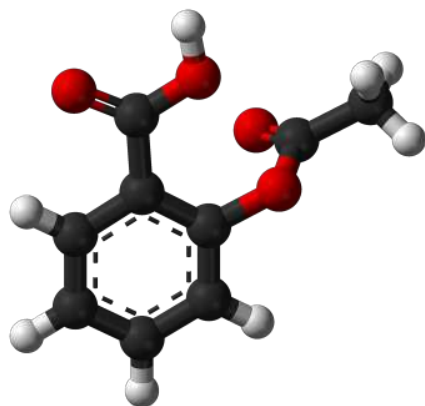
- amount given
- frequency
- method (oral, patch, etc.)

Understanding PKPD can help in picking the optimal dose regimen



Types of Drugs

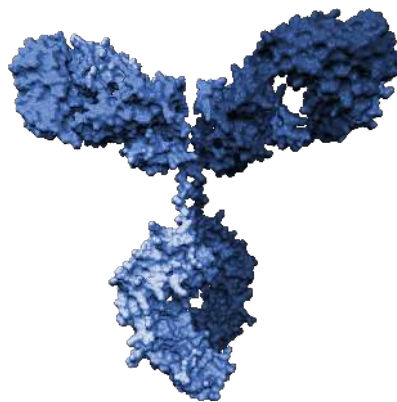
Small Molecule



~1 nm
500 Da

Aspirin
Tylenol

Antibody



~10 nm
150,000 Da

Humira
Keytruda

Cell Based Therapies



100,000 nm
~10¹⁴ Da

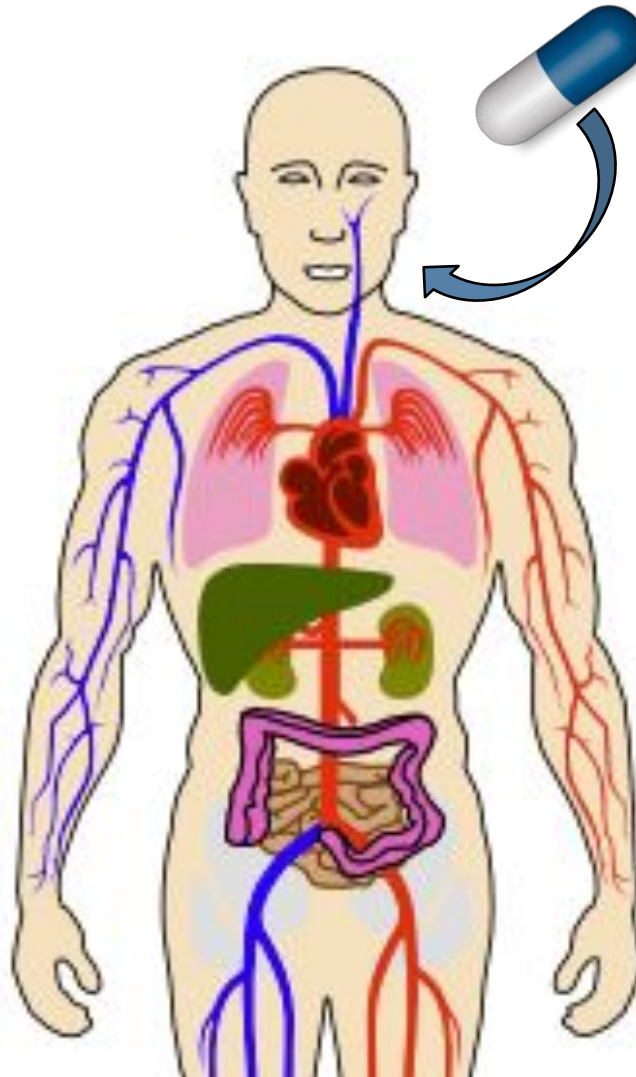
Kymriah
Stem Cell Transplant

Introduction to Pharmacokinetics

Why Do We Measure Blood or Plasma Concentrations When the Site of Action is Somewhere Else?

Key process of pharmacokinetics (ADME)

- Absorption
- Distribution
- Metabolism
- Excretion



Volume of Distribution

Key Lessons

- For intravenous dose
 - Initial Concentration = Dose/Volume
 - Volume is a “theoretical concept” and does not necessarily reflect blood or body volume

Definition of dose and concentration

Dose

Measurement: Mass

Units: mg

Concentration (C)

Measurement: Mass/Volume

Units: mg/ml

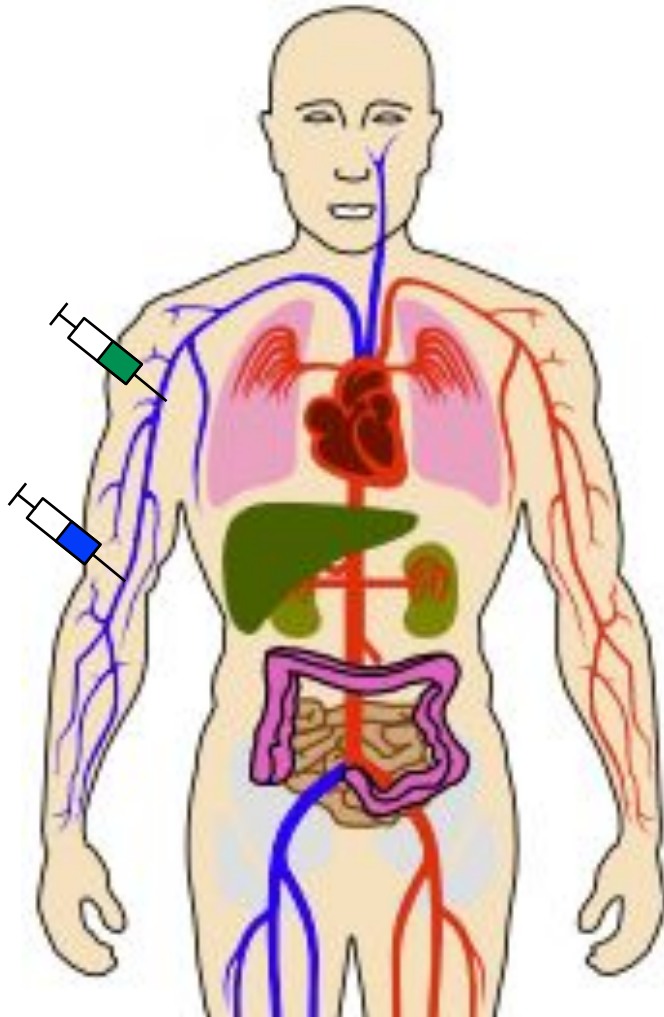
Volume (V)

“Theoretical Volume” needed to contain administered drug at the measured concentration

Key Formula

Right after IV dosing (time = 0)

$$C(0) = \text{Dose}/V \rightarrow V = \text{Dose}/C_0$$



Volume of distribution example

$$C_0 = \text{Dose}/V \quad \text{or} \quad \text{Dose} = C_0 \cdot V$$

Drug Concentration
in Beaker

Drug Concentration
with Activated Charcoal
(absorbs drug)

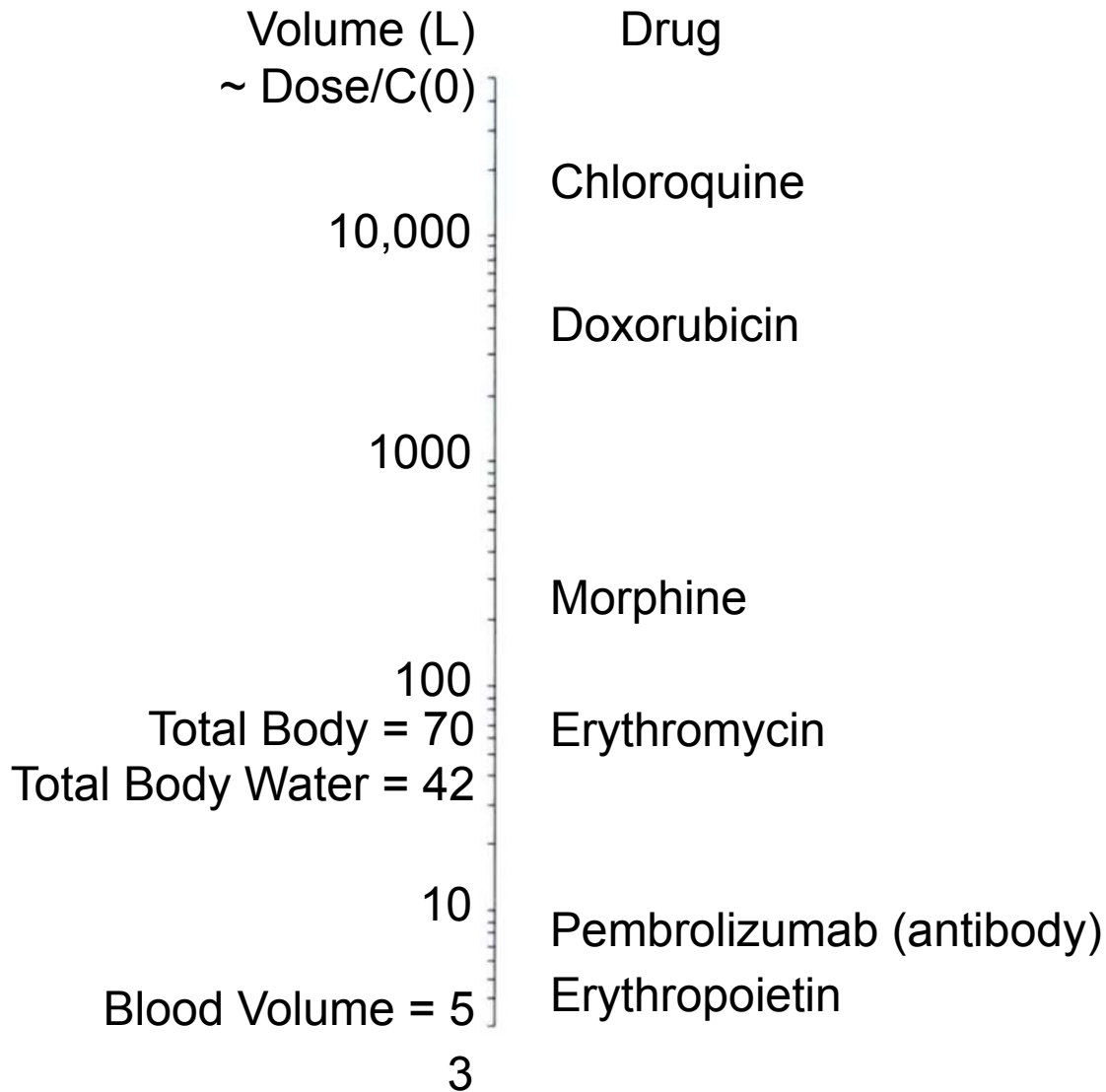


$$\begin{aligned} \text{Dose} &= 1000 \text{ mg} \\ C_0 &= 20 \text{ mg/mL} \\ V &= 50 \text{ mL} \end{aligned}$$

$$\begin{aligned} \text{Dose} &= 1000 \text{ mg} \\ C_0 &= 0.2 \text{ mg/mL} \\ V &= 5000 \text{ mL} \end{aligned}$$



Volumes for different drugs



How can chloroquine have a volume of 10,000L, the size of an X?

- A drug may appear to have a larger volume if
 - It is lipophilic (sticks to fat, instead of water) and distributes to body and is not observed in blood.
 - Accumulates in red blood cells and not present in the plasma sample
- Key lesson: Volume (and all PK parameters) are “apparent” and cannot always be easily related to physiological properties



Key Lessons

- Volume relates amount in body to concentration measured in circulation.
- Volumes are not necessarily physiologically meaningful and can be as large as 10,000 L.

Pharmacokinetics after single intravenous bolus dose

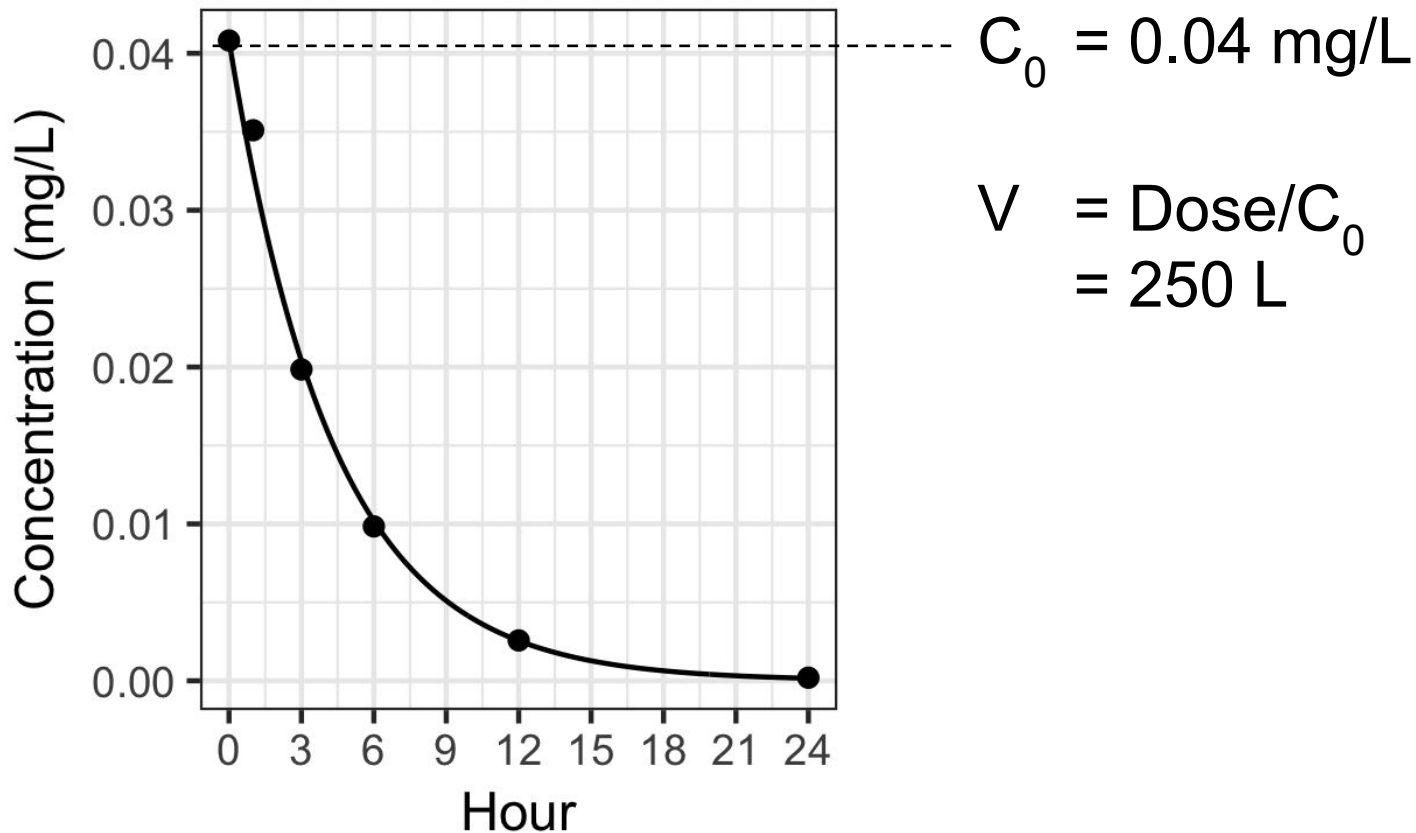
Part 1 – focus on elimination (ignore distribution)

Examples of intravenous drugs

- Chemotherapies (doxorubicin)
- Pain medications (morphine)
- Increase blood pressure (epinephrine)

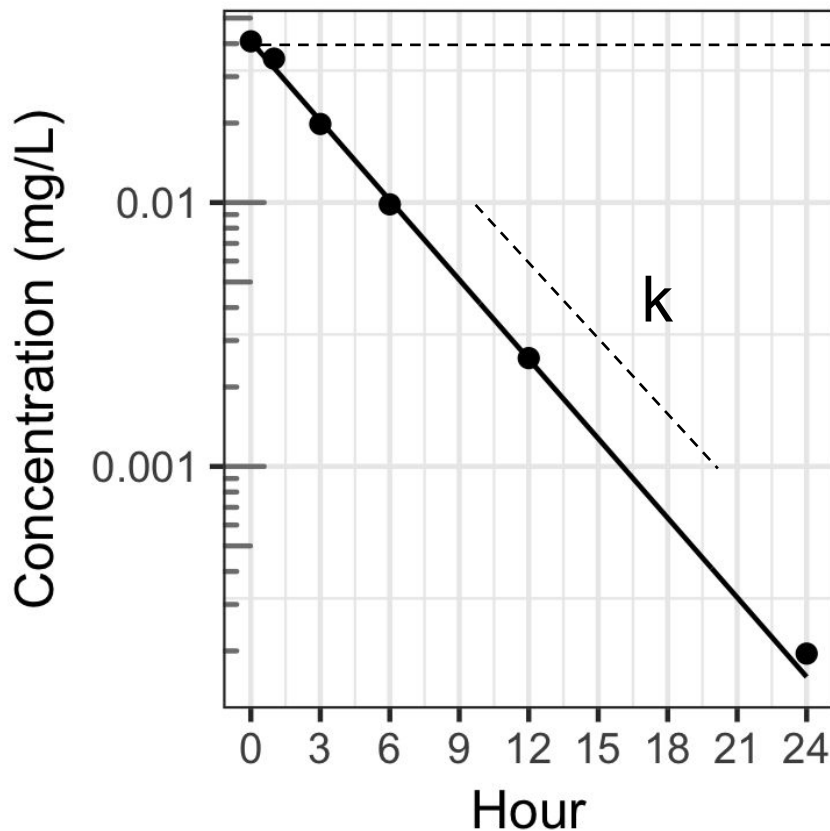
Drug concentration over time

Dose = 10 mg



Drug concentration over time

Log scale



Dose = 10 mg

$C_0 = 0.04$ mg/L

$V = 250$ L

$k = 0.23/\text{h}$

= elimination rate

units = 1/time

$$C(t) = C_0 e^{-kt}$$

$$\begin{aligned} Amt(t) &= V \cdot C(t) \\ &= V \cdot C_0 e^{-kt} \\ &= Dose \cdot e^{-kt} \end{aligned}$$

Half-life definition – how long for half of drug to be eliminated

$$C(t) = C_0 e^{-kt}$$

How long does it take for half the drug to be eliminated?

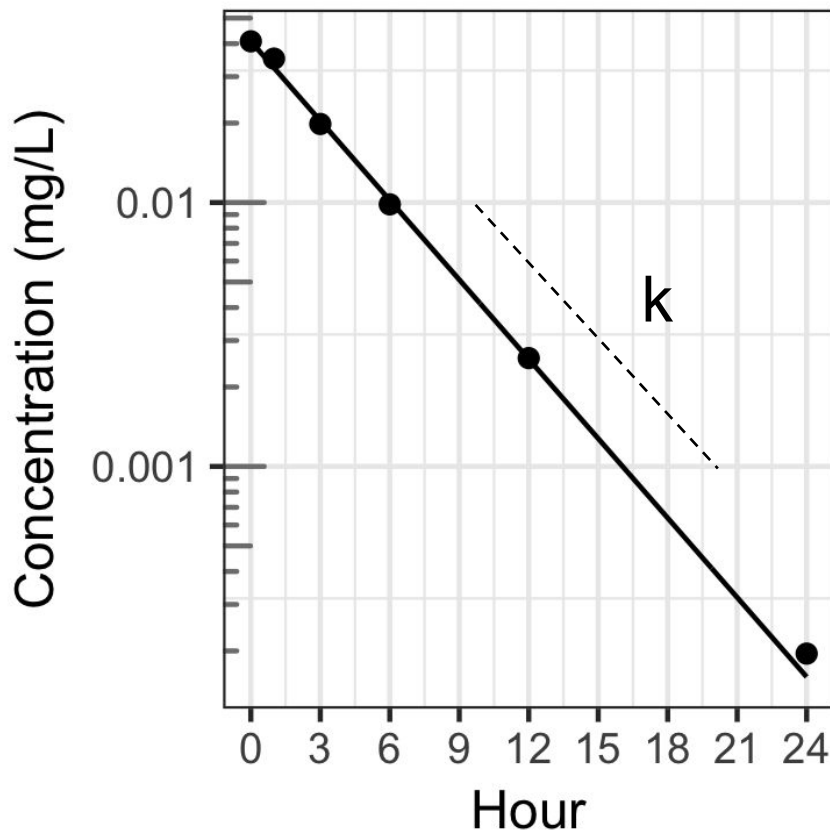
At what time does:

$$\frac{1}{2} \cdot C_0 = C_0 e^{-kt_{1/2}}$$

$$\frac{1}{2} = e^{-kt_{1/2}}$$

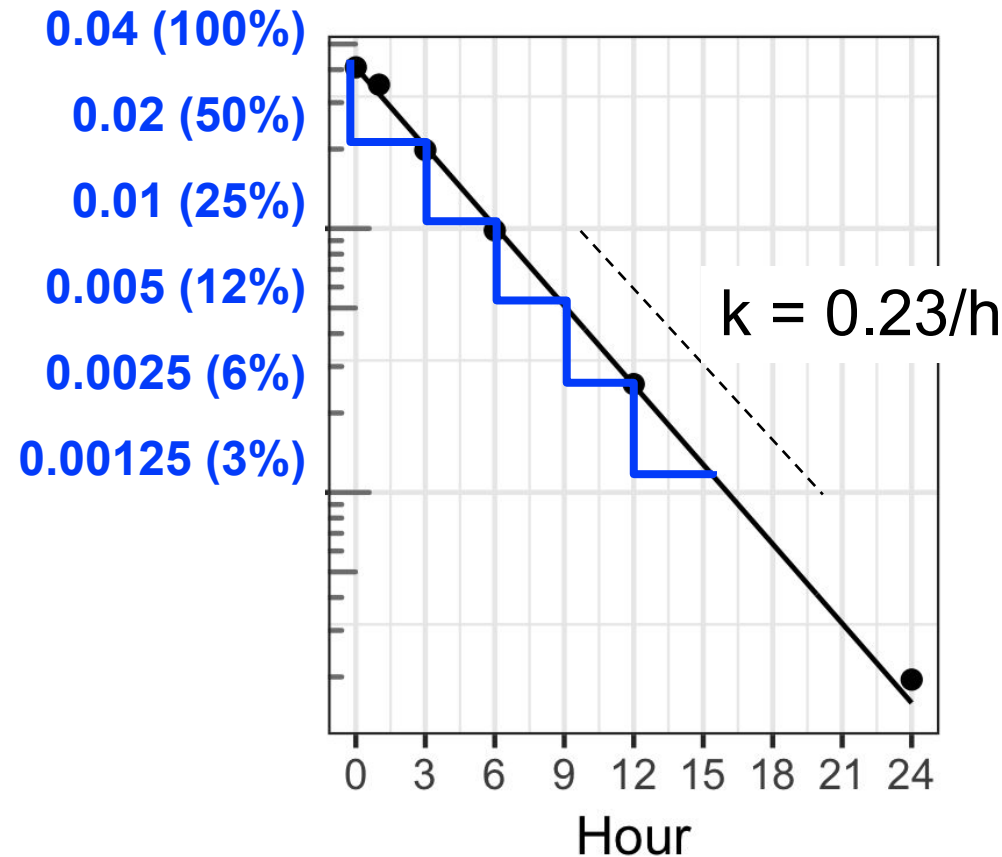
$$\ln(\frac{1}{2}) = -kt_{1/2}$$

$$\boxed{\frac{0.693}{k} = t_{1/2}}$$



Half-life example

$$C(t) = C_0 e^{-kt}$$



$$\begin{aligned} t_{1/2} &= \frac{0.693}{k} \\ &= \frac{0.693}{0.23/h} \\ &= 3 \text{ h} \end{aligned}$$

Every 3 hours,
concentration declines by half

The shorter the terminal half-life, the more frequently the drug is dosed

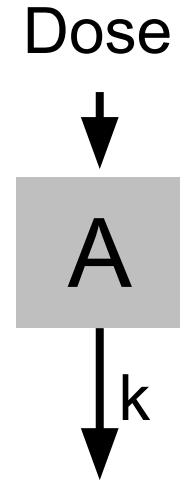
Name	Half-life	Dose Frequency
Tylenol	3 hours	4 per day
Aleve	14 hours	2 per day
Keytruda	25 days	1 per 3 weeks

Dosing interval also depends on duration of effect

SEE QUIZ QUESTIONS

Compartmental Model

Concentration (mg/L): $C(t) = C_0 \cdot e^{-kt}$
Amount (mg): $A(t) = Dose \cdot e^{-kt}$



Rate of change of
amount in body

$$\frac{dA}{dt} = -k \cdot A$$

Mathematical introduction to Clearance [L/h]

$$\frac{dA}{dt} = -k \cdot A$$

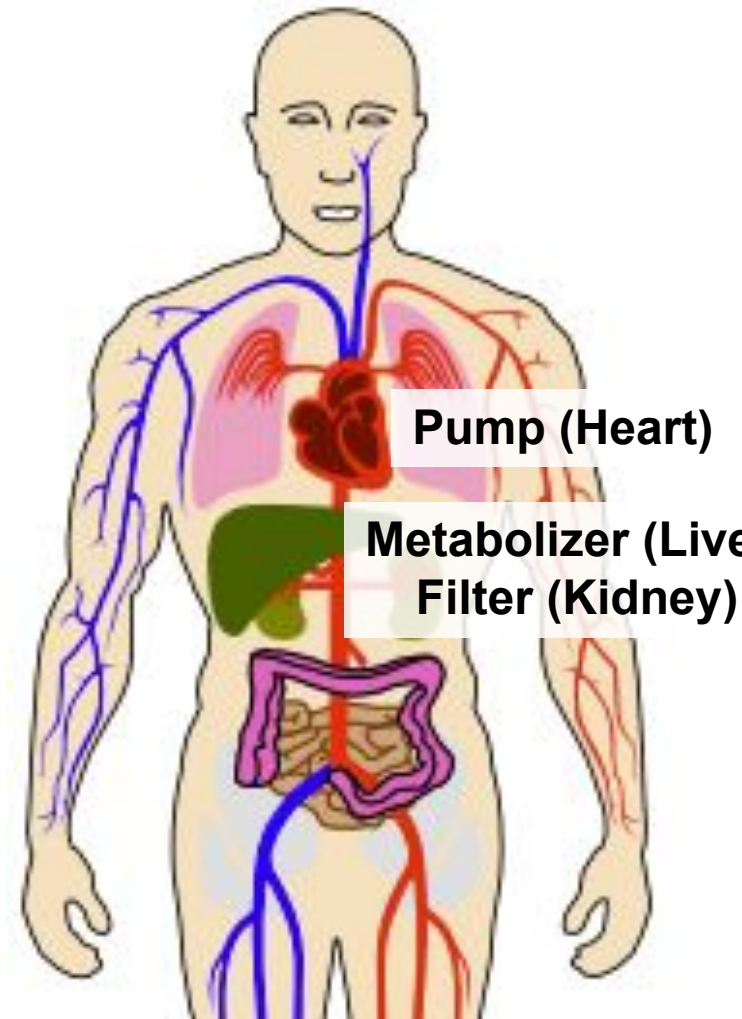
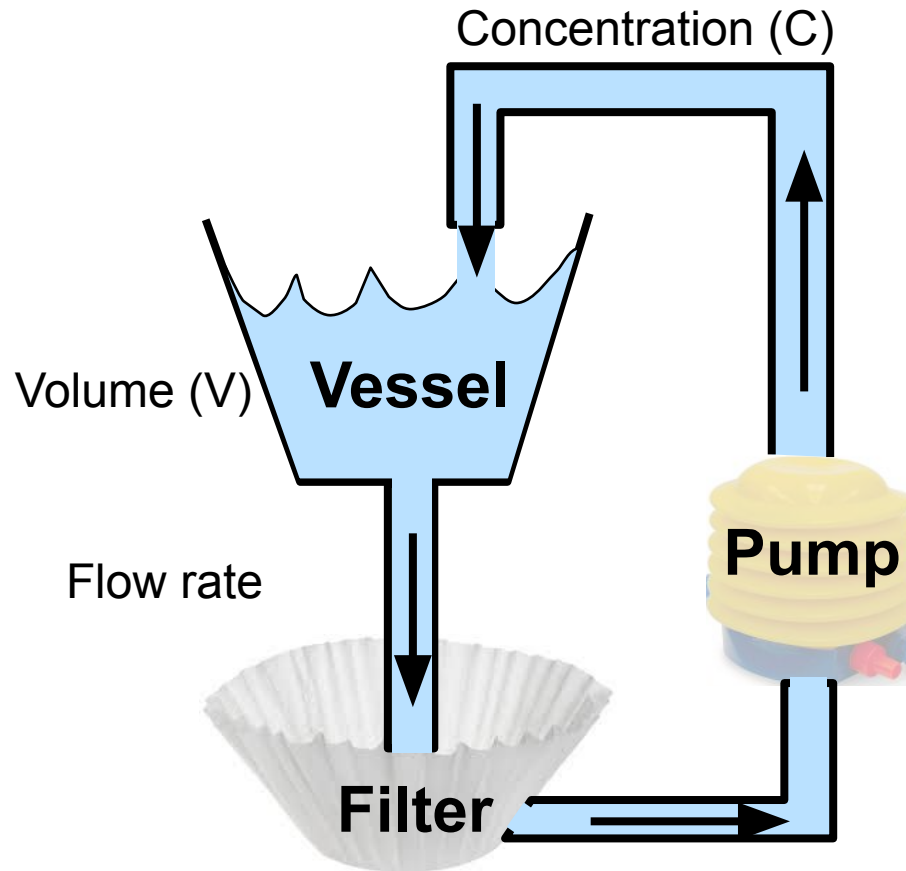
$$\frac{dA}{dt} = -(k \cdot V) \cdot \left(\frac{A}{V}\right)$$

$$\frac{dA}{dt} = -CL \cdot C$$

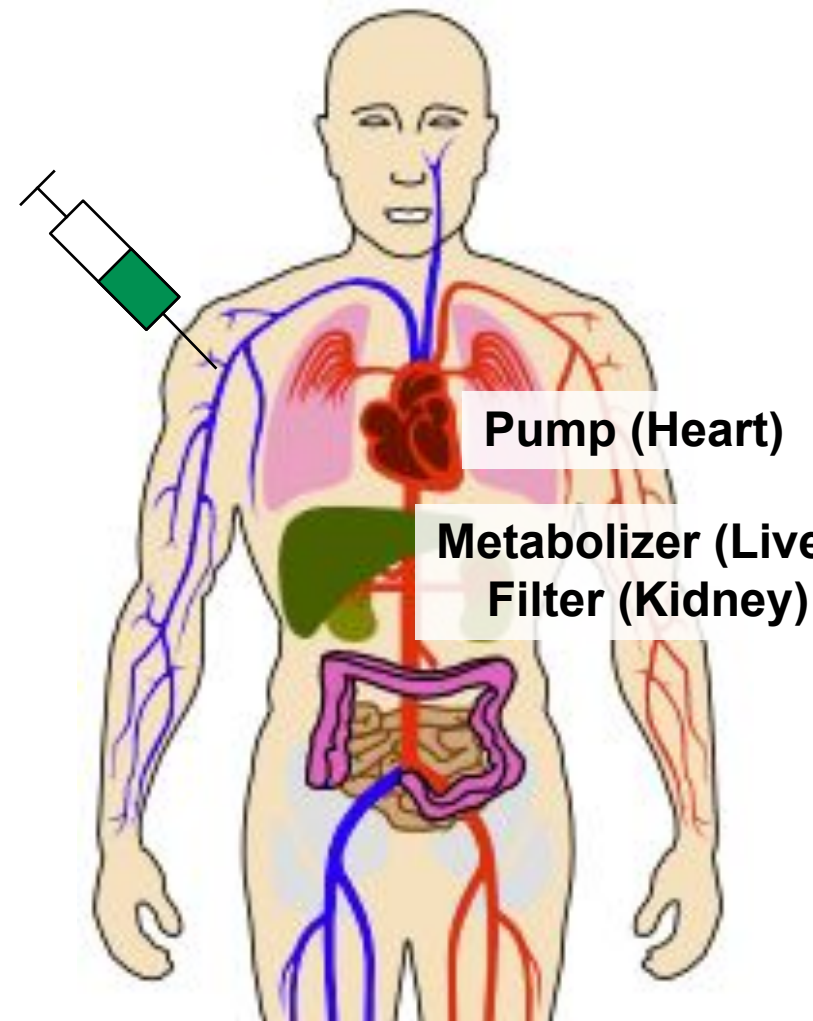
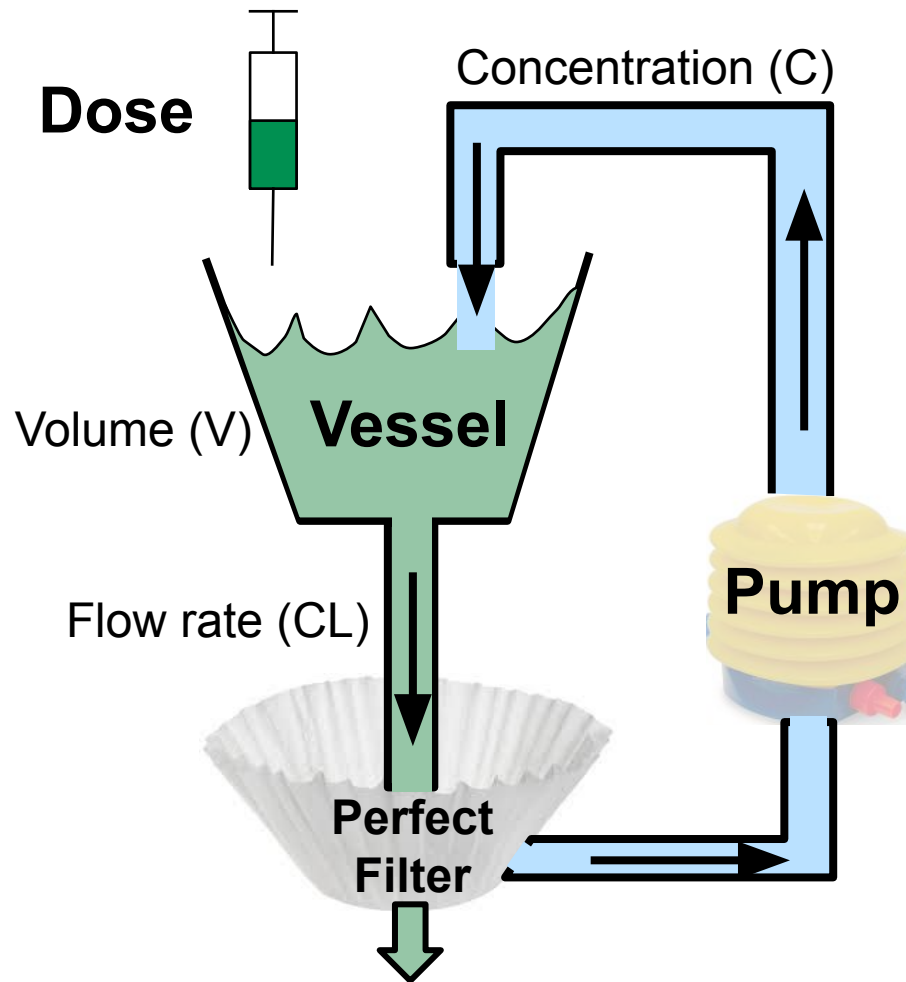
$$\frac{mg}{L} = \frac{L}{h} \cdot \frac{mg}{L}$$

Clearance is a flow rate of plasma that is completely eliminated of drug

Mechanical Analogy



Mechanical Analogy



If filter eliminates all drug that passes through, then CL is the flow rate

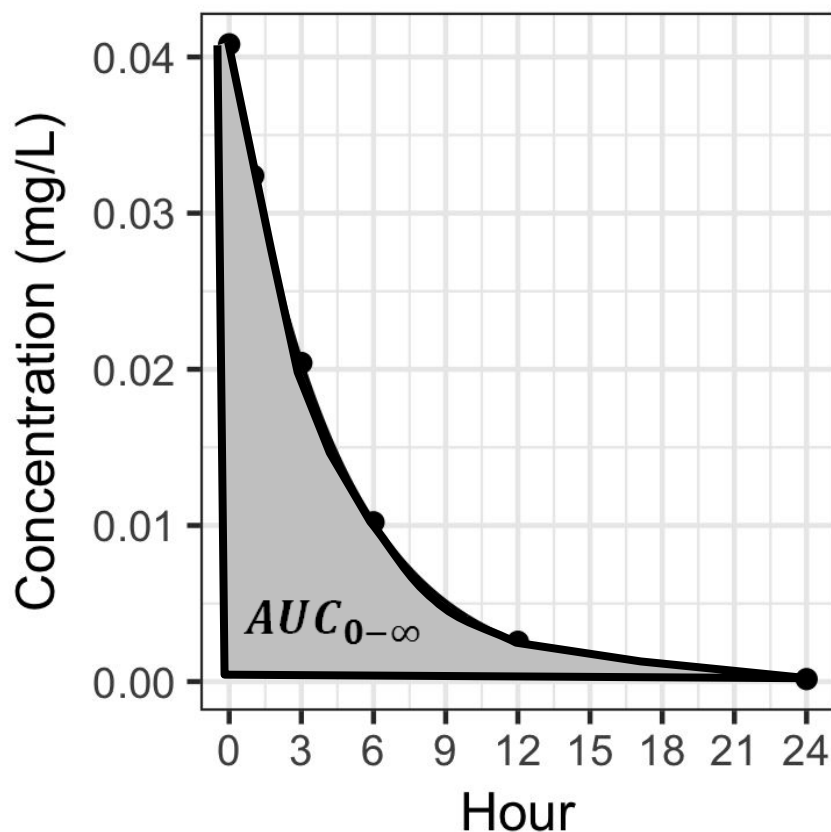
$$\frac{dAmt}{dt} = -CL \cdot C$$

Clearance is the most important PK parameter

Clearance is helpful in understanding the average concentration at steady state

- After sufficient time under the same dosing regimen, one reaches “steady state”, where
 - $\text{Rate In} = \text{Rate Out} = \text{CL} \cdot C$
- Let's say:
 - You want to maintain concentration $\sim 10 \text{ mg/L}$
 - You know that $\text{CL} = 3 \text{ L/h}$
- Then:
 - $\text{Rate Out} = (3 \text{ L/h}) \cdot (10 \text{ mg/L}) = 30 \text{ mg/h}$
- The maintenance dose (Rate In) is 30 mg/h .

Clearance relates to the Area Under the conc. Curve ($AUC_{0-\infty}$)



Total drug in = Total drug out

$$\text{Dose} = \int_0^{\infty} CL \cdot C(t) dt$$

If clearance does not depend on concentration (linear)

$$\text{Dose} = CL \cdot \int_0^{\infty} C(t) dt$$

$$\text{Dose} = CL \cdot AUC_{0-\infty}$$

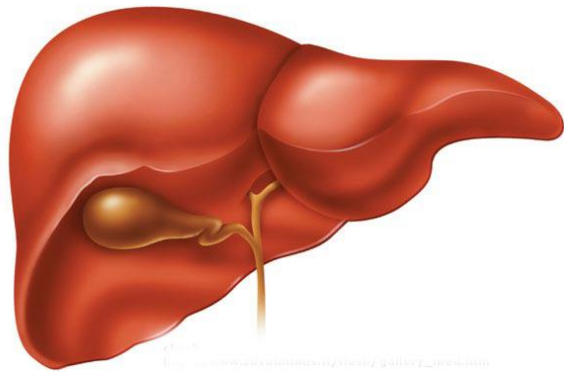
$$AUC_{0-\infty} = \frac{\text{Dose}}{CL}$$

Formula doesn't depend on specific model for $C(t)$, Volume or half-life. It only requires linear clearance

Major Sites of Elimination

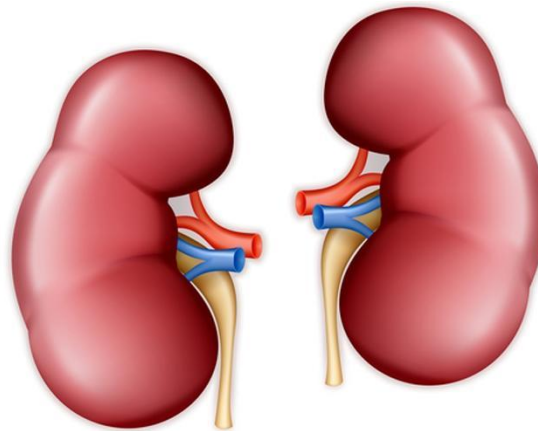
Small Molecules

Liver



Mainly metabolism

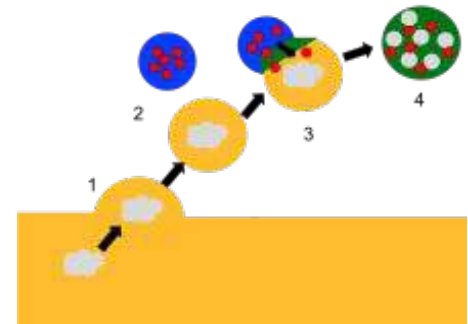
Kidneys



Mainly excretion
(urine)

Biologics

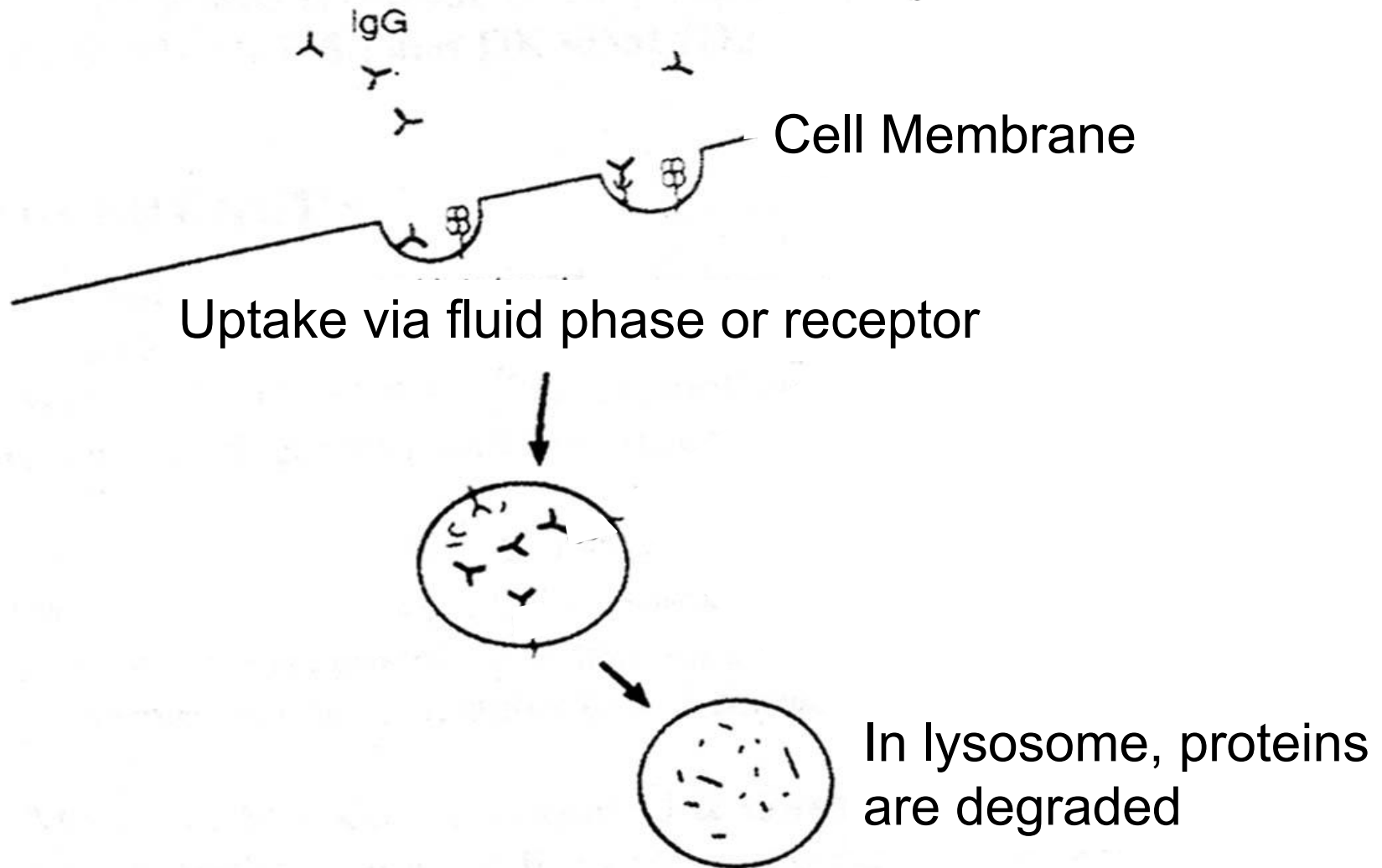
Lysosome



All cells

Proteolysis
(in cells)

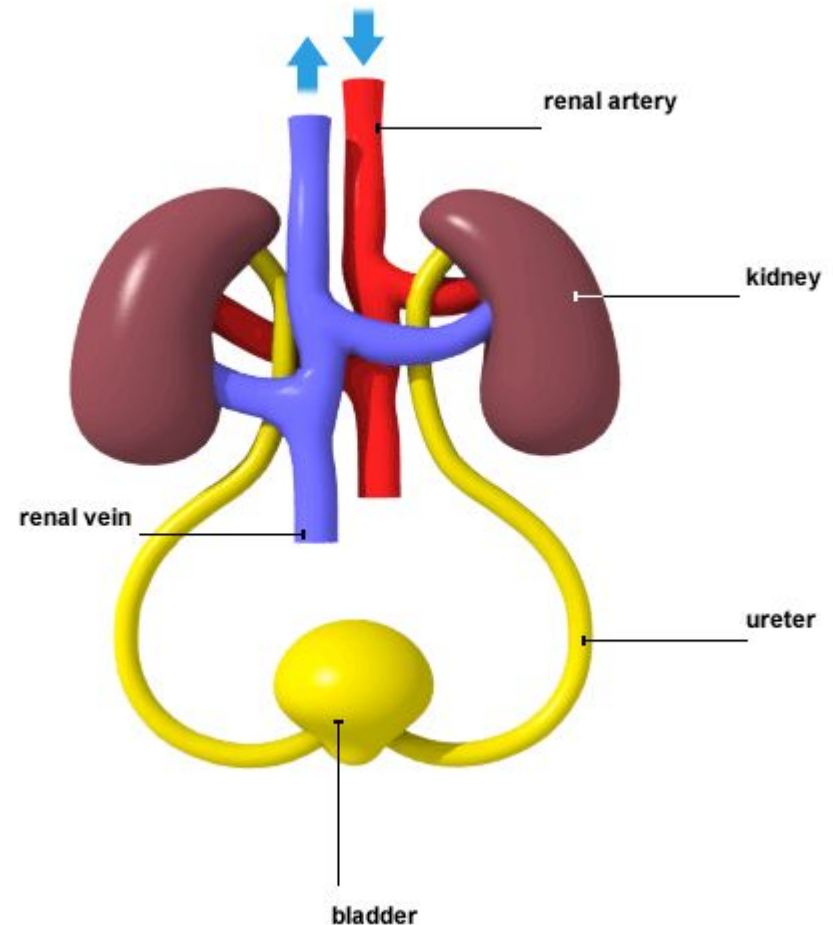
Proteins in general are eliminated through lysosomal degradation



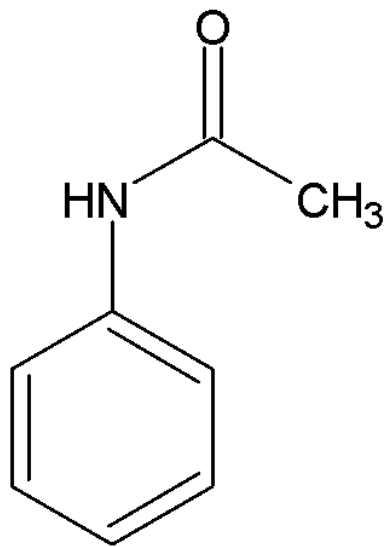
This process can occur in many tissues. Endothelial cells is one major location

Function of Kidneys

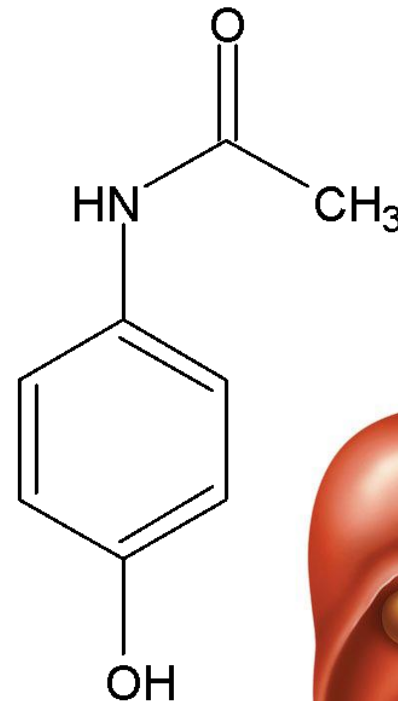
- “Cleans the blood”
 - Filter the blood and remove endogenous metabolic waste, such as urea, uric acid, and creatinine
 - Remove foreign substances
- Regulate body water content, hormones, mineral composition, and acidity
- Can also metabolize drugs (glucuronidation)



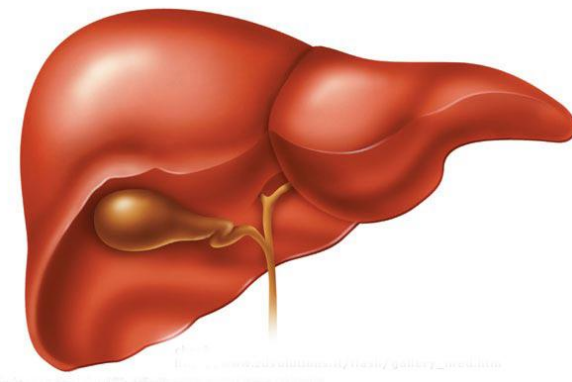
Phase 1 Metabolism: add small polar groups. Hydroxylation



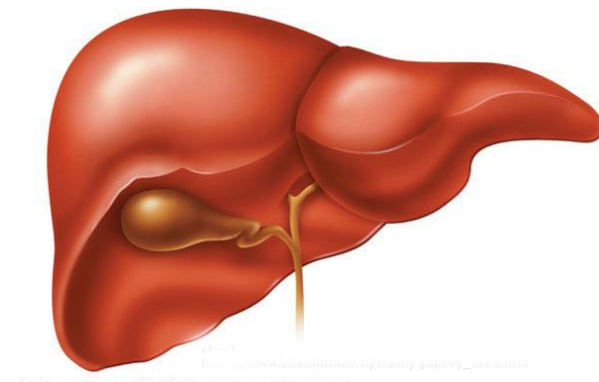
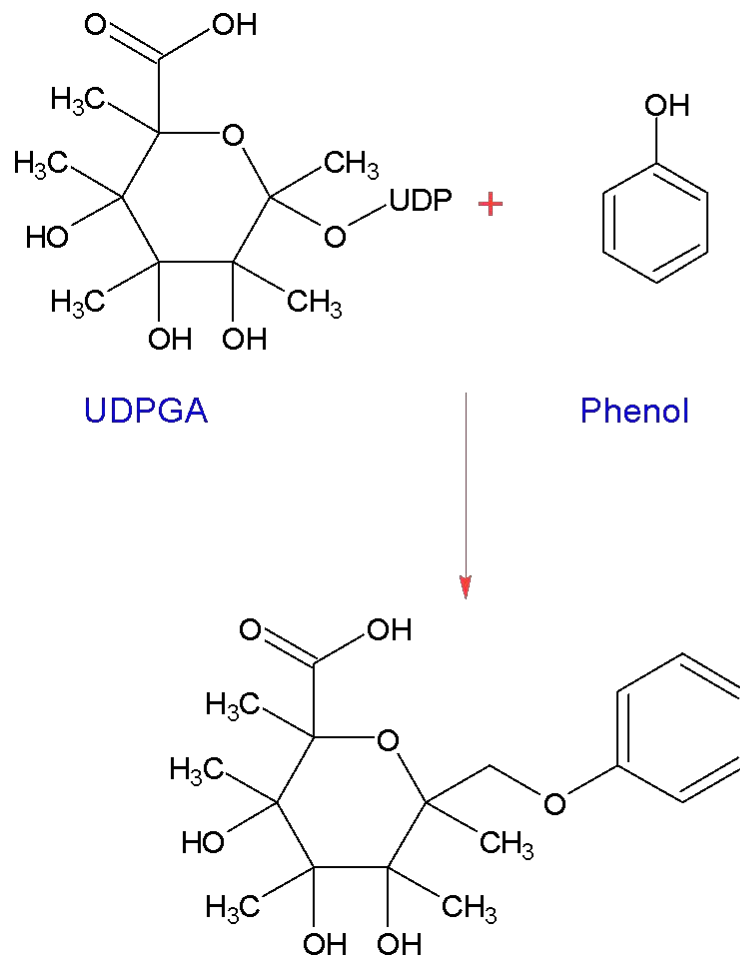
Acetanilid



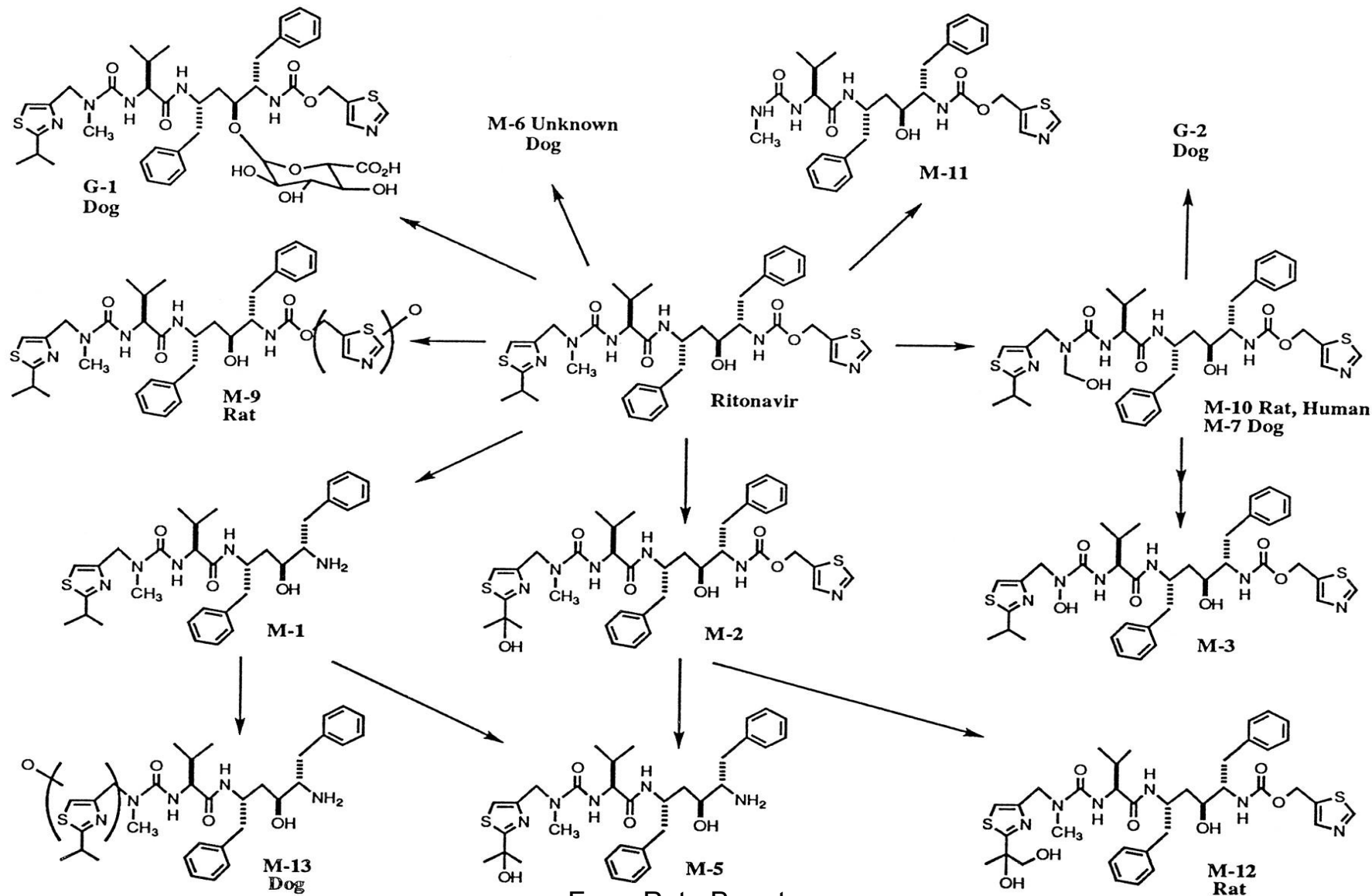
p-hydroxyacetanalid



Phase 2 Metabolism: add larger polar molecules



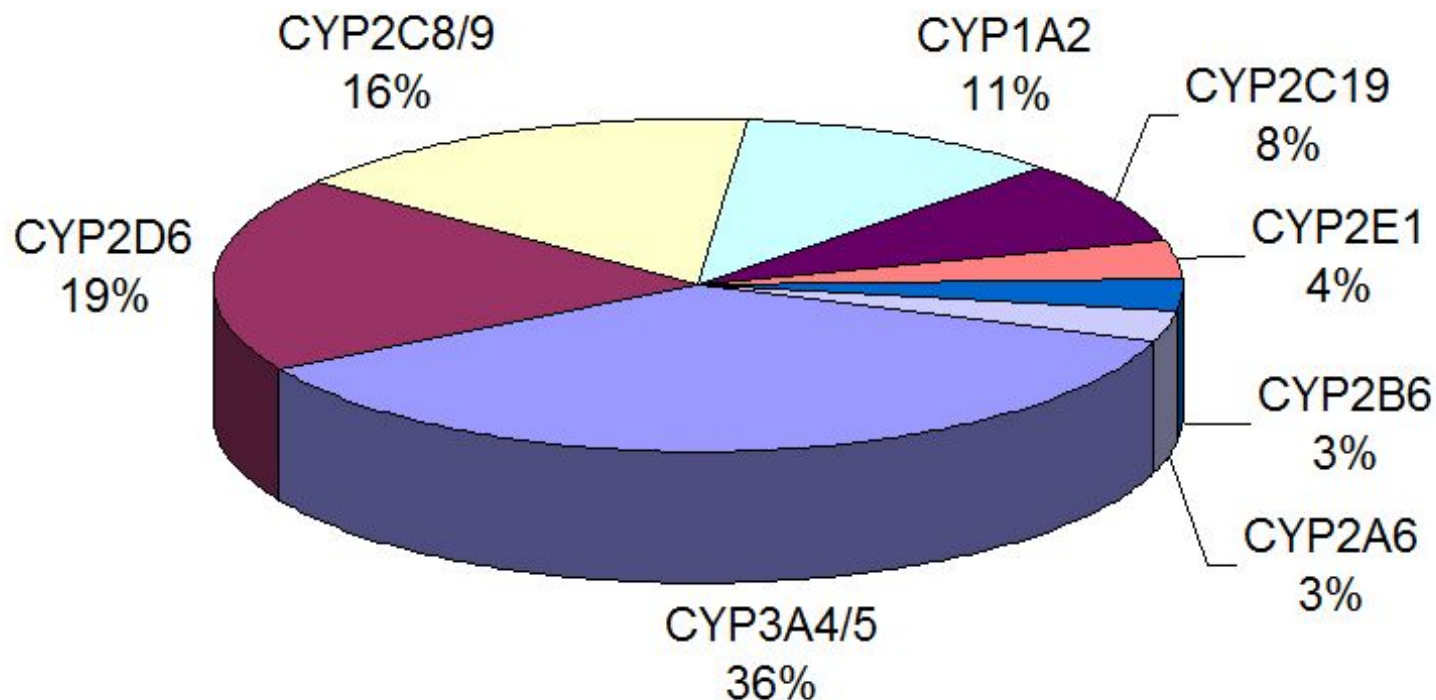
Metabolic Pathways Can Be Complex and Consist of Both Phase 1 and Phase 2



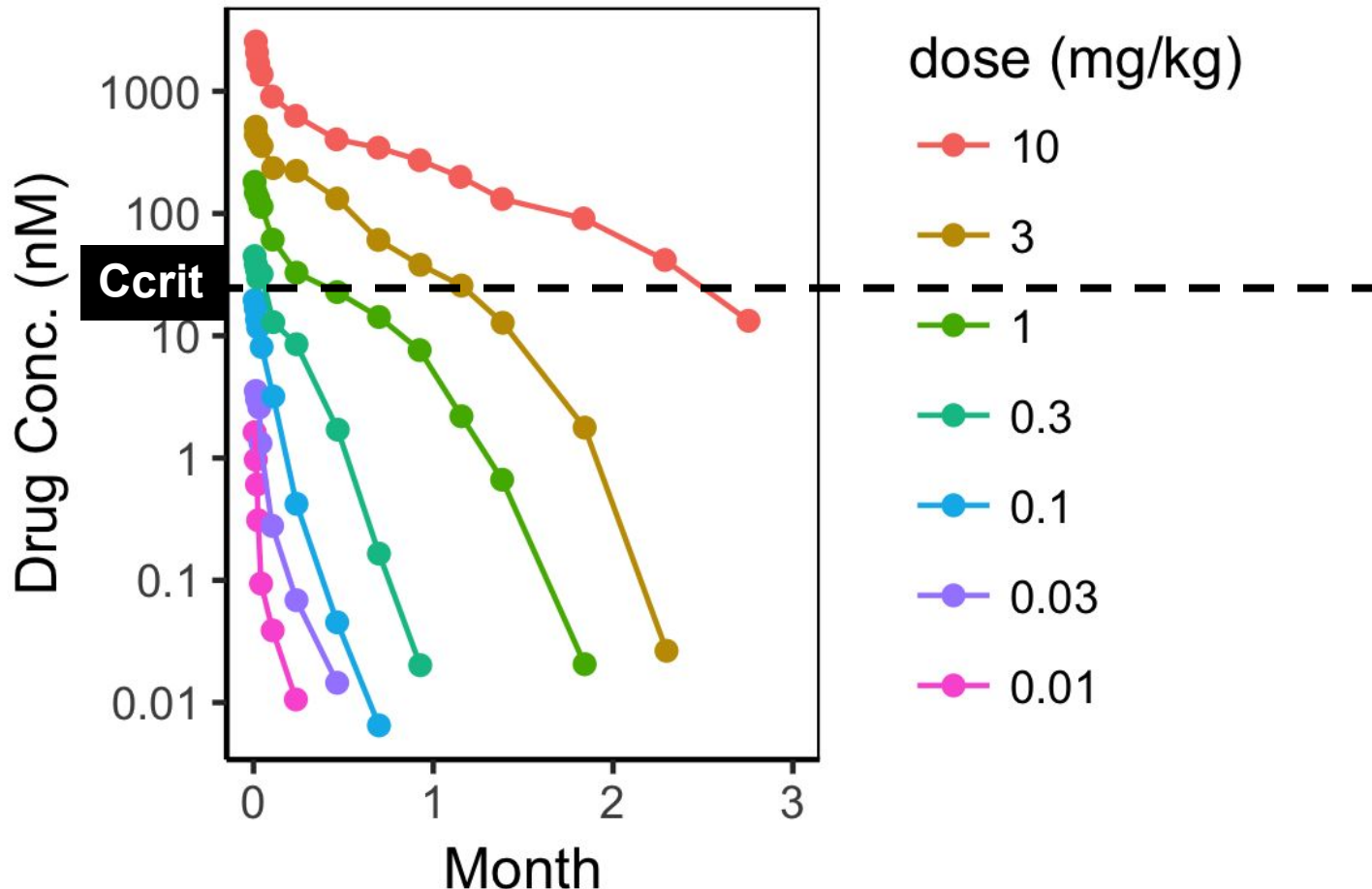
From Pete Bonate

Cytochrome P450 (CYP) metabolizes drug

- Catalyze most Phase I biotransformations
- Found in every species and every tissue
 - In particular in the liver, kidney, GI tract, and brain



Nonlinear pharmacokinetics occurs at “critical concentration” = C_{crit}



Burmester, G. R. et al. Mavrilimumab, a human monoclonal antibody targeting gm-csf receptor- α , in subjects with rheumatoid arthritis: a randomised, double-blind, placebo- controlled, phase I first-in-human study. *Annals of the rheumatic diseases* 70, 1542–1549 (2011).

If route of elimination saturates, elimination is reduced

$$\frac{dA}{dt} = -CL \cdot C - \underbrace{\frac{V_{max} \cdot C}{K_m + C}}$$

At small
concentrations,

$$\begin{aligned}\frac{dA}{dt} &= -CL \cdot C - \underbrace{\frac{V_{max} \cdot C}{K_m}} \\ &= \left(-CL - \frac{V_{max}}{K_m}\right) C\end{aligned}$$

At large
concentrations,

$$\begin{aligned}\frac{dA}{dt} &= -CL \cdot C - \underbrace{V_{max}} \\ &\approx -CL \cdot C\end{aligned}$$

Faster elimination at lower concentrations

“Derivation” for C_{crit}

$$\frac{dA}{dt} = -CL \cdot C - \frac{V_{\text{max}}C}{C + K_m};$$

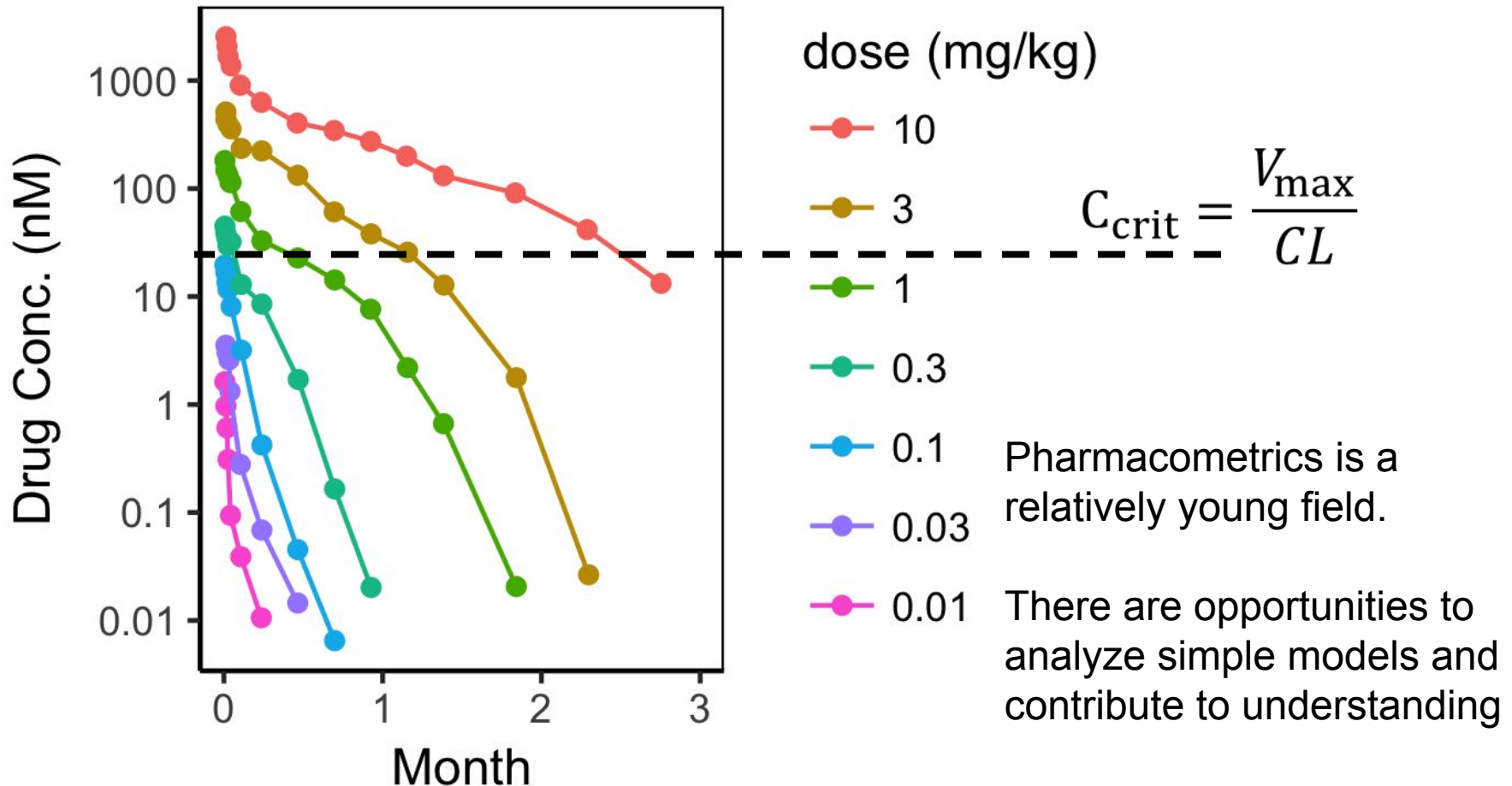
For large doses (and concentrations), $C \gg K_m$

$$\frac{dA}{dt} \approx -CL \cdot C - V_{\text{max}}$$

Define C_{crit} to be where the linear ($CL \cdot C$) and nonlinear (V_m) components contribute equally to total elimination

$$CL \cdot C_{\text{crit}} = V_{\text{max}} \rightarrow \boxed{C_{\text{crit}} = \frac{V_{\text{max}}}{CL}}$$

Nonlinear pharmacokinetics occurs at “critical concentration” = C_{crit}



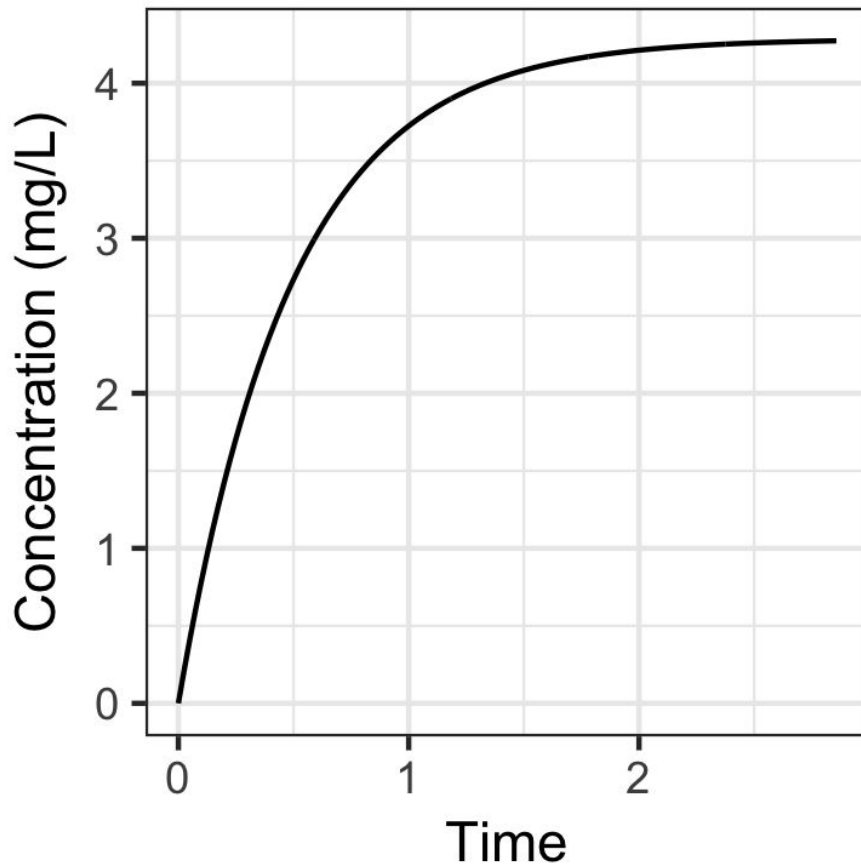
SEE QUIZ QUESTIONS

Key Lessons

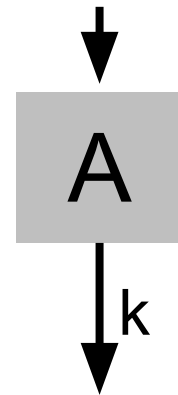
- Clearance tells you the average concentration at steady state (given an input dosing rate)
 - $\text{Rate In} = \text{Rate Out} = \text{CL} \cdot C$
- Small molecules are eliminated mainly by the liver and the kidneys.
- Large molecules (proteins) are eliminated mainly by endocytosis and proteolysis.

Continuous Dosing: Infusion

Continuous infusion

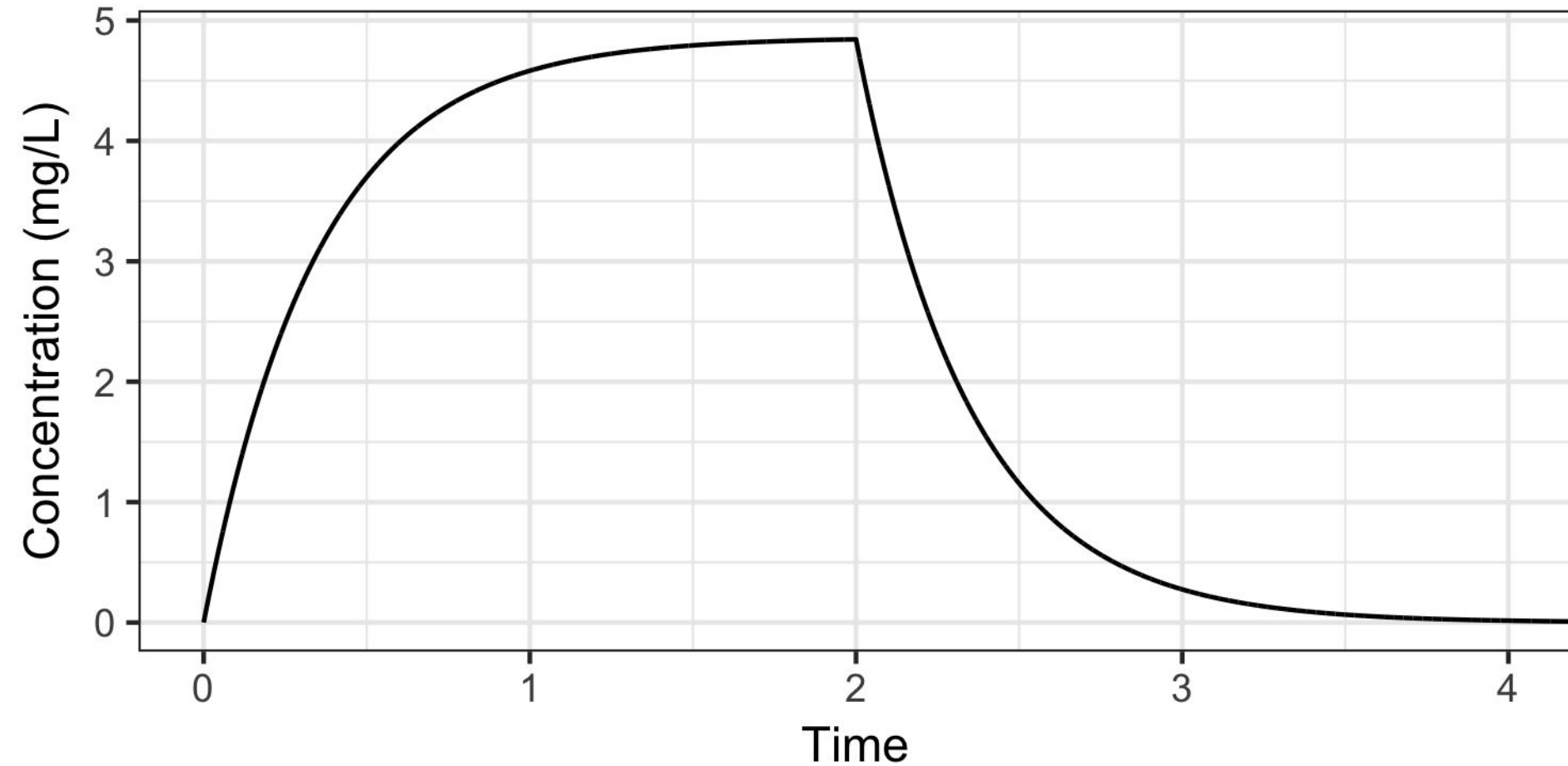


Dose Rate (R_0 , mg/h)

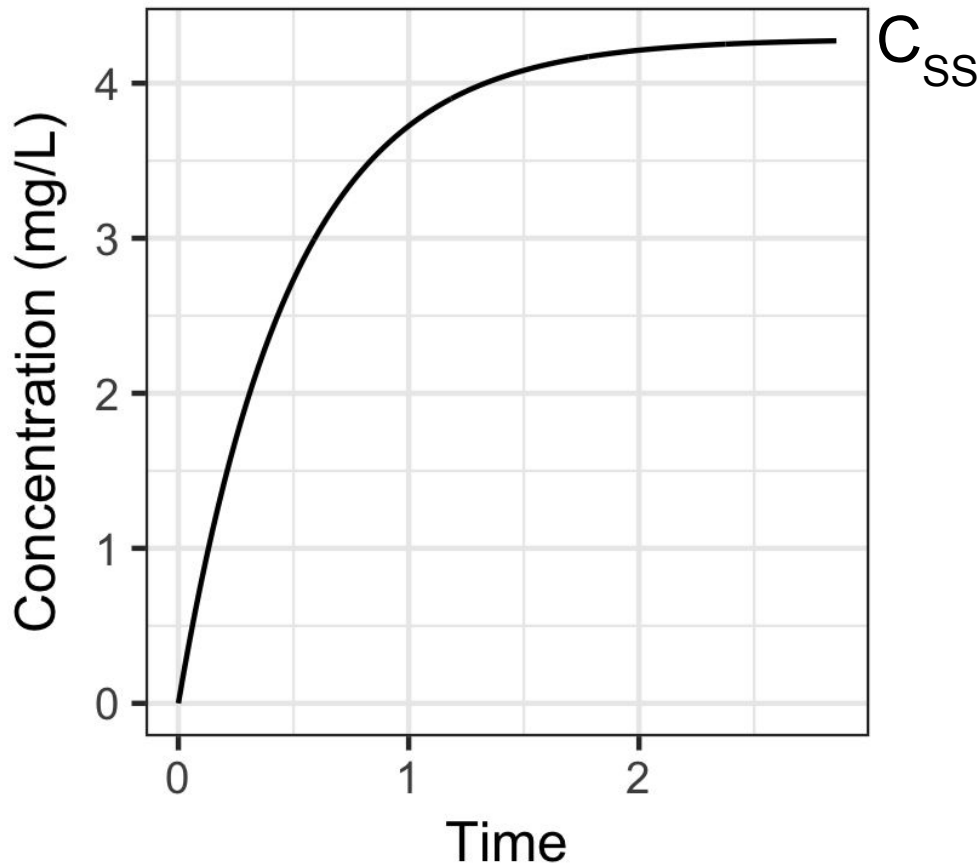


$$\frac{dA}{dt} = R_0 - k \cdot A$$

Continuous infusion



Continuous infusion



$$\frac{dA}{dt} = R_0 - k \cdot A$$

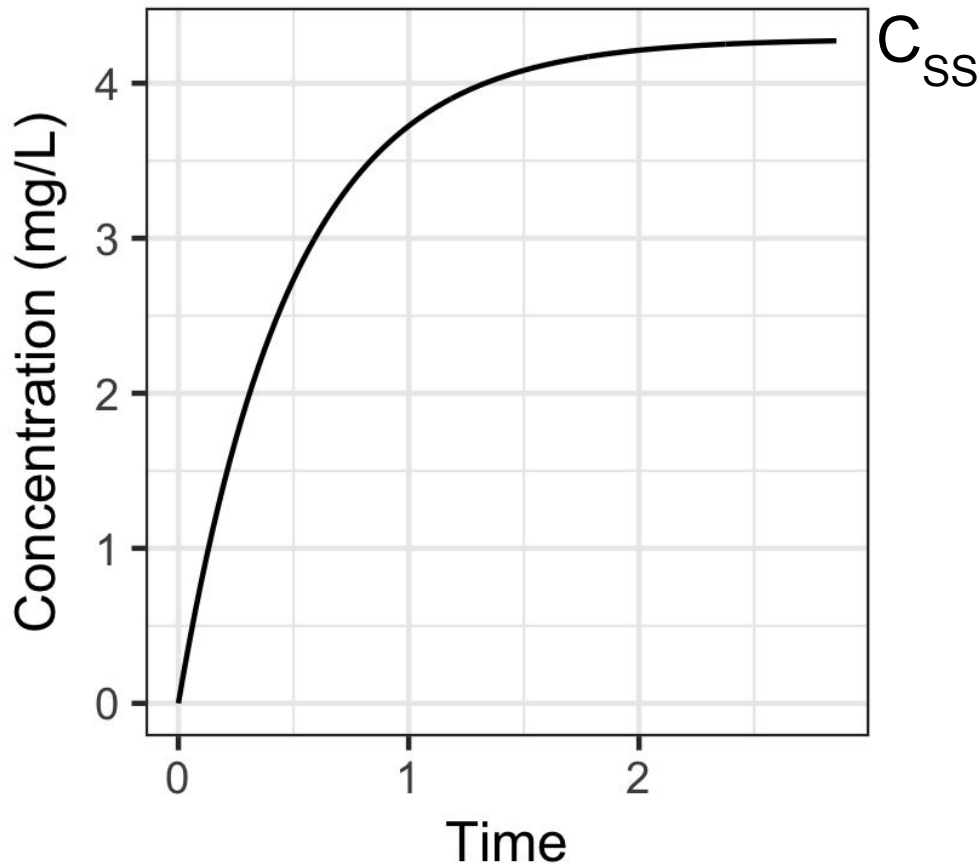
At steady state, $\frac{dA}{dt} = 0$

$$0 = R_0 - k \cdot A_{ss}$$

$$A_{ss} = \frac{R_0}{k}$$

$$C_{ss} = \frac{A_{ss}}{V} = \frac{R_0}{k \cdot V} = \frac{R_0}{CL}$$

Continuous infusion



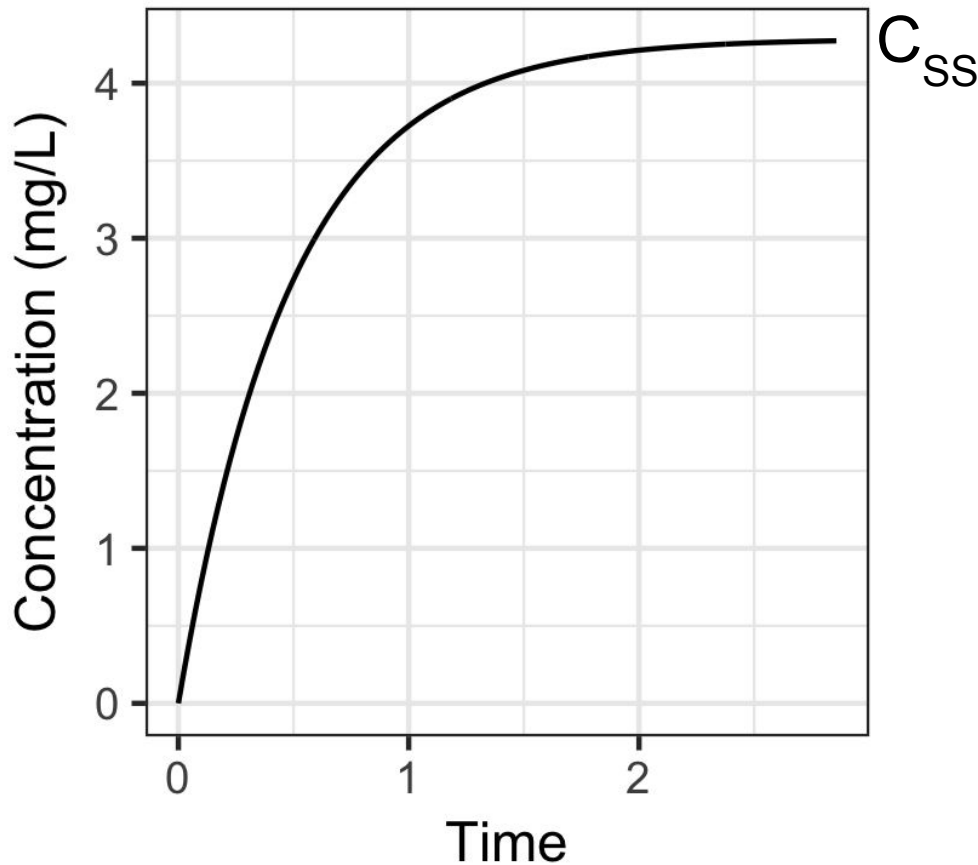
$$\frac{dA}{dt} = R_0 - k \cdot A$$

$$A_{ss} = \frac{R_0}{k}, \quad C_{ss} = \frac{R_0}{CL}$$

$$A(t) = A_{ss}(1 - e^{-kt})$$

$$C(t) = C_{ss}(1 - e^{-kt})$$

At what time do you reach steady state?



$$C(t) = C_{ss}(1 - e^{-kt})$$

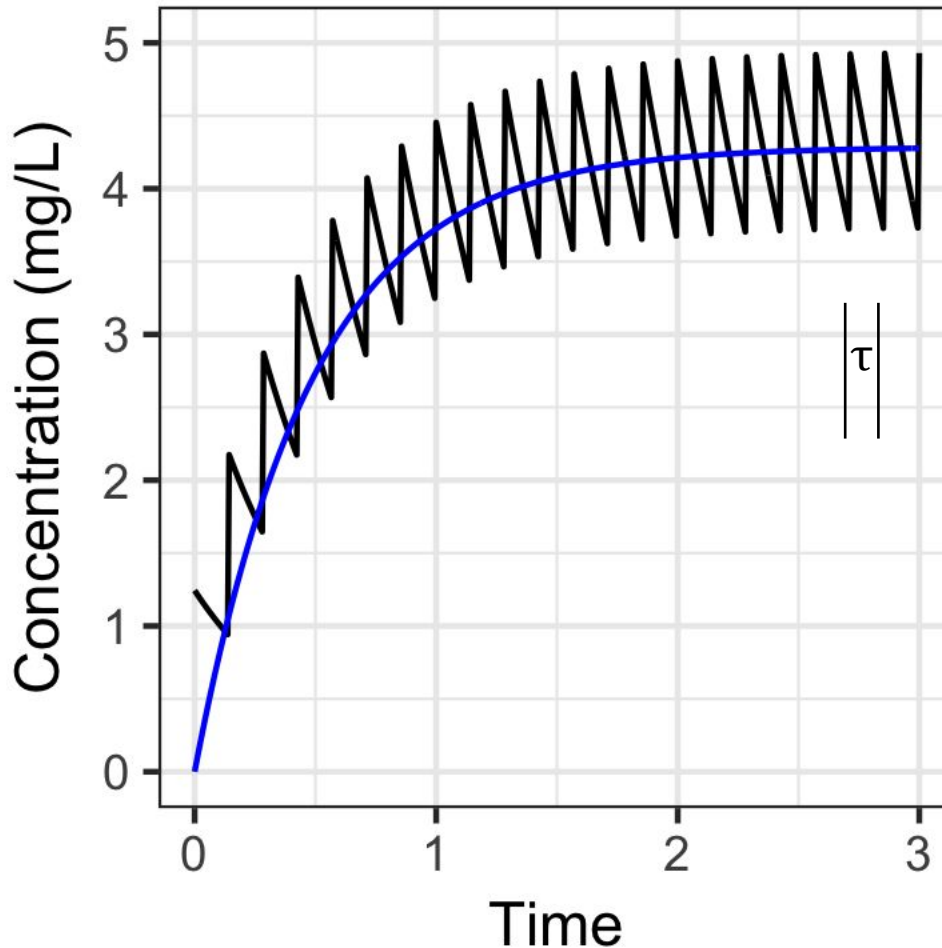
Key Lesson: Sensitivity

- If you double the infusion rate, you double the steady state drug concentration
- If a patient has reduced clearance (e.g. due to liver impairment for a drug metabolized in liver) that reduces CL, then the steady state drug concentration is reduced.

$$C_{ss} = \frac{R_0}{CL}$$

Repeated Dosing - Bolus

Repeated dosing



Similar to infusion dose

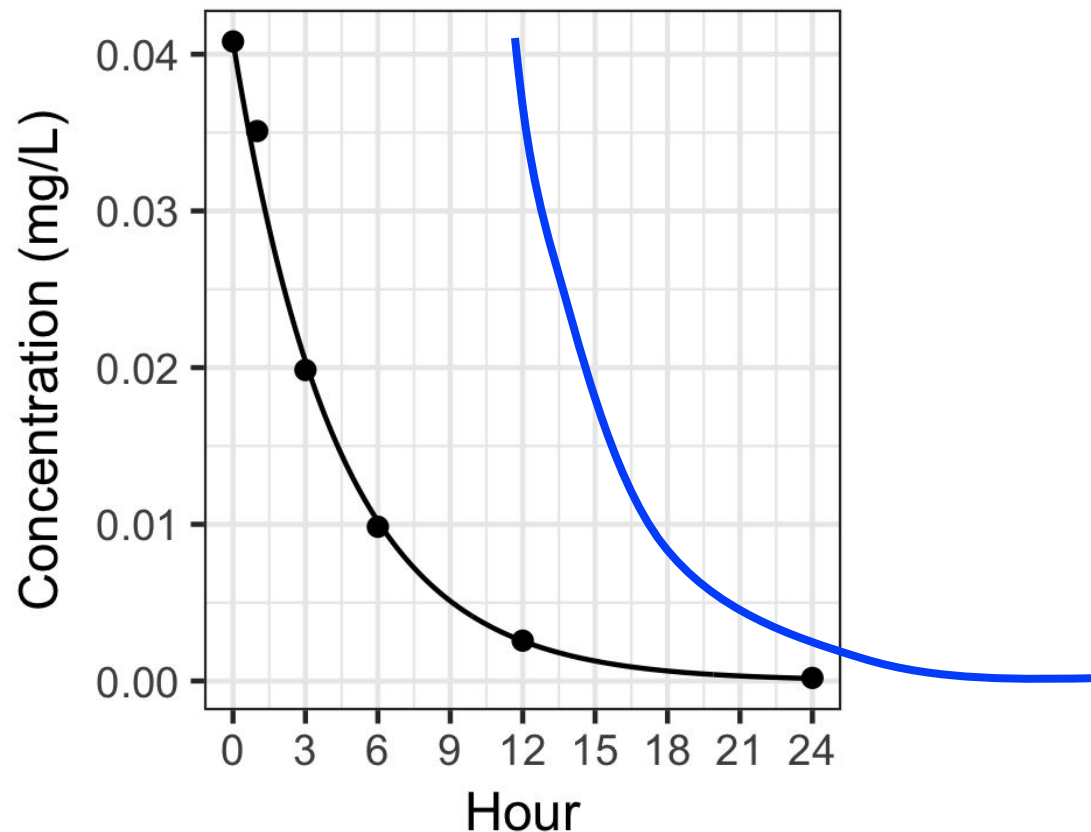
Define τ to be the dosing interval

Recall formula for single bolus dose and amend for dose at another time

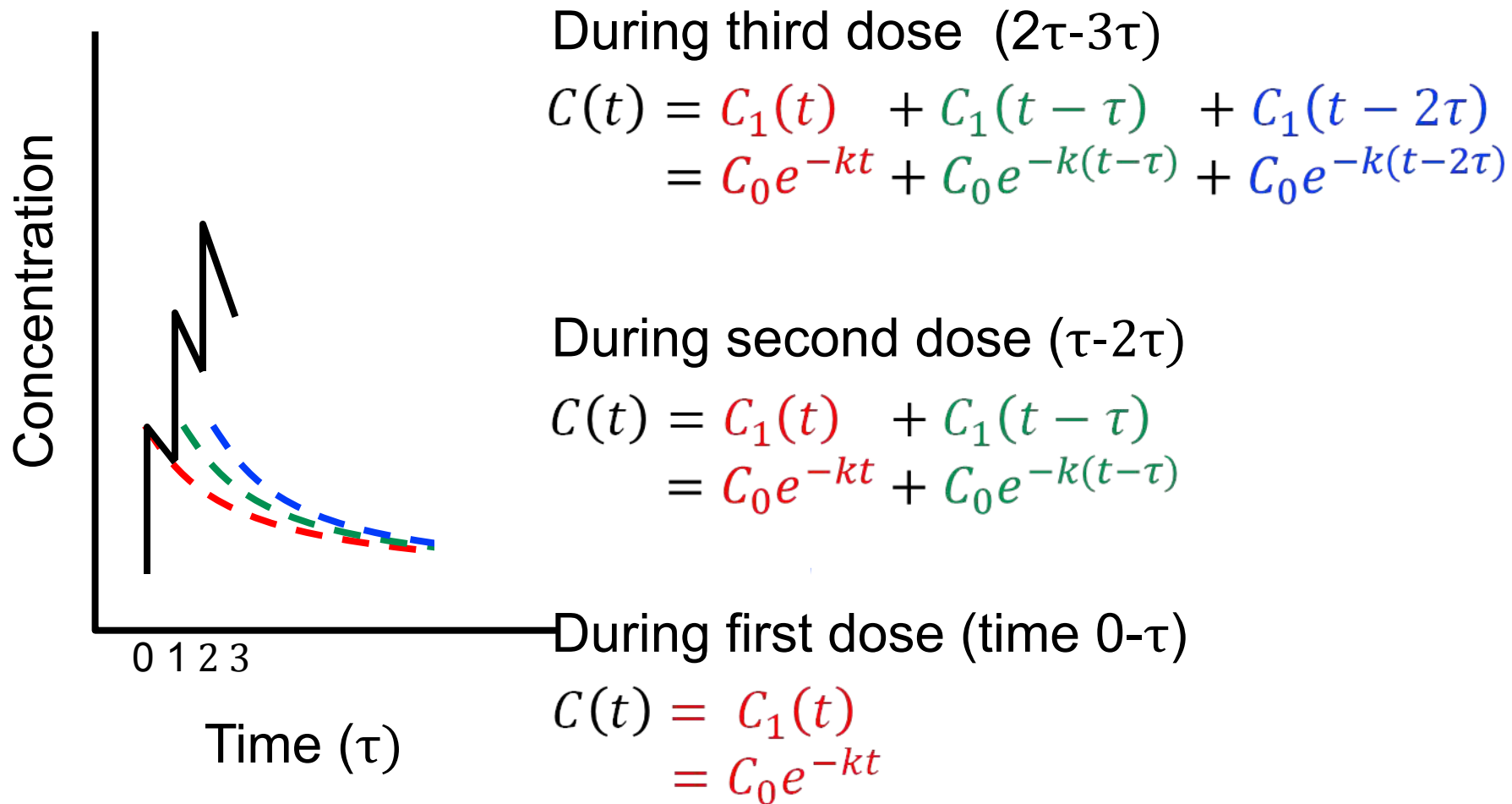
C_1 is the response of a single dose at time 0

$$C_1(t) = C_0 e^{-kt}$$

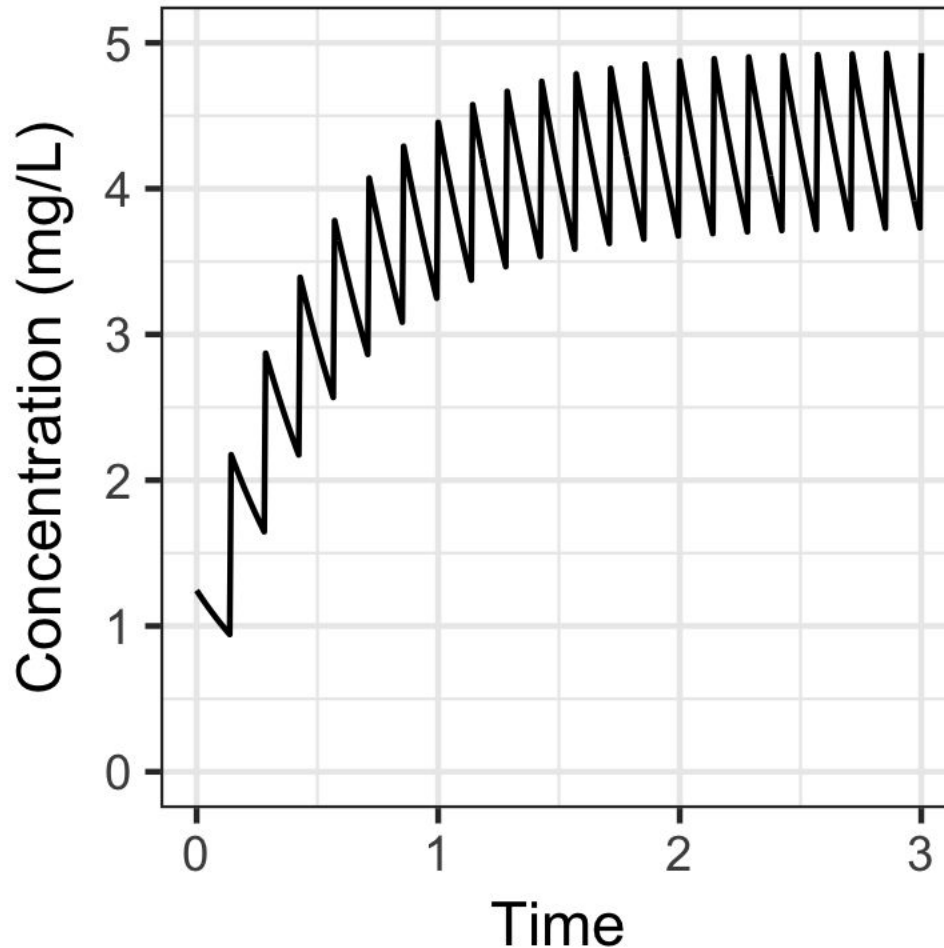
$$C_1(t - 12) = C_0 e^{-k(t-12)}$$



Each dose contributes one “bolus dose” term



The general formula for N doses

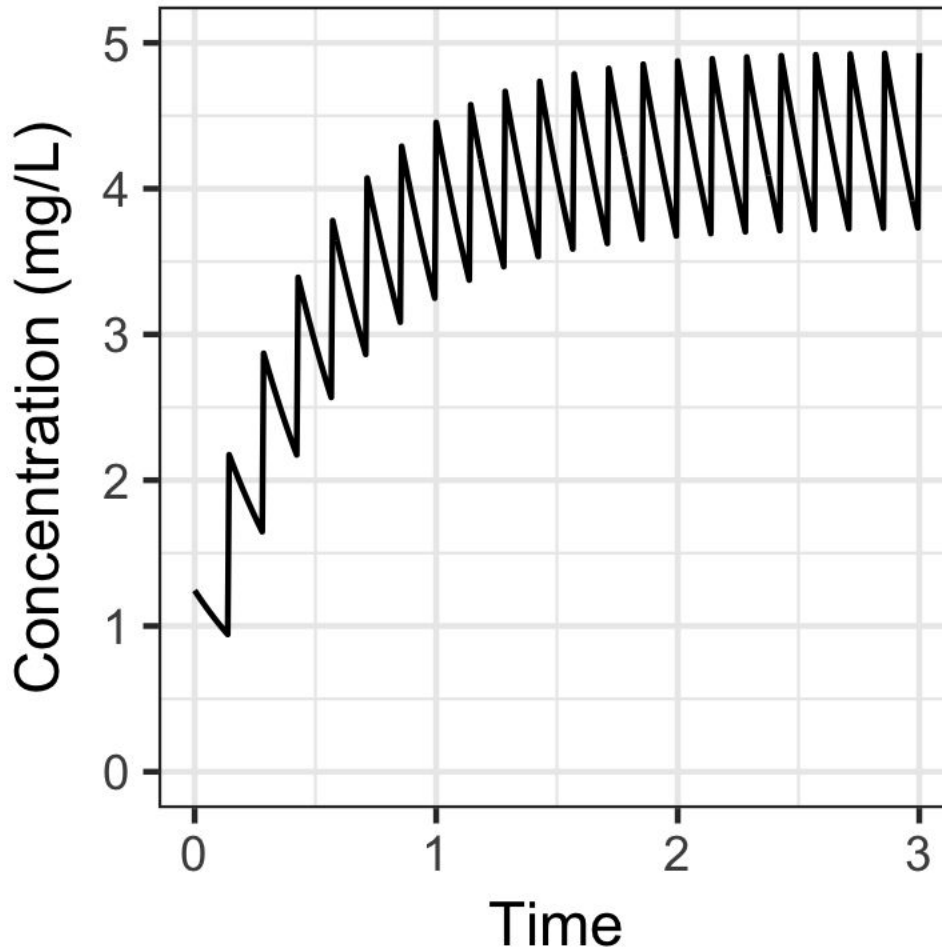


$$C_1(t) = C_0 e^{-kt}$$

$$C(t) = \sum_{n=0}^{N-1} C_1(t - n\tau)$$

$$C(t) = \sum_{n=0}^{N-1} C_0 e^{-k(t-n\tau)}$$

This formula is a geometric series

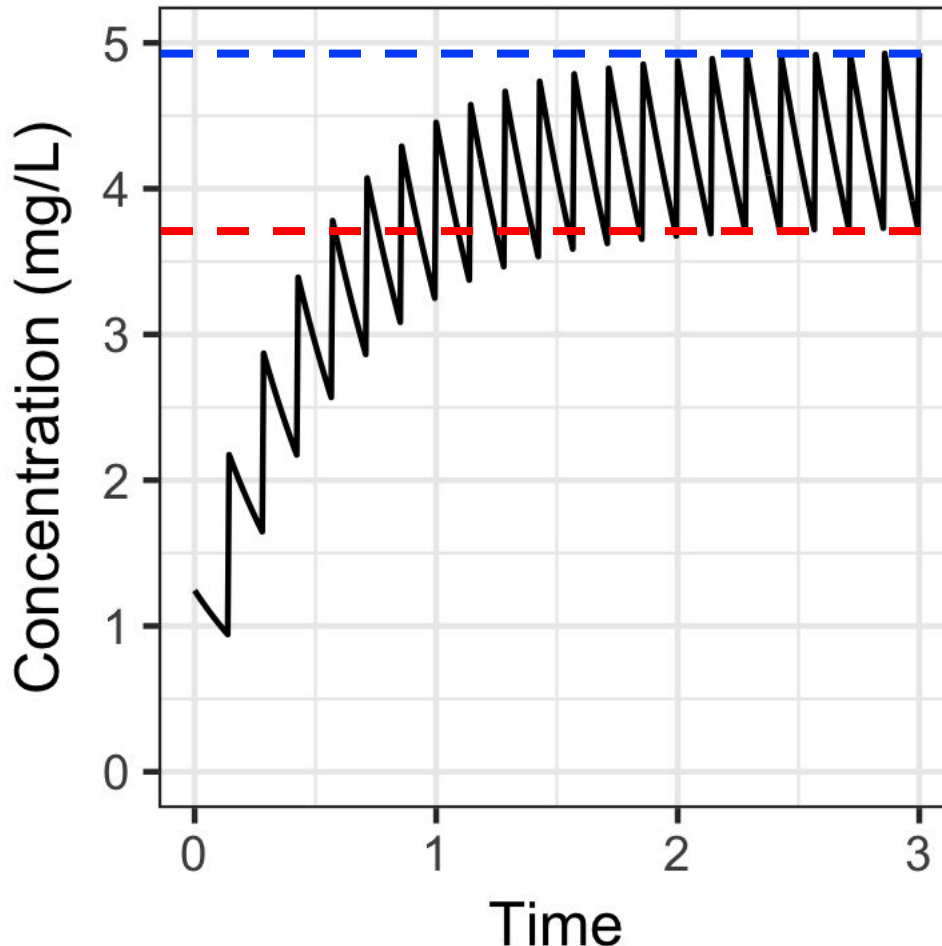


$$\begin{aligned}
 C(t) &= \sum_{n=0}^{N-1} C_0 e^{-k(t-n\tau)} \\
 &= \sum_{n=0}^{N-1} C_0 e^{-kt} e^{kn\tau} \\
 &= C_0 e^{-kt} \sum_{n=0}^{N-1} (e^{k\tau})^n
 \end{aligned}$$

As $N \rightarrow \infty$

$$C(t) = \frac{C_0 e^{-kt}}{1 - e^{-k\tau}}$$

Formulas for $C_{max,ss}$ and $C_{min,ss}$



$$C_{max,ss} = \frac{C_0}{1 - e^{-k\tau}}$$

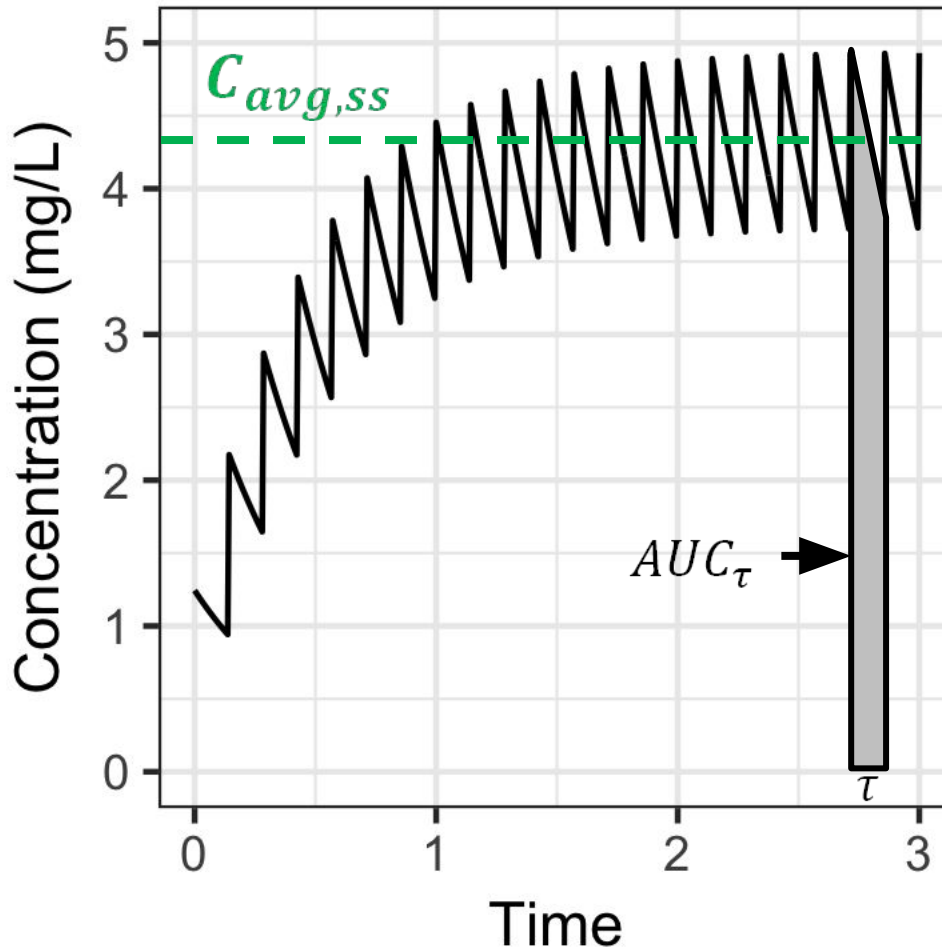
$$C_{min,ss} = \frac{C_0 e^{-k\tau}}{1 - e^{-k\tau}}$$

Recall that k and C_0 depends on both V and CL

What about average concentration $C_{avg,ss}$?

$$C(t) \xrightarrow{N \rightarrow \infty} \frac{C_0 e^{-kt}}{1 - e^{-k\tau}}$$

Formula for $C_{avg,ss}$ (for linear PK)



Total drug in = Total drug out

$$\text{Dose} = \int_{n\tau}^{(n+1)\tau} CL \cdot C(t) dt$$

If clearance doesn't depend on concentration (linear)

$$\text{Dose} = CL \cdot \int_{n\tau}^{(n+1)\tau} C(t) dt$$

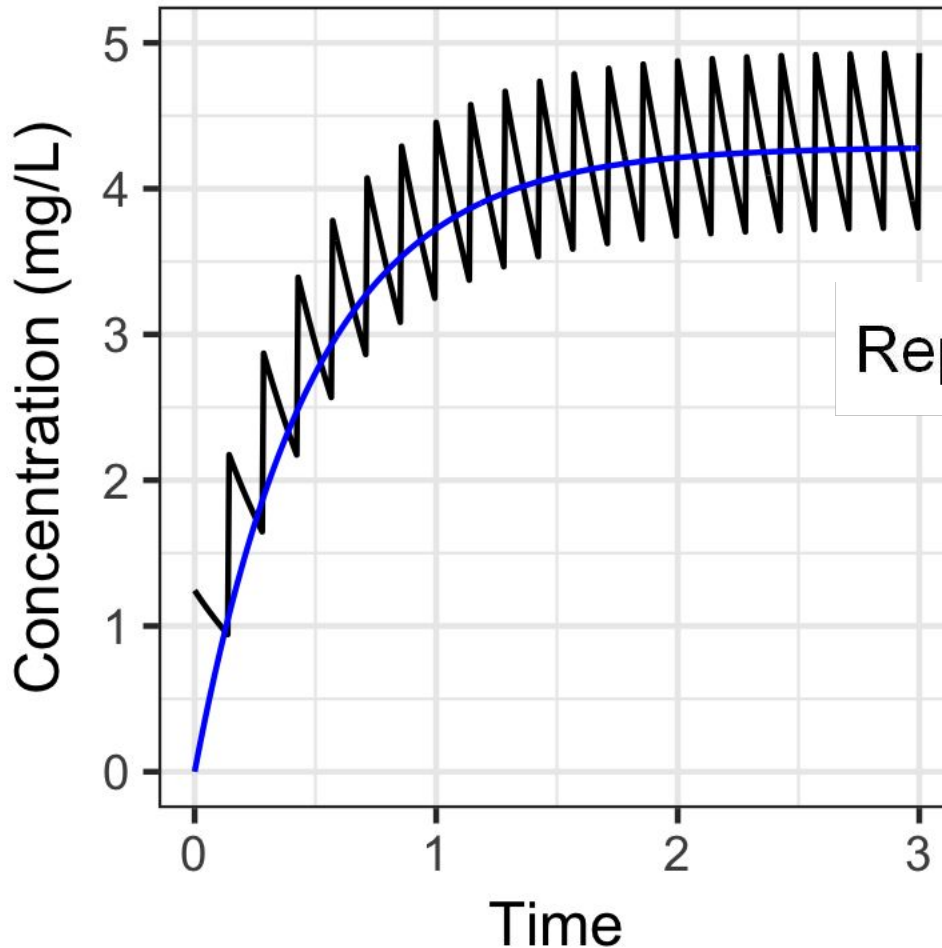
$$\text{Dose} = CL \cdot AUC_{\tau}$$

$$AUC_{\tau} = \frac{\text{Dose}}{CL}$$

$$C_{avg,ss} = \frac{AUC_{\tau}}{\tau} = \frac{\text{Dose}}{CL \cdot \tau}$$

*Formula doesn't depend on specific model for $C(t)$
It only requires linear clearance*

Repeated dosing similar to infusion



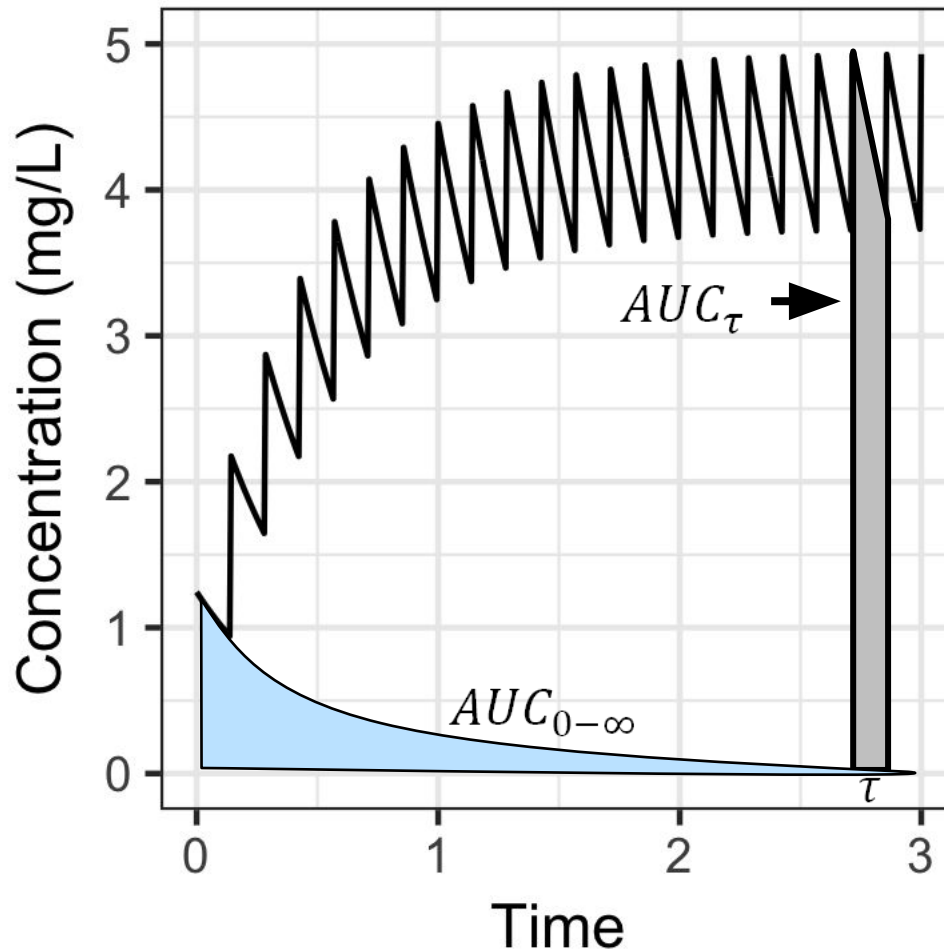
Infusion: $C_{ss} = \frac{\text{Infusion Rate}}{CL}$

Repeat dose $C_{avg,ss} = \frac{\text{Dose}/\tau}{CL}$

Infusion Rate $\sim$ Dose Rate

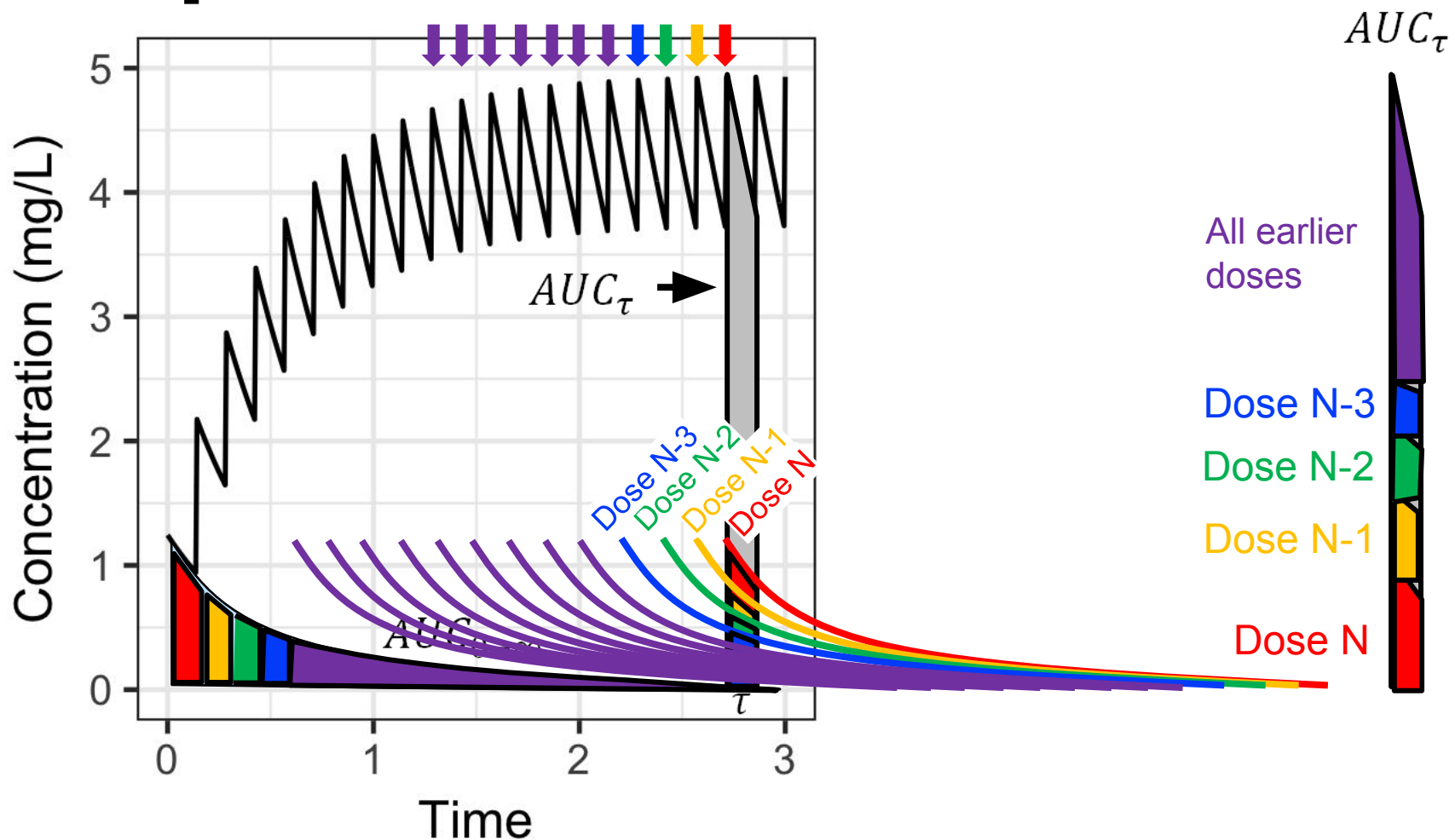
Infusion Rate $\sim$ Dose/ τ

Cool and useful result:

$$AUC_{0-\infty} = AUC_{\tau}$$


$AUC_{0-\infty} = AUC_{\tau}$

Graphical Demonstration



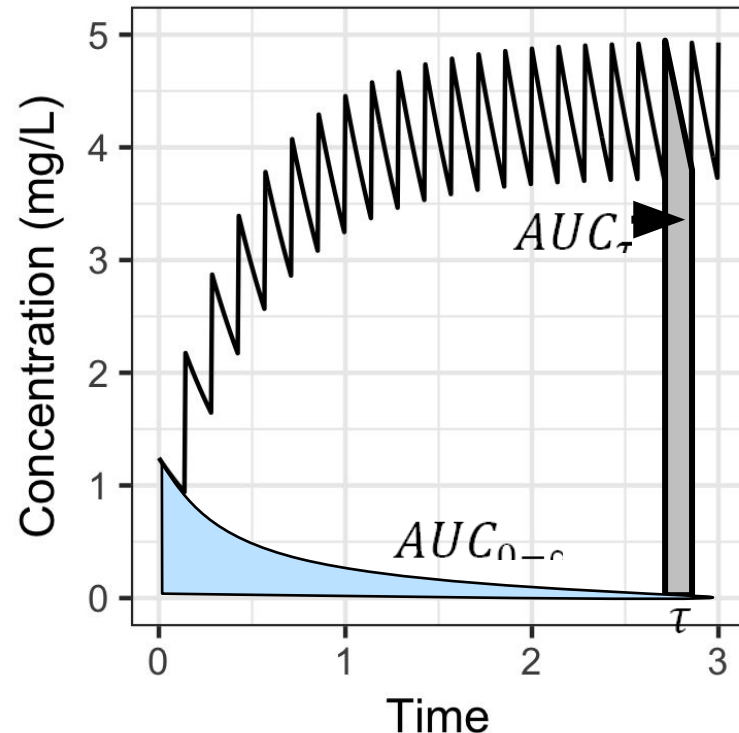
$AUC_{0-\infty} = AUC_{\tau}$

Mathematical Demonstration

$$\begin{aligned}
 AUC_{\tau} &= \int_{n\tau}^{(n+1)\tau} C(t) dt \\
 &= \int_{n\tau}^{(n+1)\tau} [C_1(t) + C_1(t - \tau) + C_1(t - 2\tau) + \dots + C_1(t - n\tau)] dt \\
 &= \int_{n\tau}^{(n+1)\tau} C_1(t) dt + \int_{n\tau}^{(n+1)\tau} C_1(t - \tau) dt + \int_{n\tau}^{(n+1)\tau} C_1(t - 2\tau) dt + \dots + \int_{n\tau}^{(n+1)\tau} C_1(t - n\tau) dt \\
 &= \int_{n\tau}^{(n+1)\tau} C_1(t) dt + \int_{(n-1)\tau}^{n\tau} C_1(t) dt + \int_{(n-2)\tau}^{(n-1)\tau} C_1(t) dt + \dots + \int_0^{\tau} C_1(t) dt \\
 &= \int_0^{(n+1)\tau} C_1(t) dt \\
 &\rightarrow \int_0^{\infty} C_1(t) dt \text{ as } n \rightarrow \infty \\
 AUC_{\tau} &= AUC_{0-\infty}
 \end{aligned}$$

Key Insights

- For IV drugs, $C_{avg,ss}$ depends only on dose, dosing interval and clearance
 - $C_{avg} = \text{Dose}/(\text{CL} \cdot \tau)$
 - CL can be estimated from either $AUC_{0-\infty}$ or AUC_{τ}
- The time to steady state depends on volume and half-life.



$$C_{avg,ss} = \frac{AUC_{\tau}}{\tau} = \frac{AUC_{0-\infty}}{\tau} = \frac{\text{Dose}}{\text{CL} \cdot \tau}$$

SEE QUIZ QUESTIONS

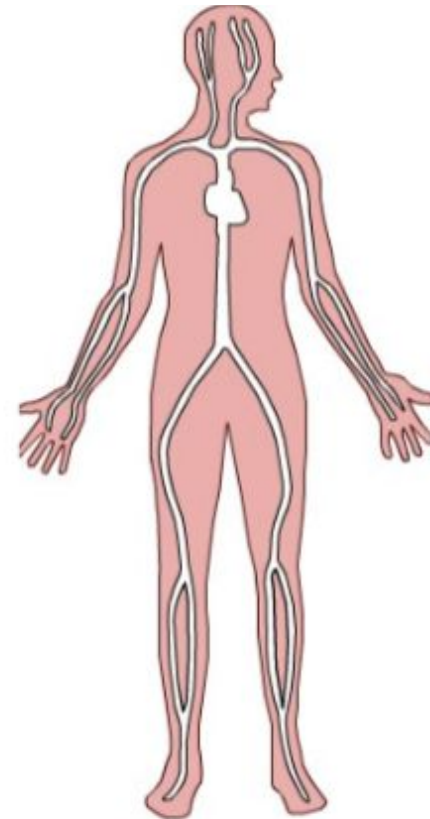
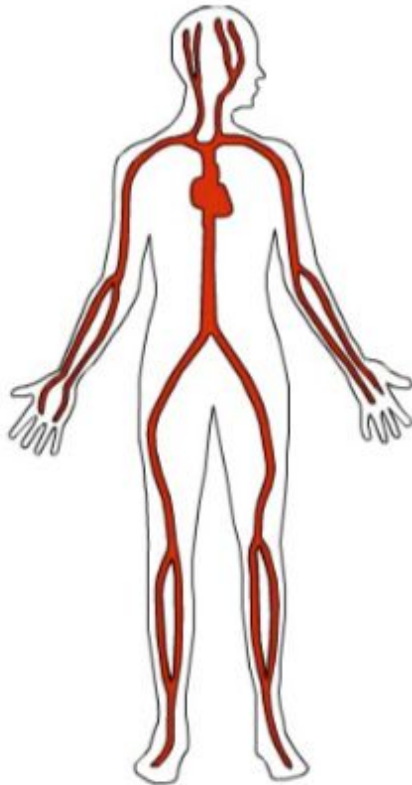
Distribution

Distribution

Systemic
Circulation

Distribution

Other
Tissues

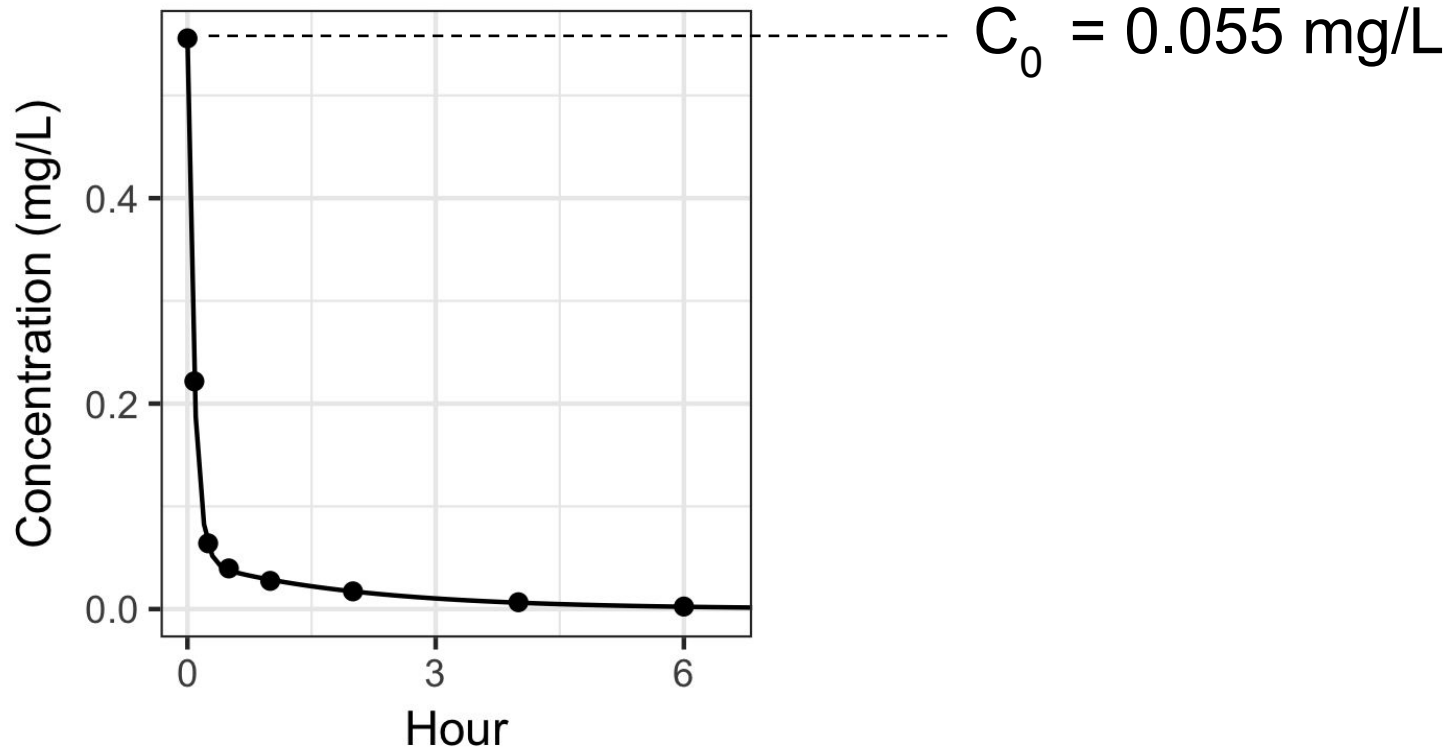


Factors that can effect distribution

- Lipophilicity (able to dissolve and move through fats)
- Transport proteins can move drugs around
- Blood proteins (e.g. albumin) will bind to low molecular weight drugs and prevent them from moving into tissue

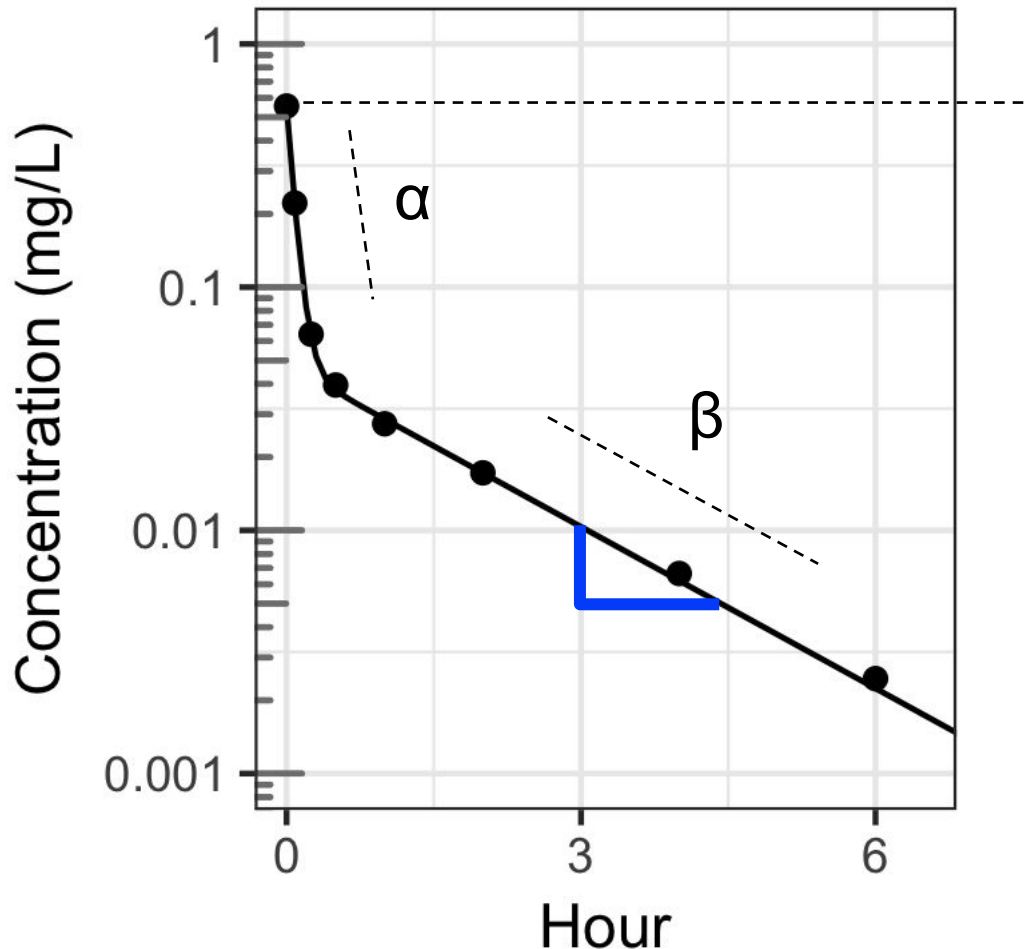
Profile of a single dose (Linear Space)

Dose = 10 mg



Profile of a single dose (Log Space)

$$C(t) = Ae^{-\alpha t} + Be^{-\beta t}$$



Dose = 10 mg

$C_0 = 0.55$ mg/L

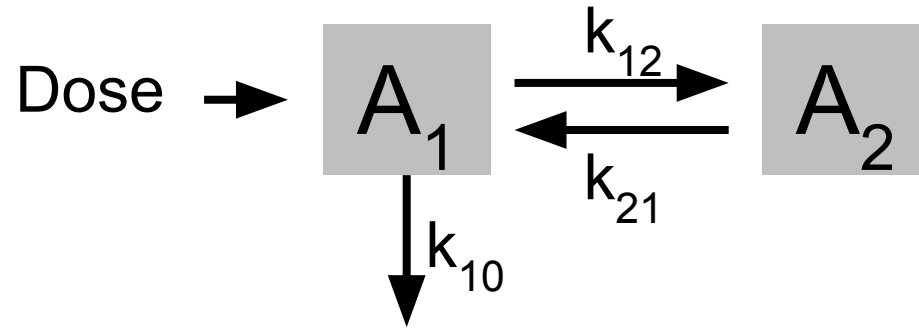
$V_1 = \text{Dose}/C_0$
= 18 L

α = initial decline
= 12/h

β = terminal slope
= 0.5/h

$t_{1/2\beta} = 1.4$ h

Compartmental Model formulation

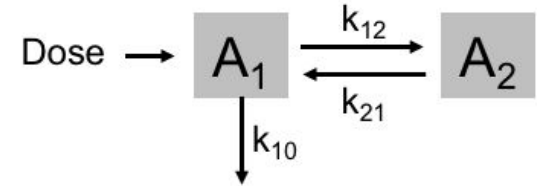


Rate of change of
amount in each
compartment

$$\begin{aligned}\frac{dA_1}{dt} &= -k_{10} \cdot A_1 - k_{12} \cdot A_1 + k_{21} \cdot A_2 \\ \frac{dA_2}{dt} &= k_{12} \cdot A_1 - k_{21} \cdot A_2\end{aligned}$$

Finding the analytical solution

$$\begin{aligned}\frac{dA_1}{dt} &= -k_{10} \cdot A_1 - k_{12} \cdot A_1 + k_{21} \cdot A_2 \\ \frac{dA_2}{dt} &= k_{12} \cdot A_1 - k_{21} \cdot A_2\end{aligned}$$



$$\frac{d}{dt} \begin{pmatrix} A_1 \\ A_2 \end{pmatrix} = \underbrace{\begin{pmatrix} -(k_{10} + k_{12}) & k_{21} \\ k_{12} & -k_{21} \end{pmatrix}}_M \begin{pmatrix} A_1 \\ A_2 \end{pmatrix}$$

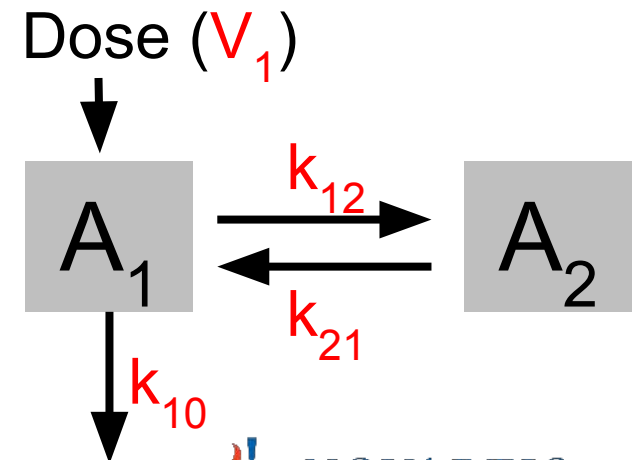
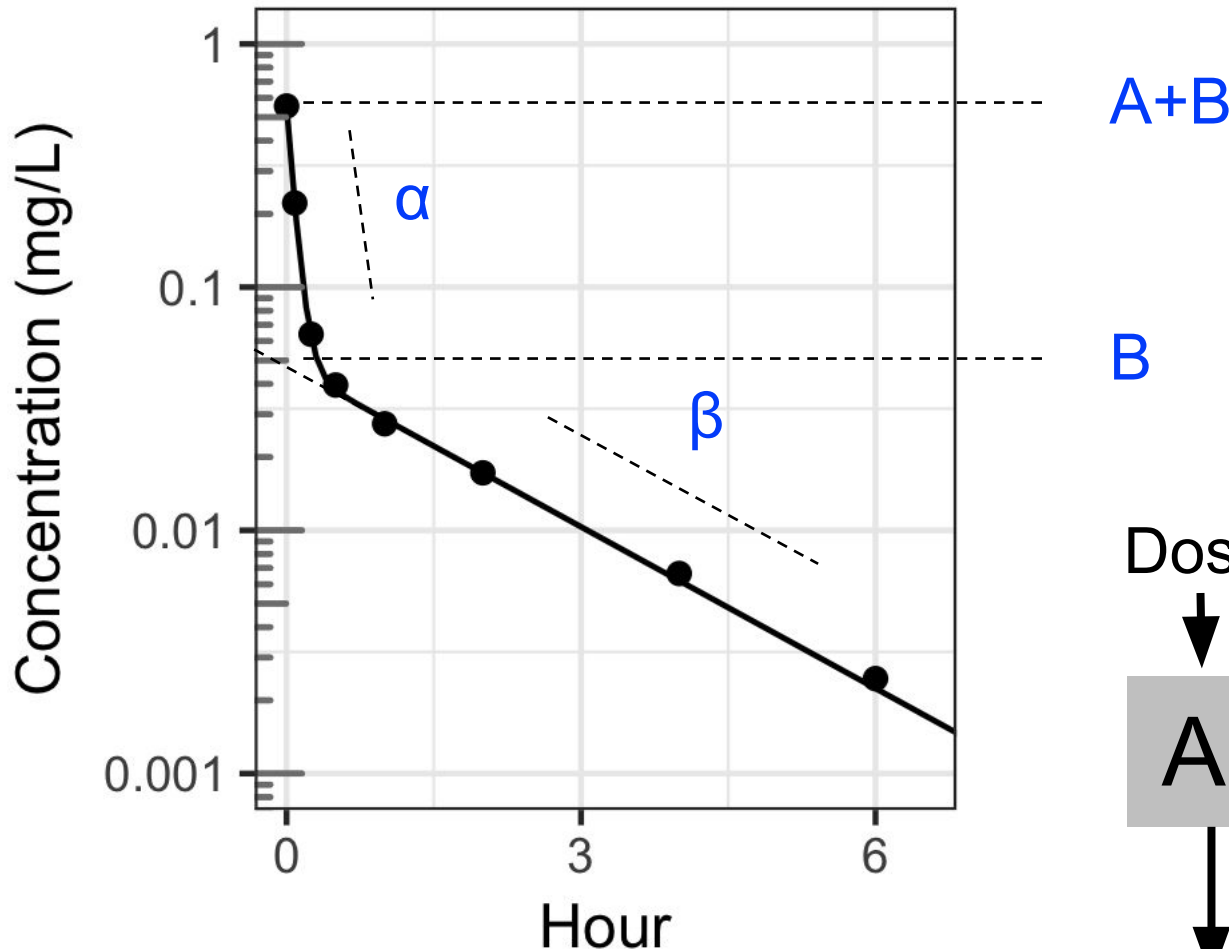
α and β are the eigenvalues of M

A and B come from the eigenvectors of M and the initial dose

Details in www.pfim.biostat.fr/PFIM_PKPD_library.pdf

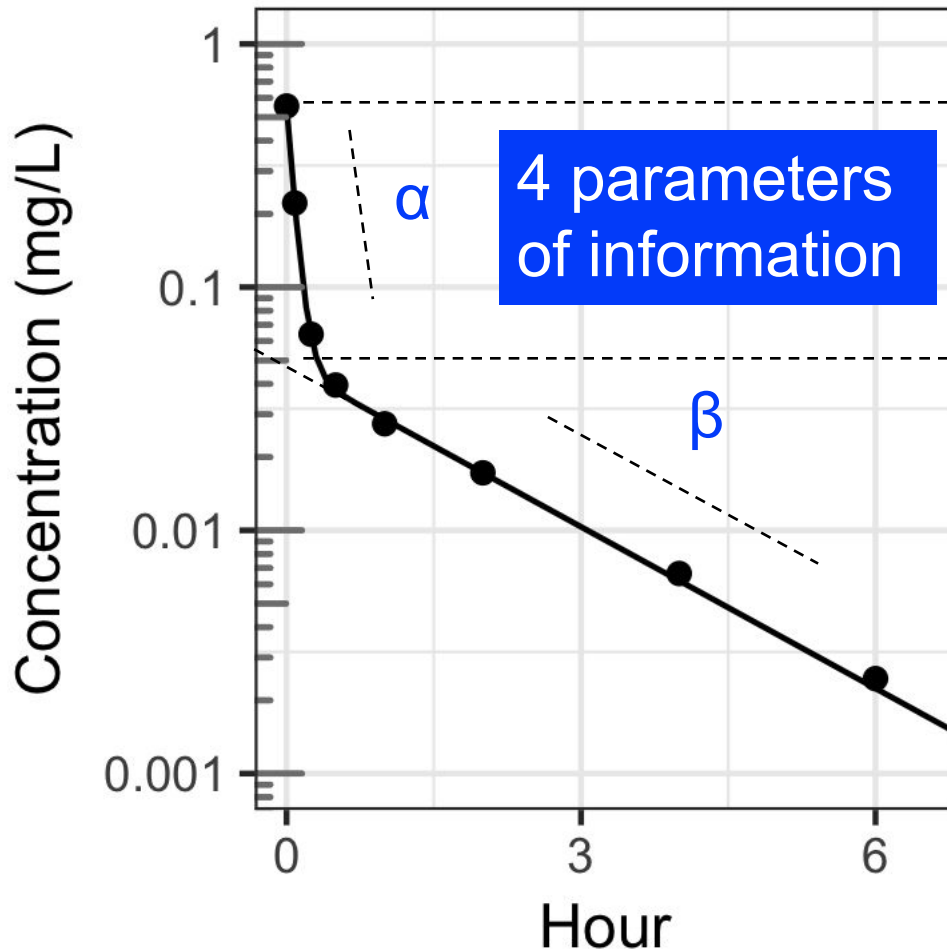
Compartment model and prolife each have 4 parameters

$$C(t) = Ae^{-\alpha t} + Be^{-\beta t}$$



Elimination from the peripheral compartment not identifiable.

$$C(t) = Ae^{-\alpha t} + Be^{-\beta t}$$

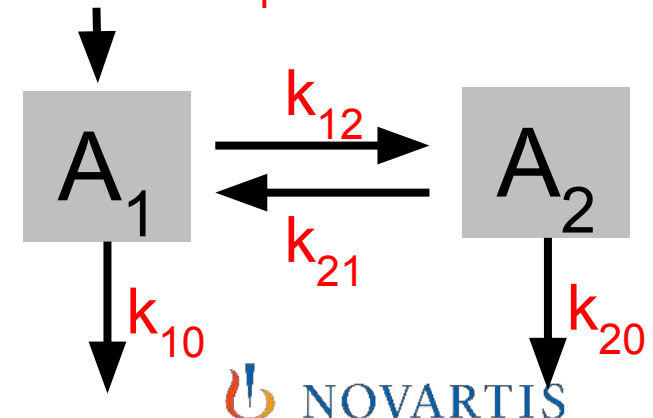


A+B

B

5 parameters
In model is too
many

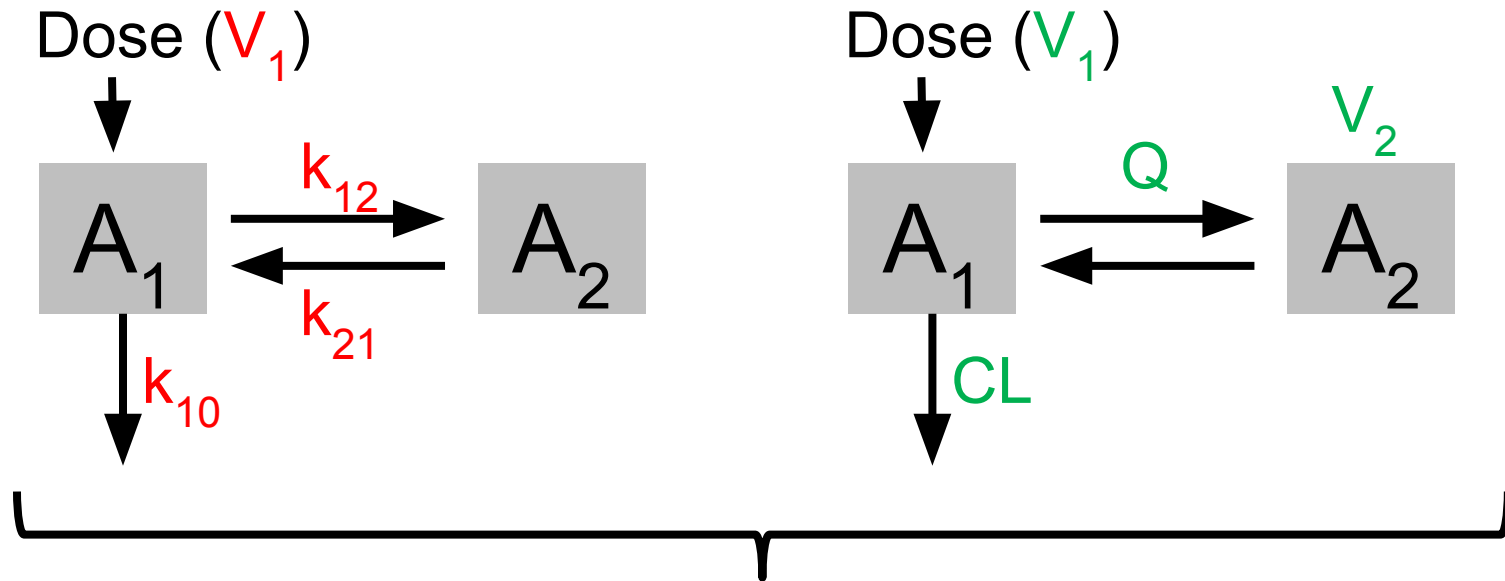
Dose (V_1)



Alternative parameterization for 2 compartment model

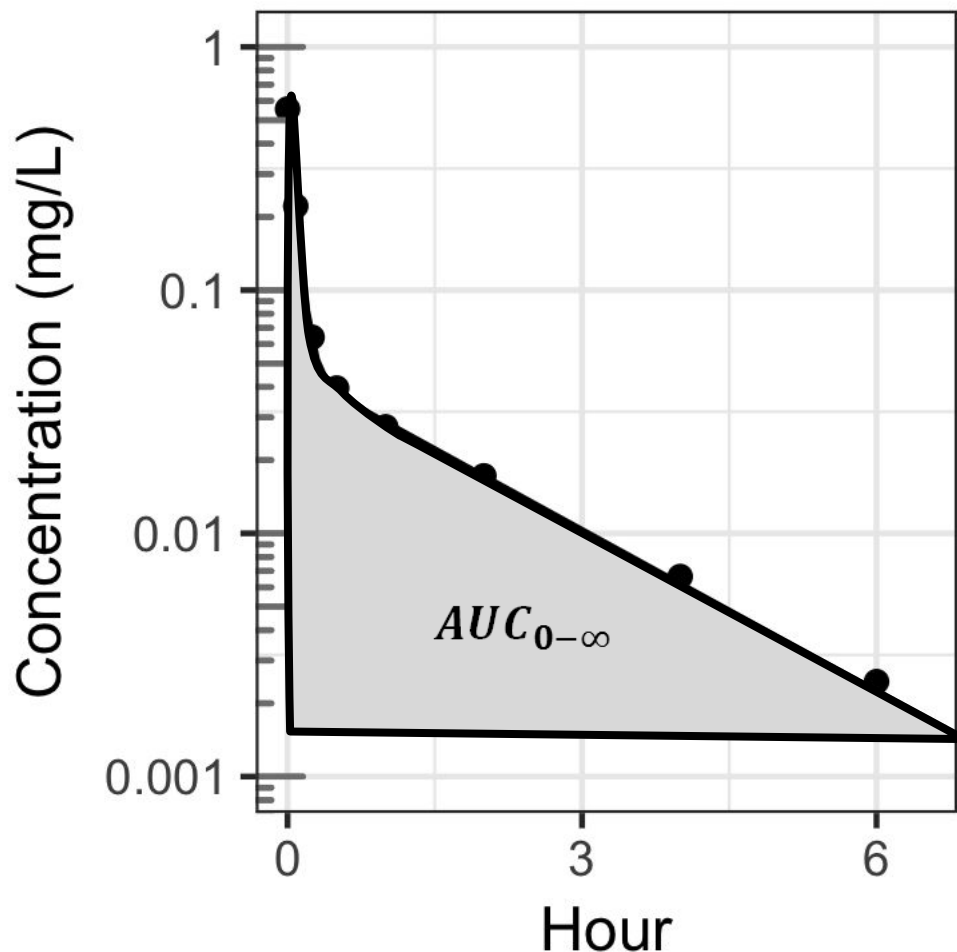
$$\{V_1, k_{10}, k_{12}, k_{21}\}$$

$$\{V_1, CL, Q, V_2\}$$



$$\begin{aligned} CL &= k_{10} \cdot V_1 \\ Q &= k_{12} \cdot V_1 \\ V_2 &= V_1 \cdot (k_{12} / k_{21}) \end{aligned}$$

Clearance still relates to the Area Under the conc. Curve ($AUC_{0-\infty}$)



Total drug in = Total drug out

$$\text{Dose} = \int_0^{\infty} CL \cdot C(t) dt$$

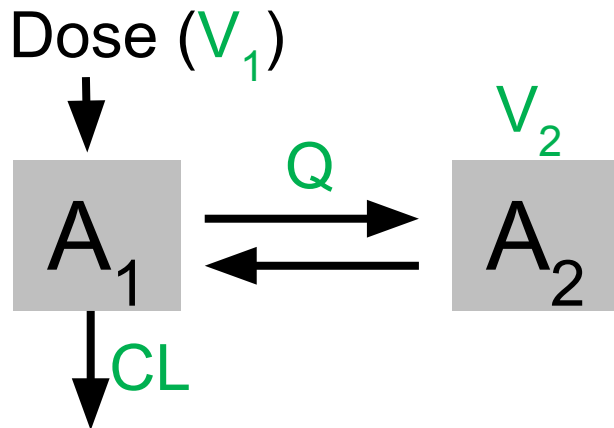
If clearance doesn't depend on concentration (linear)

$$\text{Dose} = CL \cdot \int_0^{\infty} C(t) dt$$

$$\text{Dose} = CL \cdot AUC_{0-\infty}$$

$$AUC_{0-\infty} = \frac{\text{Dose}}{CL}$$

Be careful in interpreting parameters from the model



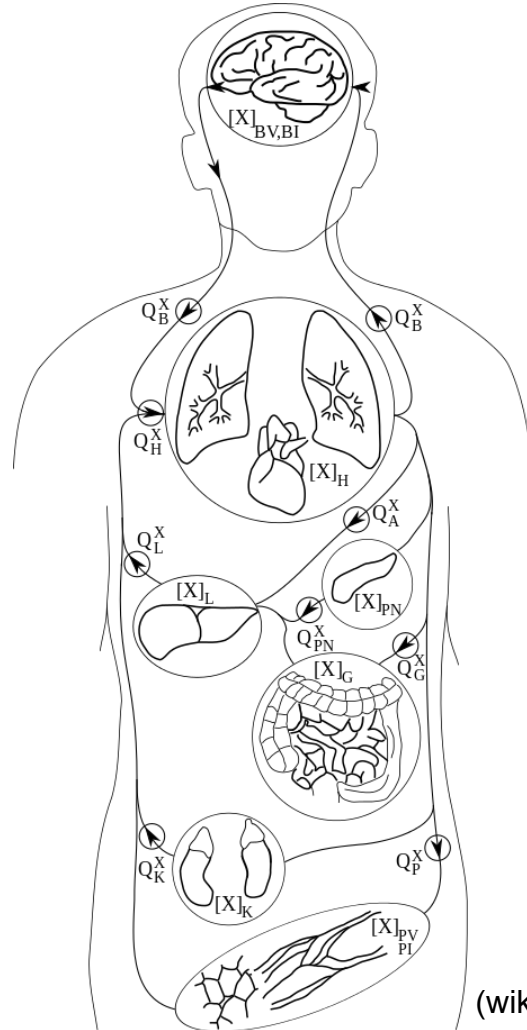
Directly observable params:

- $V_1 = \text{Dose}/C_0$
- $CL = AUC_{0-\infty} = AUC_{\tau}$

“Apparent” parameters

- V_2 is not a physiological volume and harder to “identify” from data
- $C_2 = A_2/V_2$ is not a meaningful concentration and should never be used

Really, there are many more peripheral compartments, but the 2 compartment approximation often works



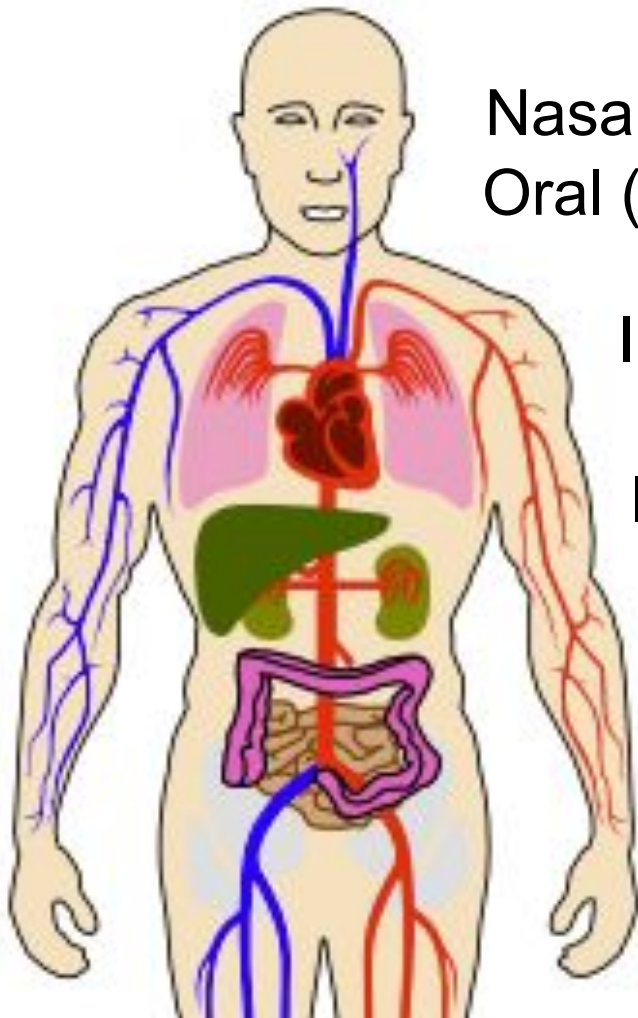
(wikipedia for PBPK)

Key Lessons

- Distribution leads to two (or more) compartment kinetics
- Multiple “half-lives” are observable in the data.
- Even for two models, $AUC_{0-\infty}$, AUC_T and $C_{avg,ss}$ are still driven by CL, when CL is independent of concentration
 - This result holds for any number of compartments
- The volume becomes a function of time and the behavior of this function at time zero (V_1) or as time goes to infinity (V_z , V_{ss}) are often what is reported

Absorption and bioavailability

Routes of Administration (examples)



Nasal (nose)

Oral (mouth)

Inhalation (lung)

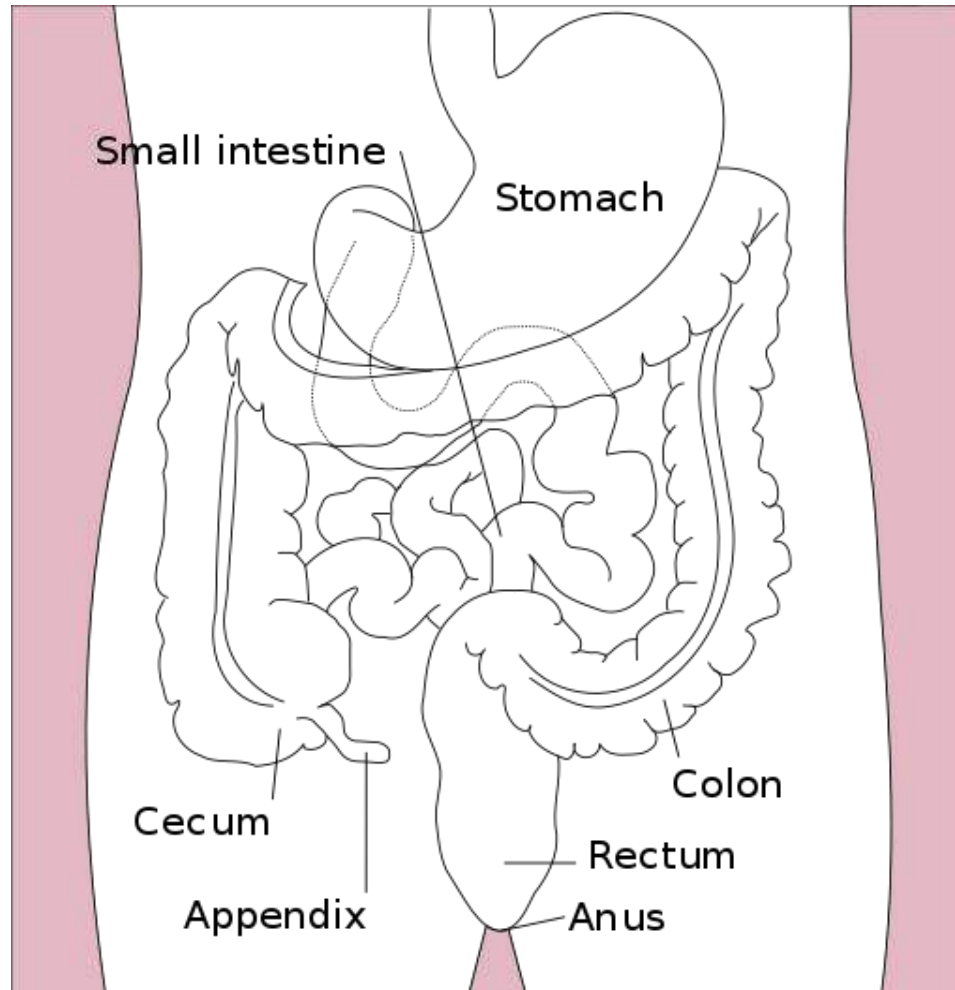
Intravenous (vein)

Intramuscular (muscle)

Subcutaneous (under skin)

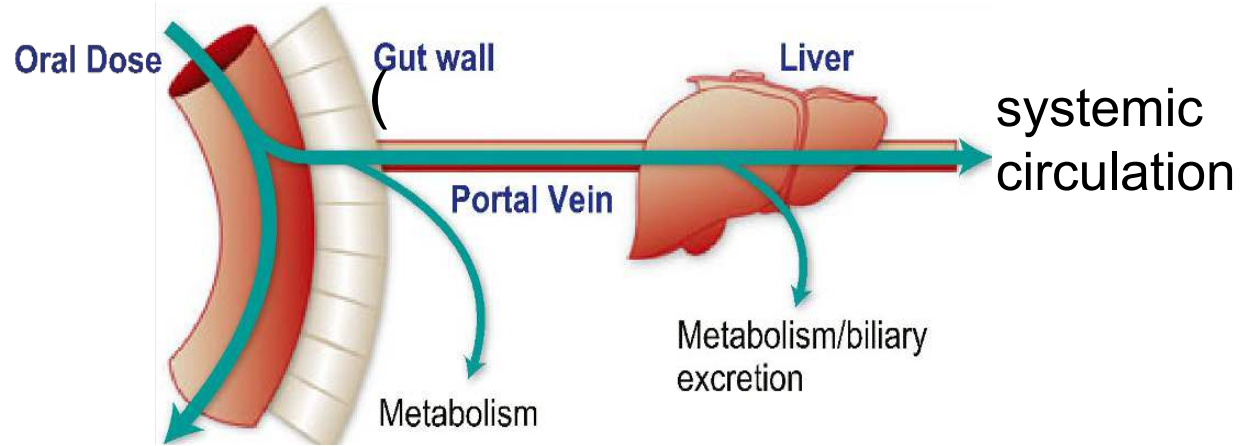
Transdermal (skin patch)

Oral dose of drug is absorbed through the gastrointestinal tract



Bioavailability (some drug is lost)

Oral dose
small molecule



Oral
Absorption

Intestinal
First Pass Elimination

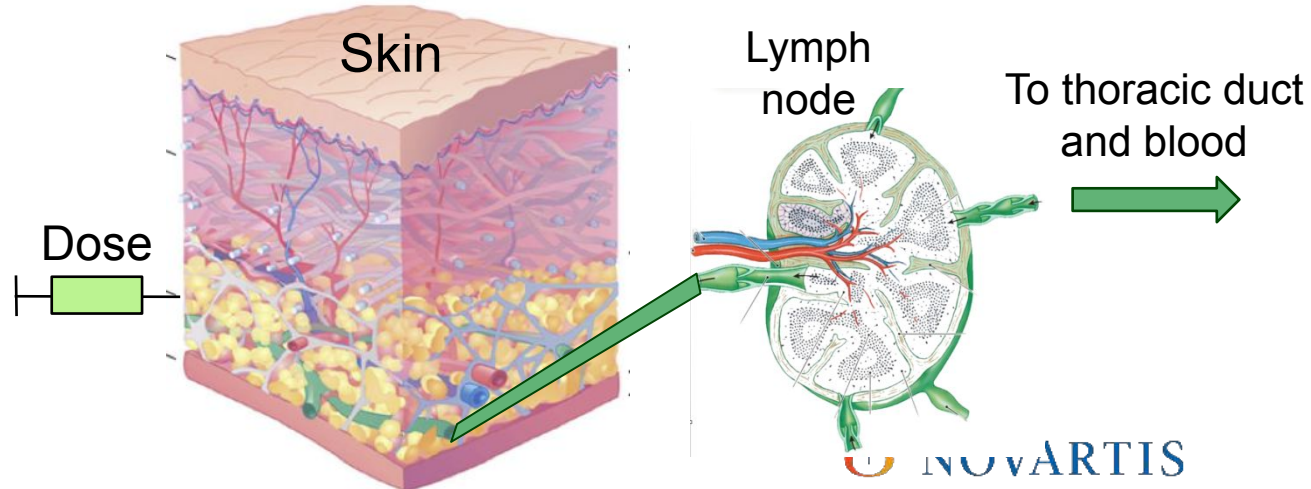
Hepatic
First Pass Elimination

Subcutaneous
Absorption

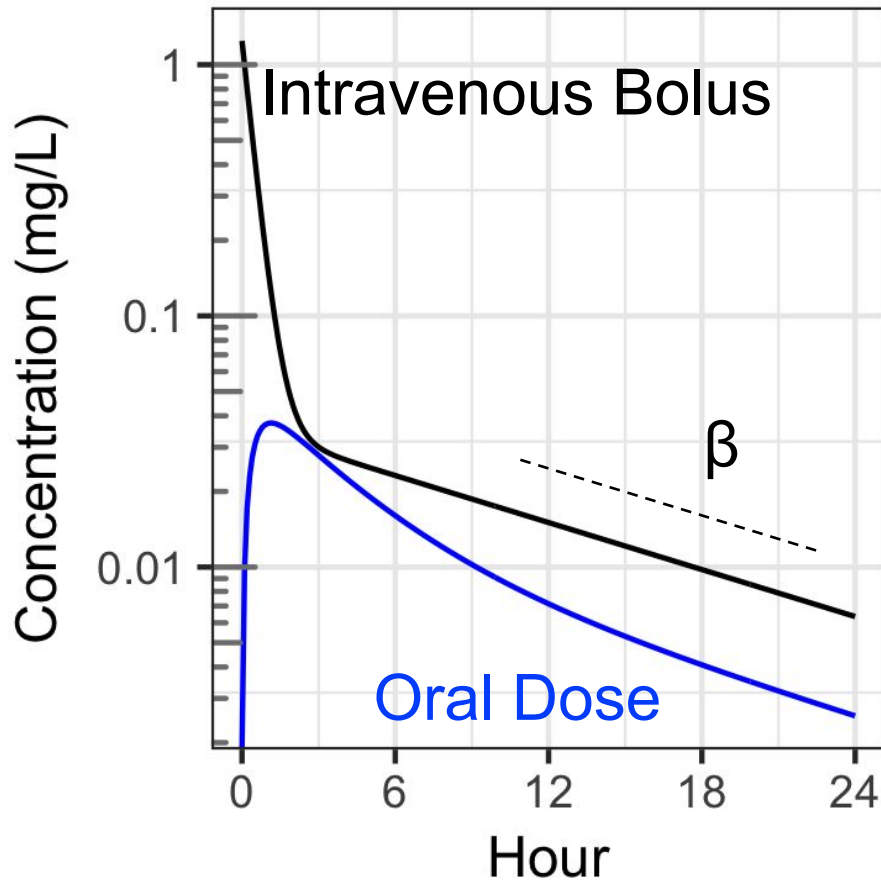
Inject Site
First Pass Elimination

Lymphatic
First Pass Elimination

Subcutaneous dose
biologic

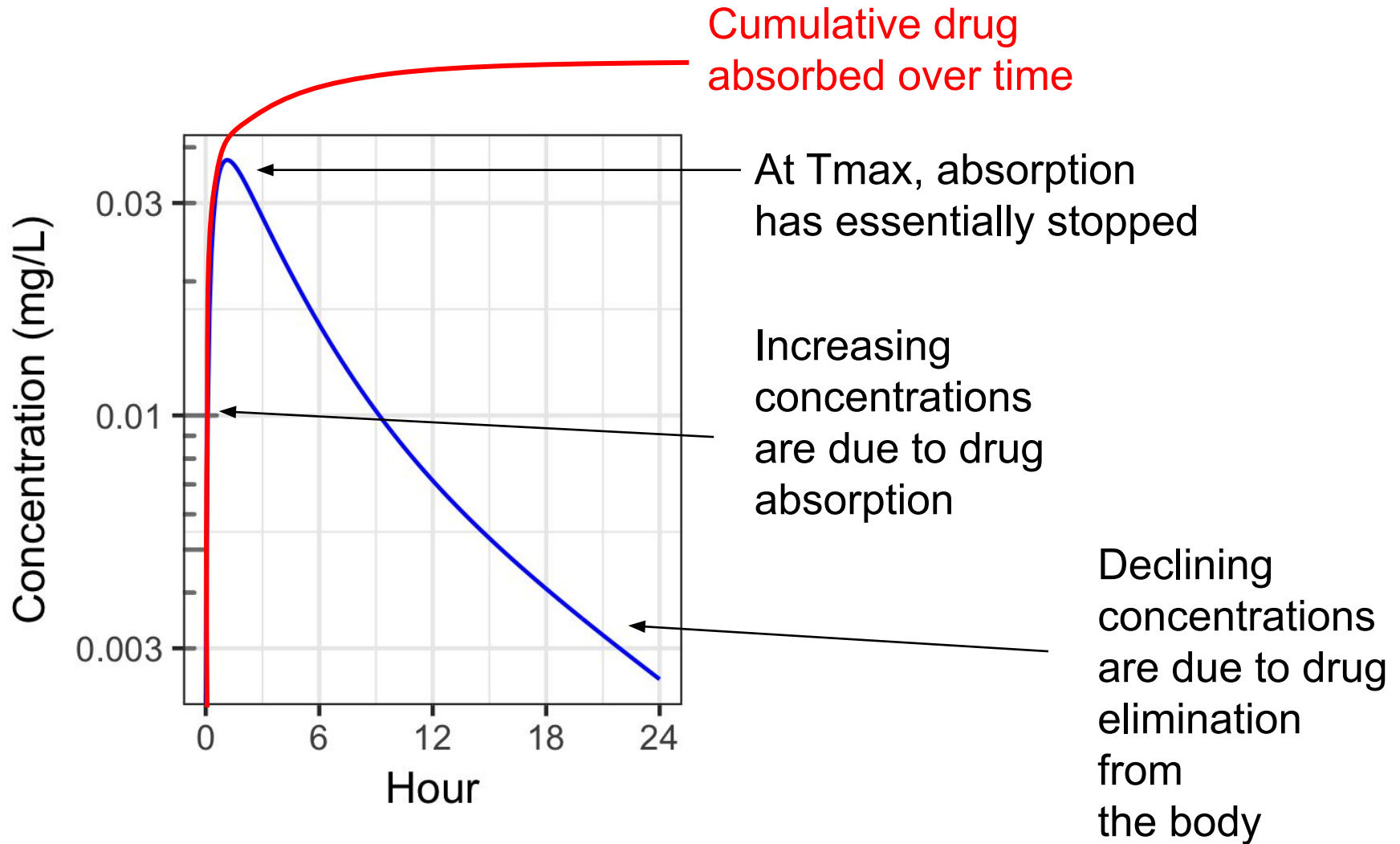


Oral dose vs intravenous dose

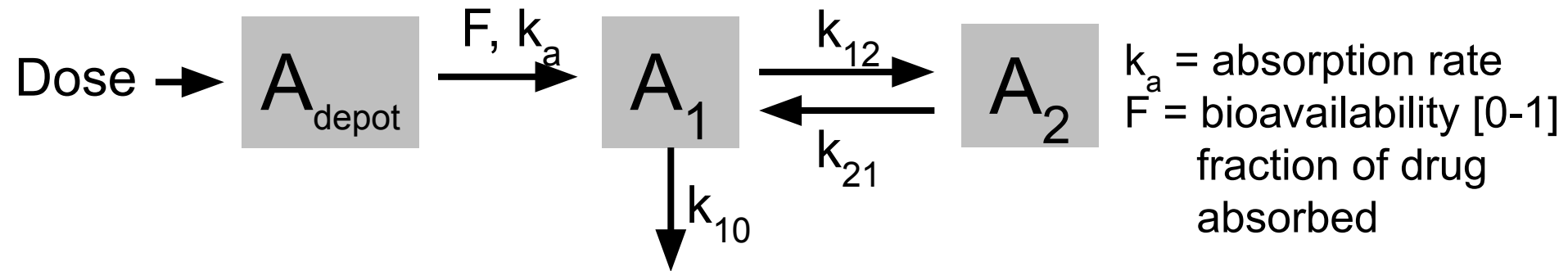


	IV Bolus	Oral
Absorption	No	Yes
Initial conc. (C ₀)	Dose/V ₁	0
Time of max conc.	0	>0
AUC _{0-∞}	Dose/CL	< Dose/CL
Terminal slope	β	β

Oral Dose



Compartment Model with Absorption

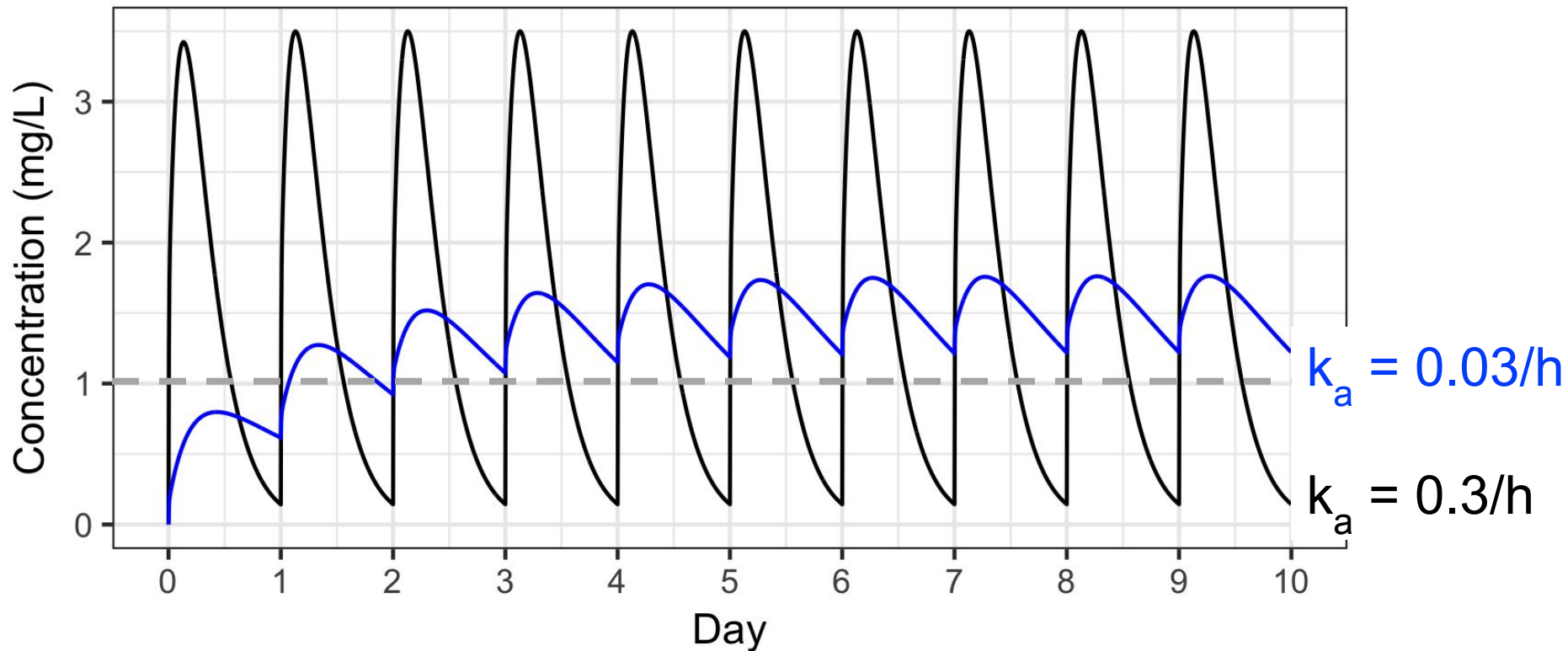


$$\frac{dA_{depot}}{dt} = \overbrace{-k_a \cdot A_{depot}}^{\text{absorption}}$$

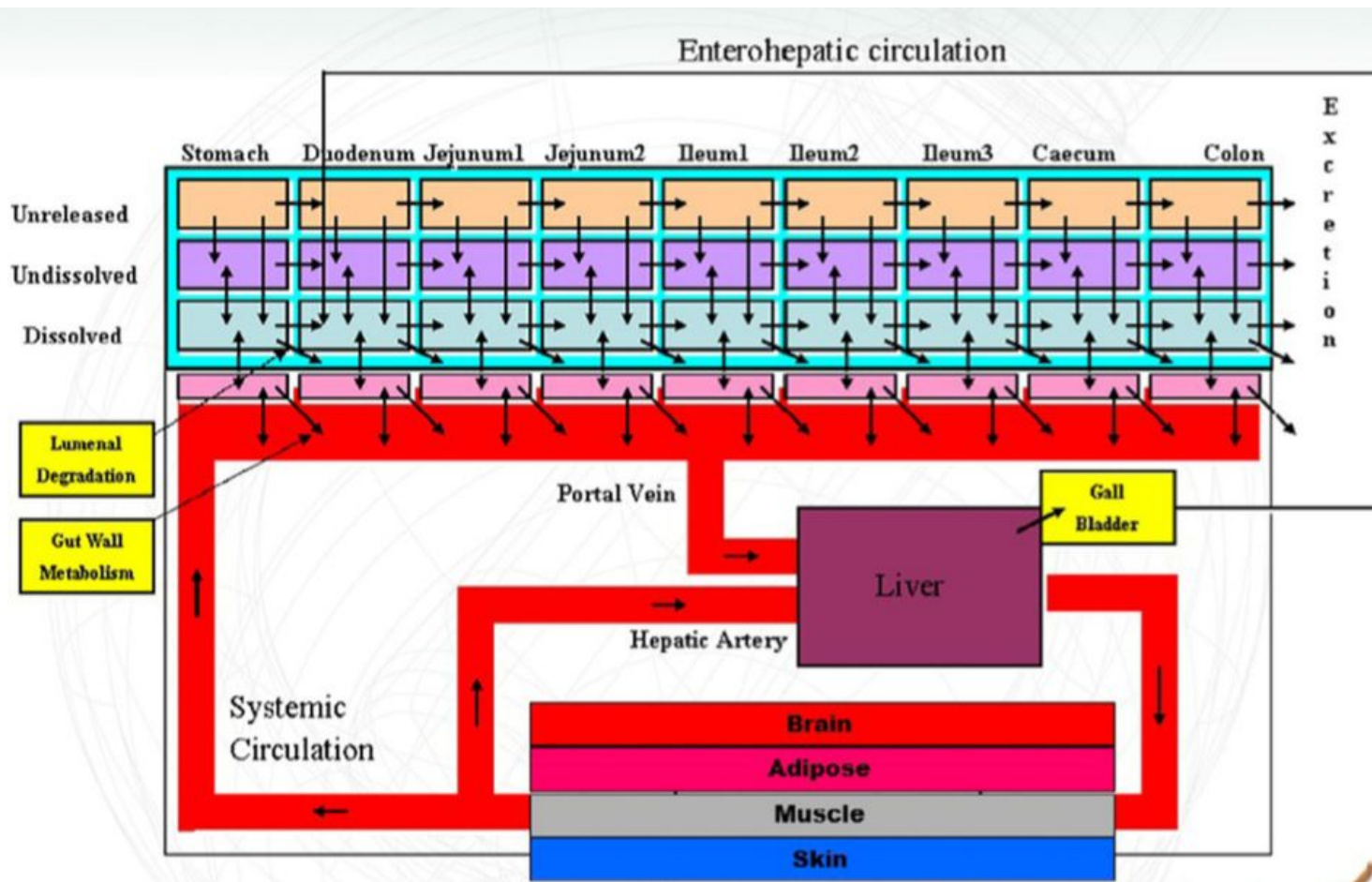
$$\frac{dA_1}{dt} = \overbrace{F \cdot k_a \cdot A_{depot}}^{\text{absorption}} \underbrace{-k_{10} \cdot A_1}_{\text{elimination}} \underbrace{-k_{12} \cdot A_1 + k_{21} \cdot A_2}_{\text{distribution}}$$

$$\frac{dA_2}{dt} = k_{12} \cdot A_1 - k_{21} \cdot A_2$$

Application – extended release prolongs exposure and can improve safety (reduce peak-trough ratio)



More complex absorption models can be developed



Abuhelwa, Ahmad Y., et al. "Food, gastrointestinal pH, and models of oral drug absorption." European Journal of Pharmaceutics and Biopharmaceutics 112 (2017): 234-248.

Question

- How would you expect changing the rate of absorption(k_a) to affect the average drug concentration at steady state?
- How does changing the bioavailability affect the average drug concentration

Updating average concentration formula

Total drug in = Total drug out

$$F \cdot \text{Dose} = \int_{n\tau}^{(n+1)\tau} CL \cdot C(t) dt$$

If clearance is linear

$$F \cdot \text{Dose} = CL \cdot \int_{n\tau}^{(n+1)\tau} C(t) dt$$

$$F \cdot \text{Dose} = CL \cdot AUC_{\tau}$$

$$AUC_{\tau} = \frac{F \cdot \text{Dose}}{CL}$$

$$C_{avg,ss} = \frac{AUC_{0-\infty}}{\tau} = \frac{F \cdot \text{Dose}}{CL \cdot \tau}$$

P Formula doesn't depend on absorption, but it does depend on F **IS**

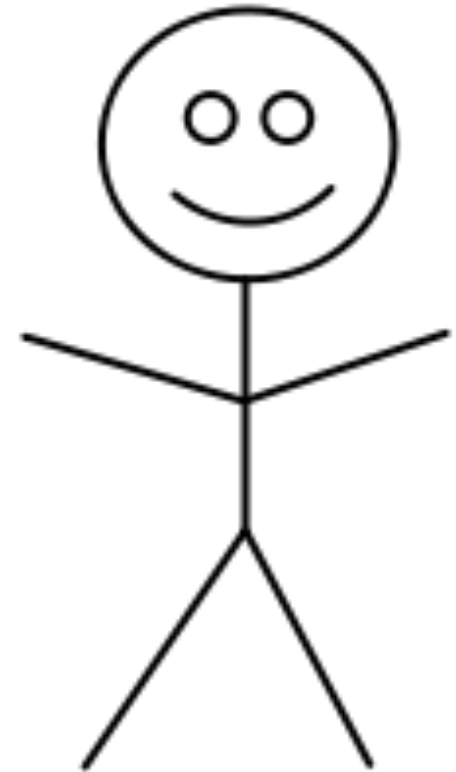
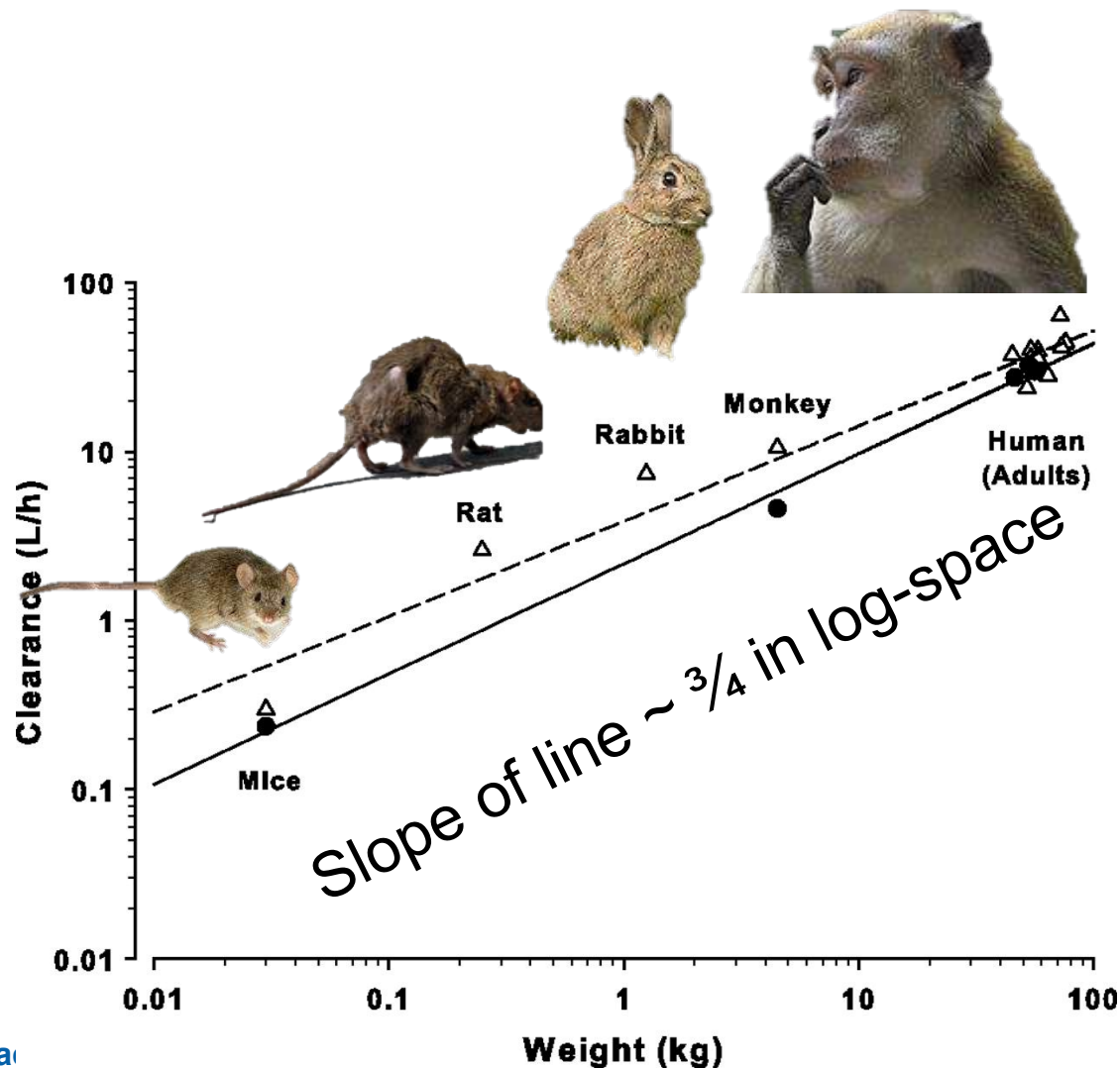
Key Lessons

- When drugs are given by alternative routes to intravenous (e.g. oral, subcutaneous, etc.), they must be absorbed before entering blood stream.
- Some of the drug may be lost before entering the blood.

Allometric Scaling

Effect of body size on PK parameters

Often, we want to predict PK in humans from animal data



Moore, Brioni R., et al.
"Pharmacokinetics, pharmacodynamics, and allometric scaling of chloroquine in a murine malaria model." *Antimicrobial agents and chemotherapy* 55.8 (2011): 3899-3907. Pictures from wikipedia

Many biological processes scale with body weight

- The weight of lifeforms spans 21 orders of magnitude:

- Smallest microbe $\sim 10^{-13}$ grams
- Largest whales $\sim 10^8$ grams

- Many fundamental biological processes scale with weight (WT) in a surprisingly simple way.

- Volume $\sim WT$
- Metabolic Rate $\sim WT^{3/4}$
- Lifespan $\sim WT^{1/4}$
- Heart rate $\sim WT^{-1/4}$
- Length of aorta $\sim WT^{1/4}$
- Height of tree $\sim WT^{1/4}$

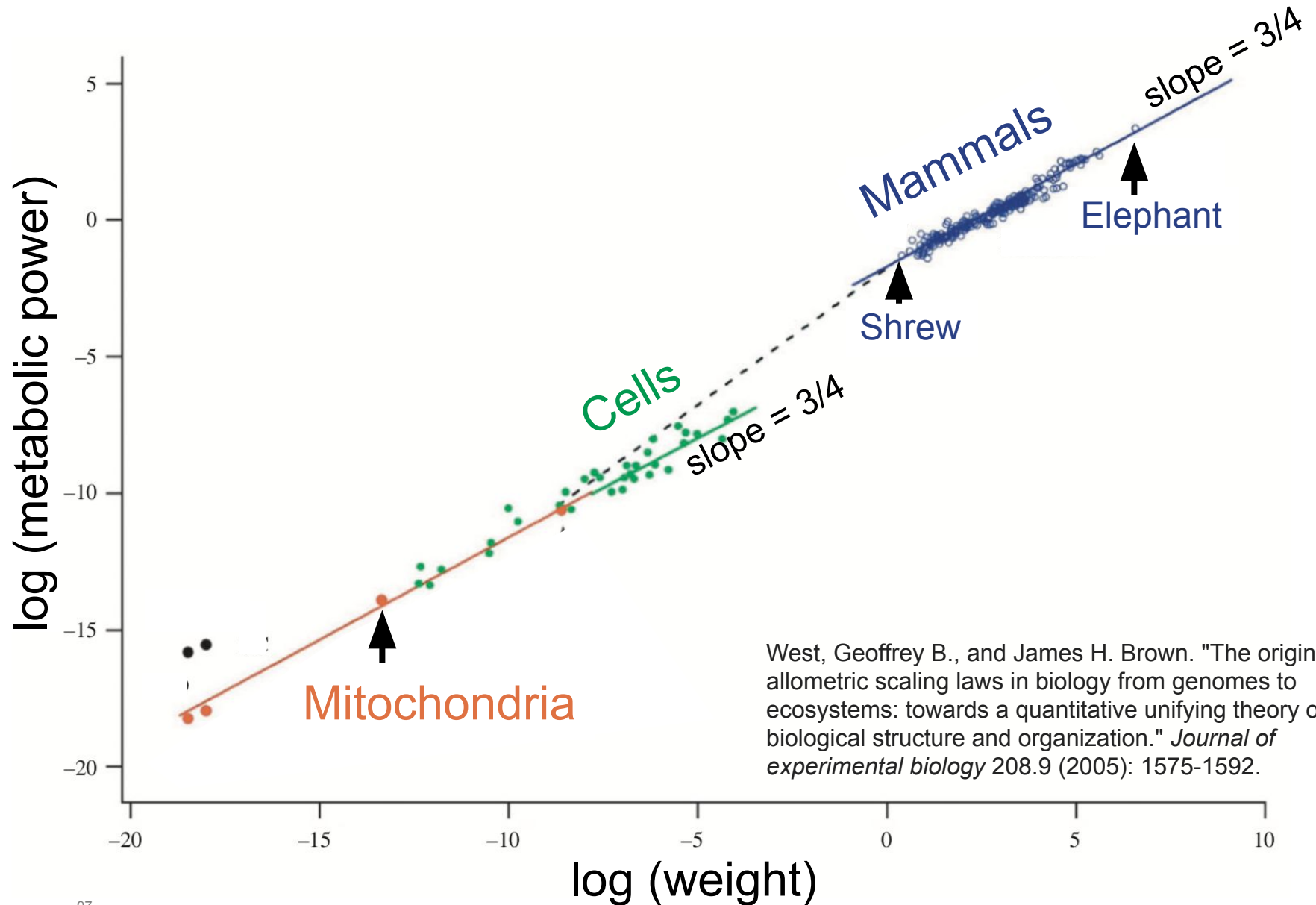
Total number of heart beats before death is independent of weight:

$$(\text{Heart rate}) \cdot (\text{Lifespan}) = WT^0$$

Mammals get about 1 billion heart beats in their lifetime (from hamster to elephant)

West, Geoffrey B., and James H. Brown. "The origin of allometric scaling laws in biology from genomes to ecosystems: towards a quantitative unifying theory of biological structure and organization." *Journal of experimental biology* 208.9 (2005): 1575-1592.

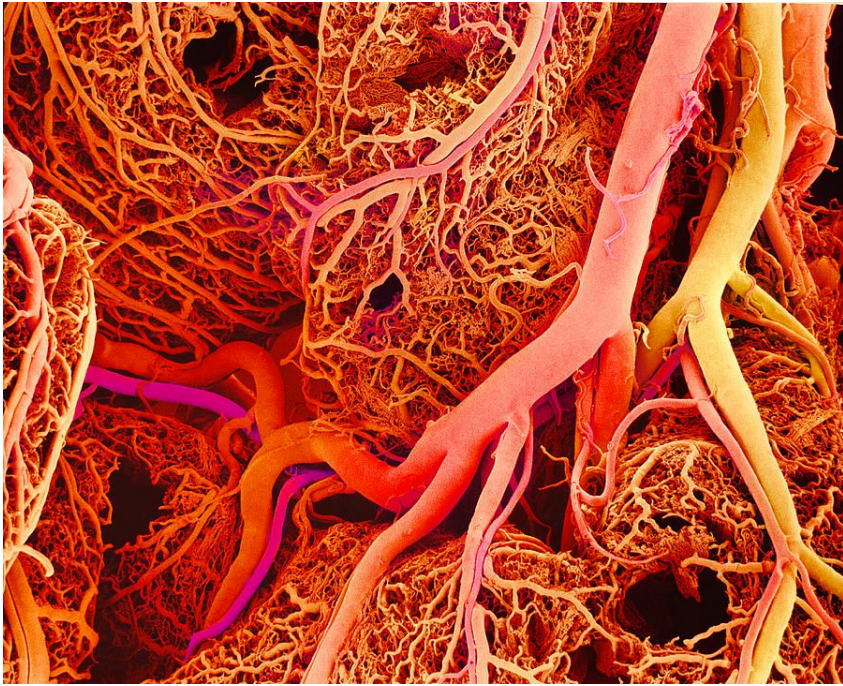
Metabolic rate $\sim WT^{3/4}$



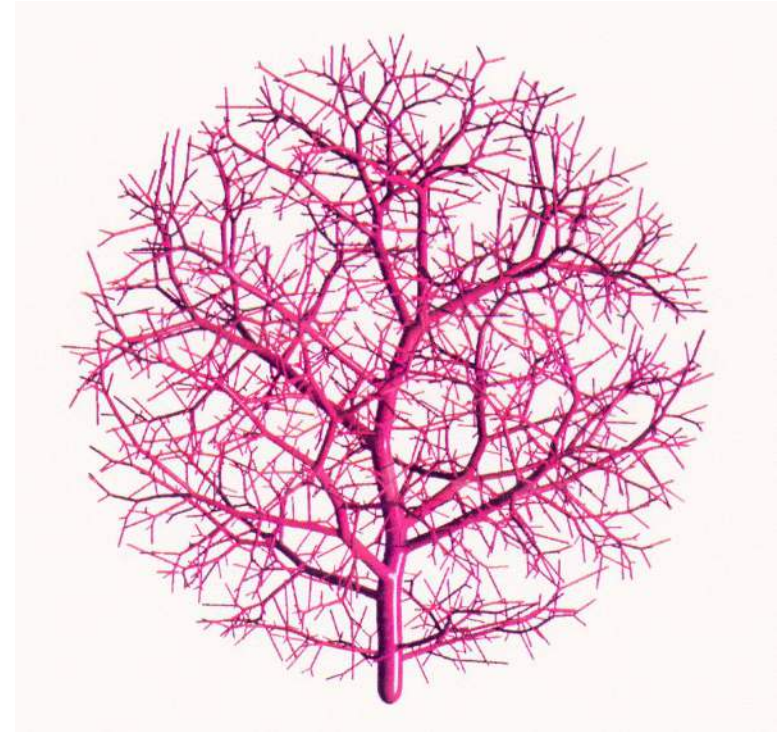
The reason for metabolism $\sim WT^{3/4}$ is to maximize surface area (SA)

- Evolution maximizes surface area (SA), in order to maximize nutrient absorption and metabolism.
- For standard geometries (cube, sphere), surface area relates to length (L), volume (V), and weight (WT) by:
 - $SA \sim L^2$
 - $V \sim L^3$
 - $SA \sim V^{2/3} \sim WT^{2/3}$ (because volume is proportional to weight)
- Because evolution pushes life to maximize surface area and a little more area can be obtained using the “fractal dimension” The maximum possible exponent is $3/4$.
- Therefore, $SA \sim WT^{3/4} > WT^{2/3}$

Blood vessels follow fractal patterns



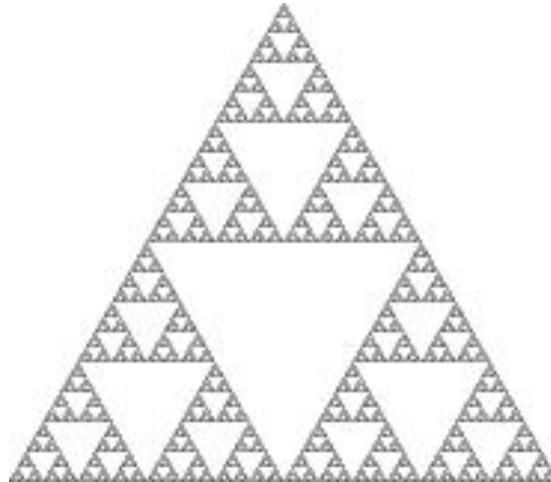
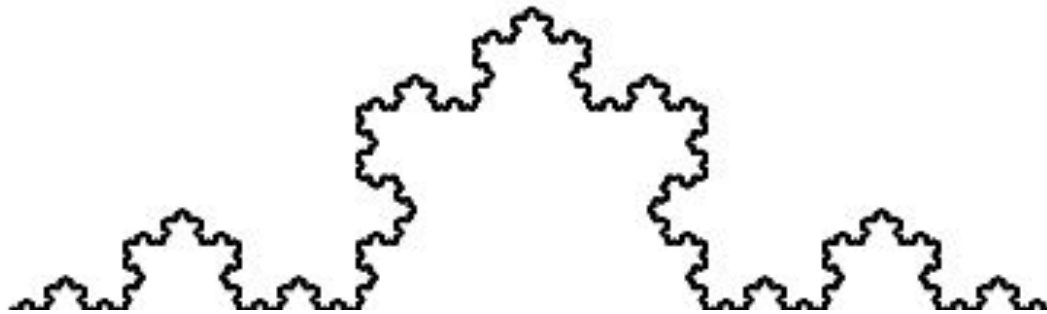
<https://blogs.uoregon.edu/artofnature/2013/12/03/fractal-of-the-week-blood-vessels/>



<https://dejavouz.wordpress.com/reflections/tree2/>

What is the optimal fractal dimensions to maximize surface area?

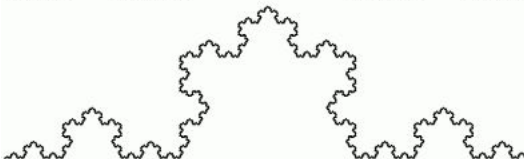
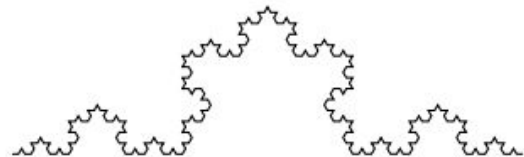
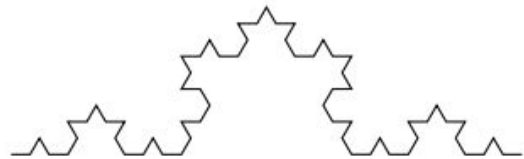
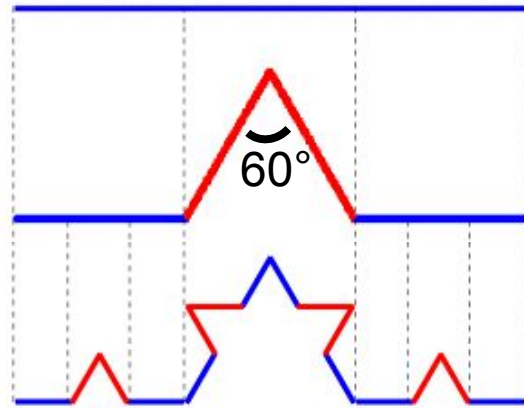
A fractal is a self similar as you zoom in to smaller scales



An example of building a fractal

Koch Curve

each line is $1/3$ the size of the original line. But now there are 4 segments (instead of 3)



Fractal

Length
1

$$4/3 = 1.3$$

$$16/9 = 1.8$$

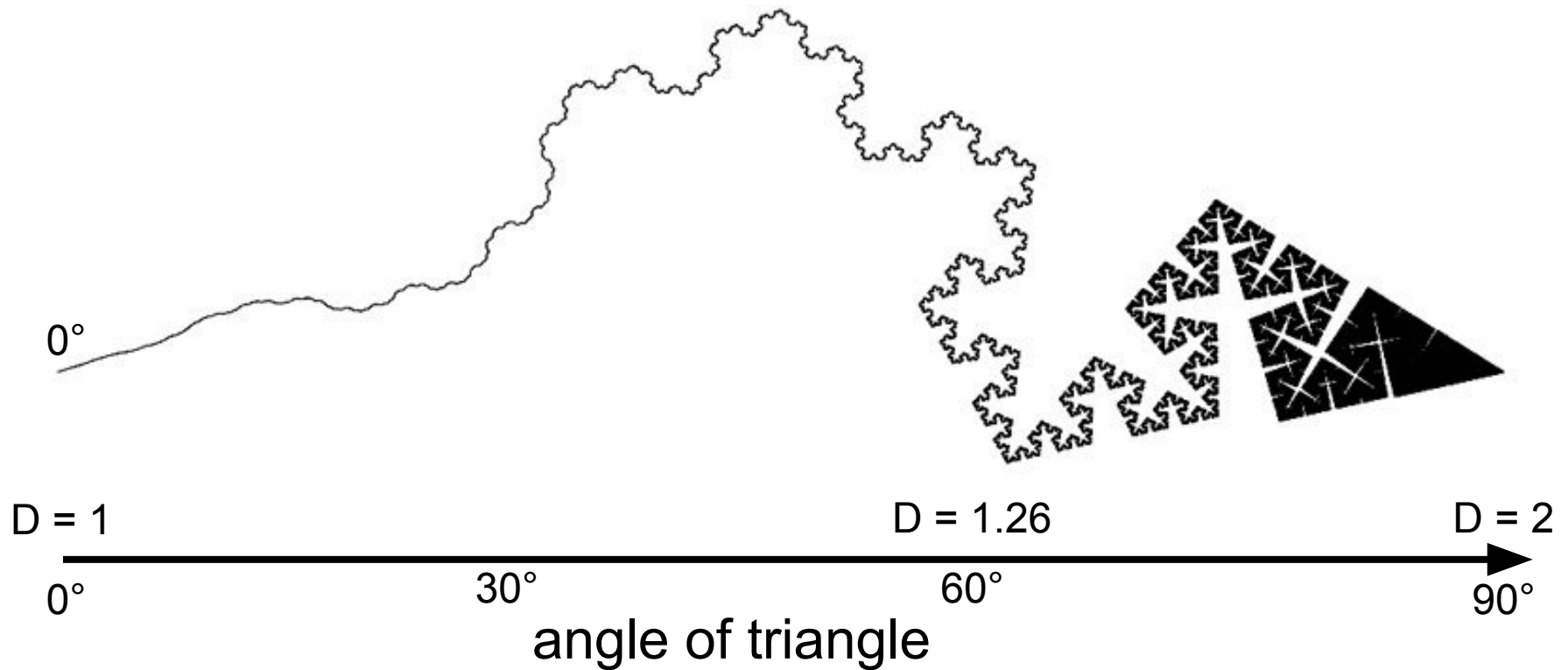
$$64/27 = 2.4$$

$$256/81 = 3.2$$

$$4^n/3^n \rightarrow \infty$$

$$\text{fractal dimension} = \log(4)/\log(3) = 1.26$$

Fractal geometry can increase the dimensionality of the space



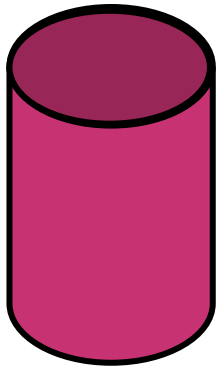
The largest a fractal dimension can be is $1 + \text{spatial dimension}$
The surface area can go from 2 $\square$ 3 dimensions

https://www.researchgate.net/figure/Von-Koch-curve-with-bend-angle-from-0-to-90-degrees_fig1_309391846

Life has found a 4th dimension using fractal geometry! This is why $CL \sim WT^{3/4}$

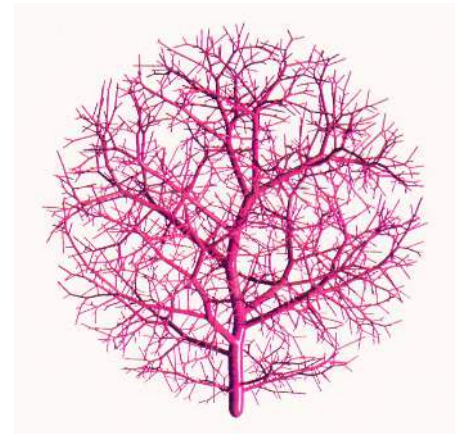
- For “normal” shapes:

- $SA \sim L^2$
- $V \sim L^3$
- $SA \sim V^{2/3} \sim WT^{2/3}$



- For blood vessels

- $SA \sim L^3$
- $V \sim L^4$
- $SA \sim V^{3/4} \sim WT^{3/4}$



1. West, Geoffrey B., James H. Brown, and Brian J. Enquist. "The fourth dimension of life: fractal geometry and allometric scaling of organisms." *Science* 284.5420 (1999): 1677-1679.

Key Lessons

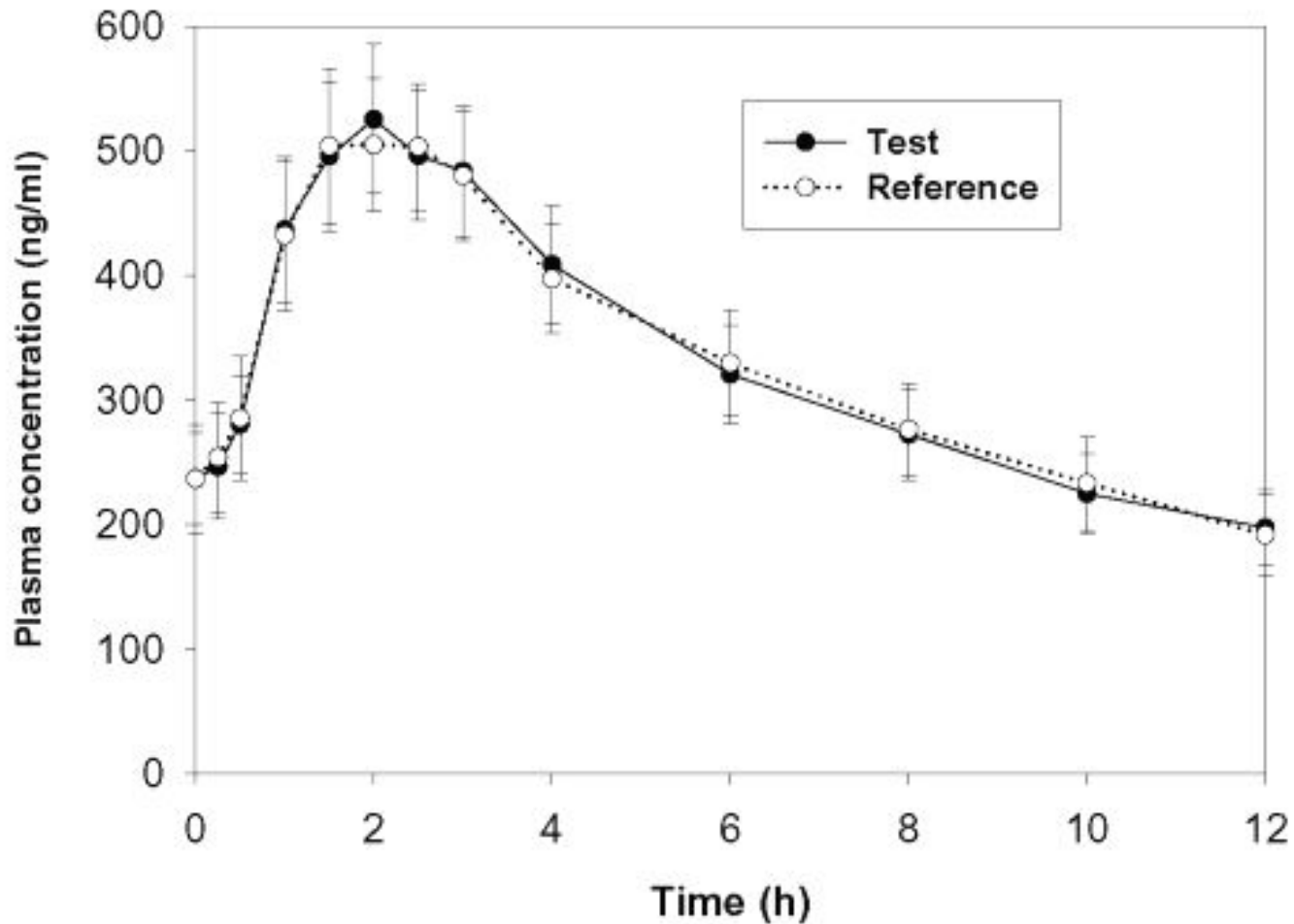
- Generally
 - Clearance scales with $CL \sim WT^{3/4}$
 - Volume scales with $V \sim WT$
- This is a rule of thumb and does not always apply.
Important caveats:
 - Differing mechanisms of drug metabolism across animals
 - Difference between “lean body weight” and total body weight
 - Differences in metabolism with age, especially under 1 year old.
- In practice, estimating the exponent for a particular drug can be challenging due to the limited range in weights that are tested. So often, the $3/4$ exponent is assumed.

Where PK measurements and models are used

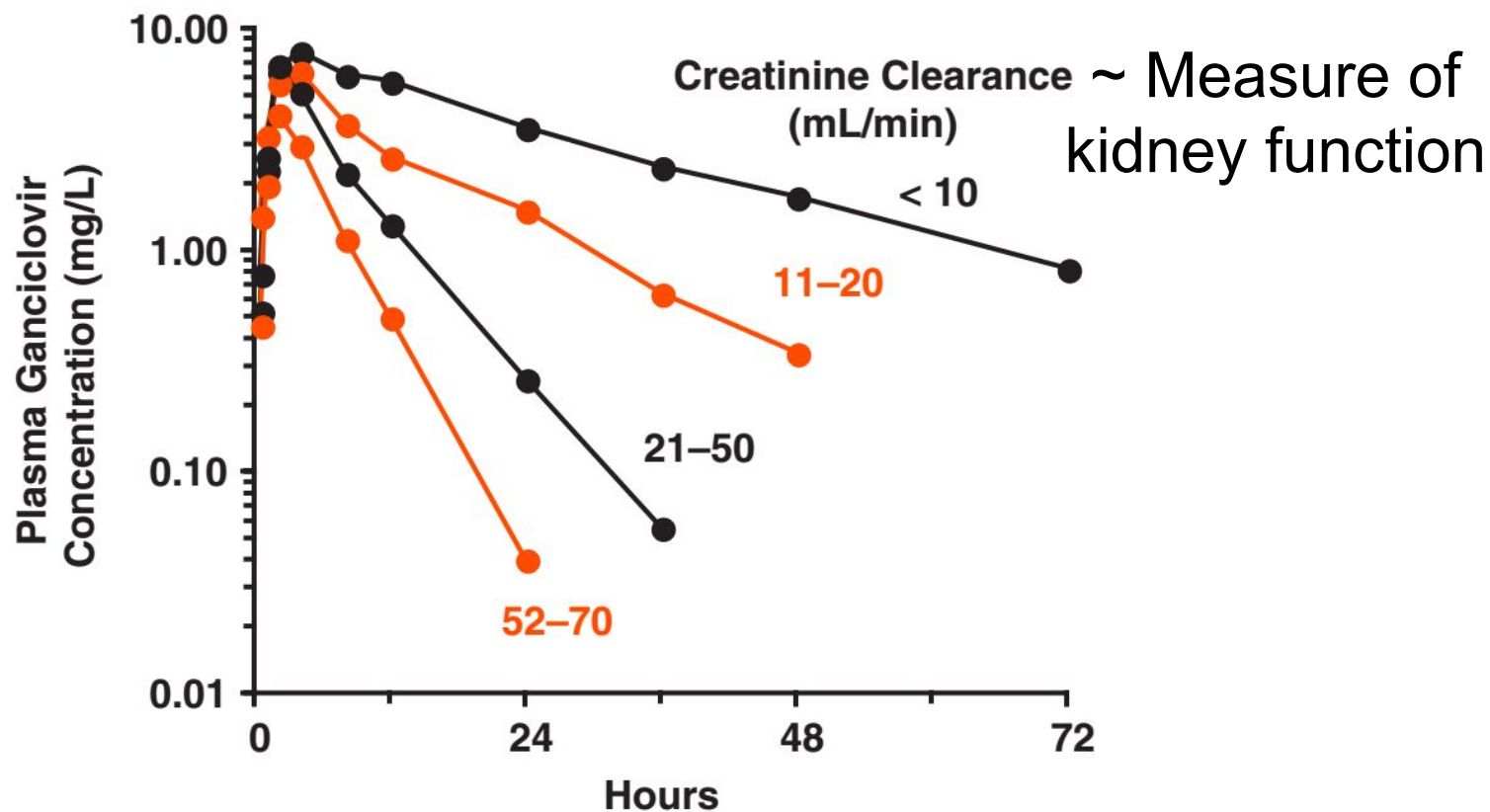
Bioequivalence Postulate

- If the concentration-time profiles for two drugs or dosing conditions are the same then efficacy and toxicity should be the same
 - Basis for generic drugs
 - Basis for formulation changes
 - Basis for examination of drug interactions, food effects, etc.

Mean clozapine plasma concentrations after 7 days of 100 mg BID for 2 formulations in 18 schizophrenic subjects



For drugs that are cleared by kidney, kidney function will affect exposure



Roland and Tozer, Figure 13-14

Some factors that may impact drug concentrations

Factor	Parameter	Mechanism
Liver and kidney function	CL	Small molecules that are cleared by liver and kidneys
Weight	CL, V	Relates to size of patient (V) and metabolizing tissue (CL)
Comedications (e.g. CYP inhibitor)	CL	Affects function of metabolizing enzyme
Comedications (proton pump inhib)	F, ka	Affects gut pH and how well it absorbs drugs
Taken with food	F, ka	impacts how
Genetics (CYP variants)	CL	Some CYPs are polyclonal

Backups

Acetaminophen Overdose

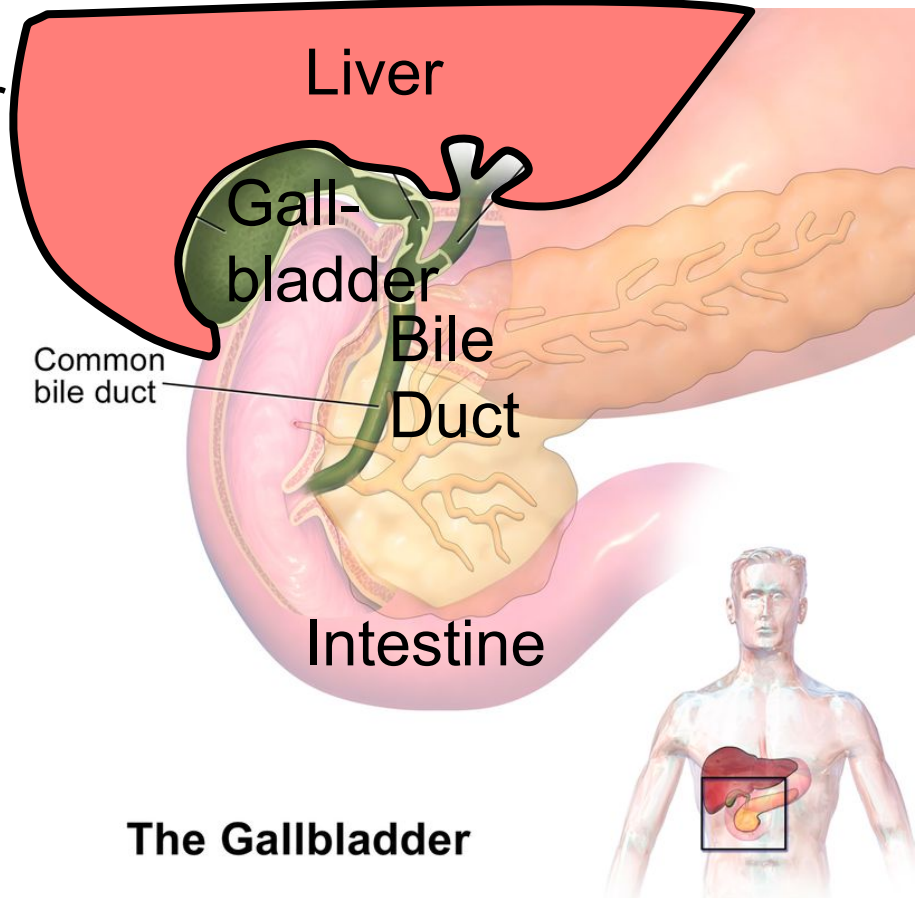
- Acetaminophen is Phase 2 conjugated by glutathione
- Large doses deplete the glutathione and sulfate pools
- Toxic metabolite then binds to cellular macromolecules
- Clinical course:
 - Nausea, vomiting (Day 1)
 - Hepatic enzymes $\uparrow$, right upper quadrant sensitive to touch (Day 2 to 3)
 - Hepatic necrosis, possibly renal failure, and cardiac abnormalities (Days 3 to 5)



- Smallest dose recorded for hepatotoxicity in adults is 5.4 g
- 10 g is lethal
- Therapy is targeted at replenishing sulfate pools

Biliary Elimination

- Bile is secreted from the liver to the gallbladder and to the intestine
- Bile aids absorption of fats
 - breaks down large fat globules into smaller ones
- Drugs may be excreted by biliary route



In the two compartment model, “volume” is a function of time

- Recall that volume relates amount in body to concentration measured in circulation.
- For 1 compartment model:
 - $C(t) = A(t)/V$
 - There is only one volume.
- For a two compartment model with central CL, there are:
 - Two volume parameters: V_1 and V_2 .
 - There is also a volume function: $C(t) = A(t)/V(t)$
 - At time 0, $C(0) = A(0)/V_1$
 - After a single dose, at long times, $C(t) = A(t)/V_z$ where $V_z = CL/\beta$
 - At steady state after multiple doses:
 - $C(t_{ss}) = A(t_{ss})/V_{ss}$ where: $V_{ss} = V_1 \cdot [1 + k_{12}/k_{21}]$

Sketch of derivation of V_z and V_{ss}

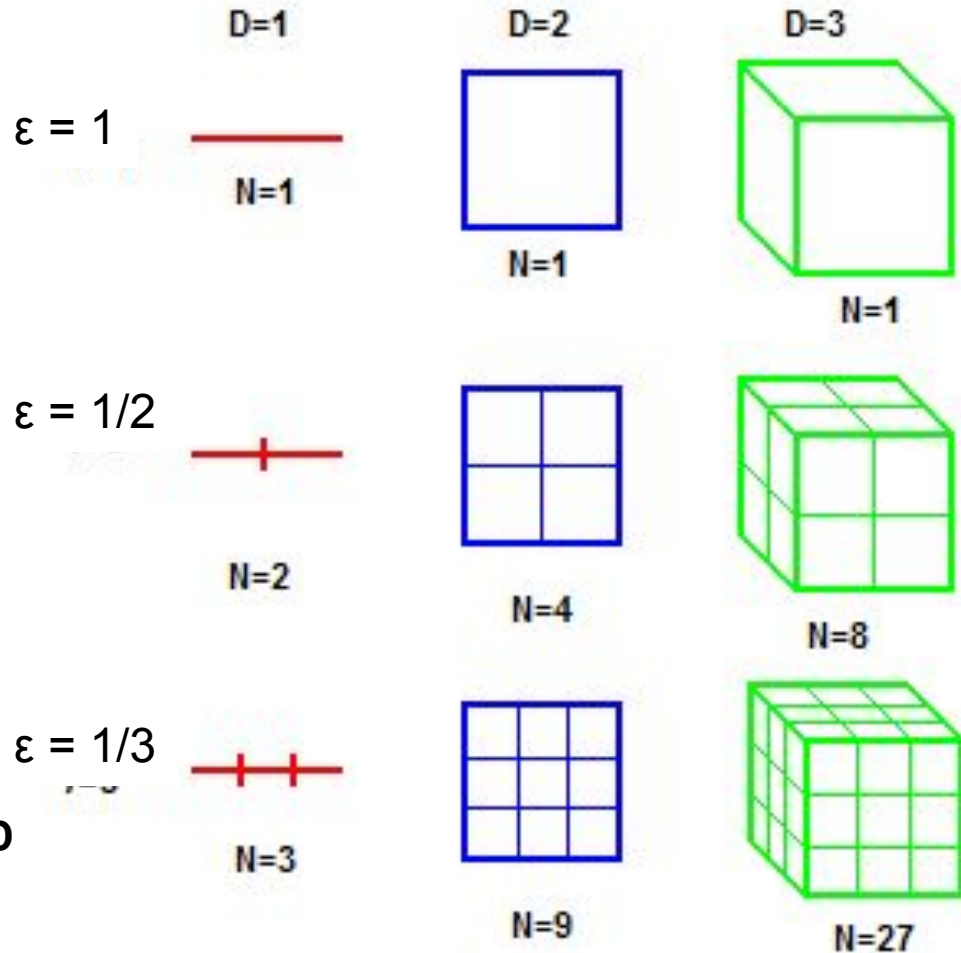
- For the derivation, we start with the definition of $V(t)$

$$V(t) = \frac{A(t)}{C(t)} = \frac{Dose - CL \int_0^t C(t)dt}{C(t)} = \frac{CL}{C(t)} \int_t^\infty C(t)dt$$

- To derive V_z and V_{ss} , we then:
 - Use the analytic expression for $C(t)$ for the either single dose (V_z) or multiple dose (V_{ss})
 - Take the limit as $t \rightarrow \infty$

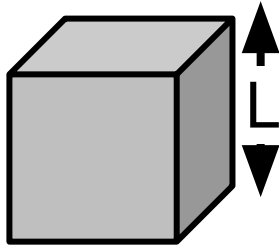
Definition of a dimension

- Let N = number of shapes (sticks, squares or cubes) needed to cover a big shape.
- Now reduce the length of each side of shape by a factor ε (e.g. $1/3$)
- Then the dimension (D) is such that: $N \sim \varepsilon^{-D}$



For normal shapes, surface area relates to weight by 2/3 power

- Cube



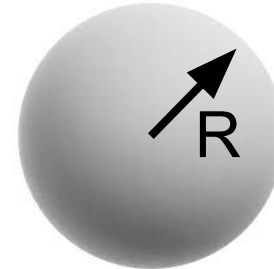
$$SA = 6L^2$$

$$V = L^3$$

$$SA = c_1 \cdot V^{2/3} \sim WT^{2/3}$$

c_1 is a constant

- Sphere



$$SA = 4\pi R^2$$

$$V = (4/3)\pi R^3$$

$$SA = c_2 \cdot V^{2/3} \sim WT^{2/3}$$

c_2 is a constant

- As V increases, SA increases too, but the $SA:V$ ratio decreases.
- This 2/3 ratio holds at the macroscale, but on the microscale, it can be possible for SA to have > 2 dimensions.